



waterscales



Engineering and
Physical Sciences
Research Council



STIFTELSEN
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JEBSEN



simula

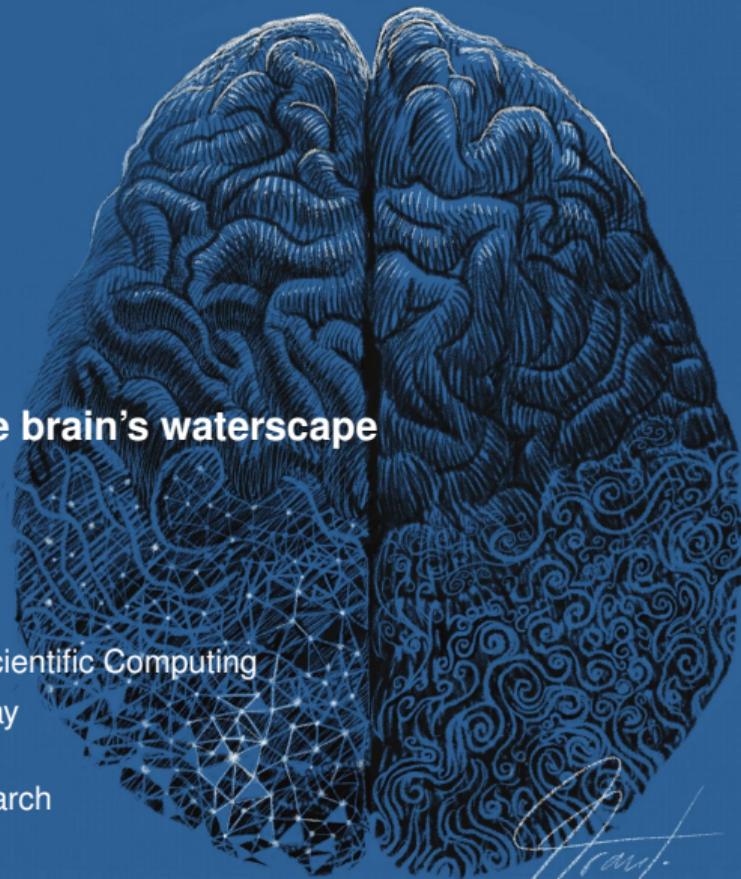
Brains in motion

Computational modelling of the brain's waterscape

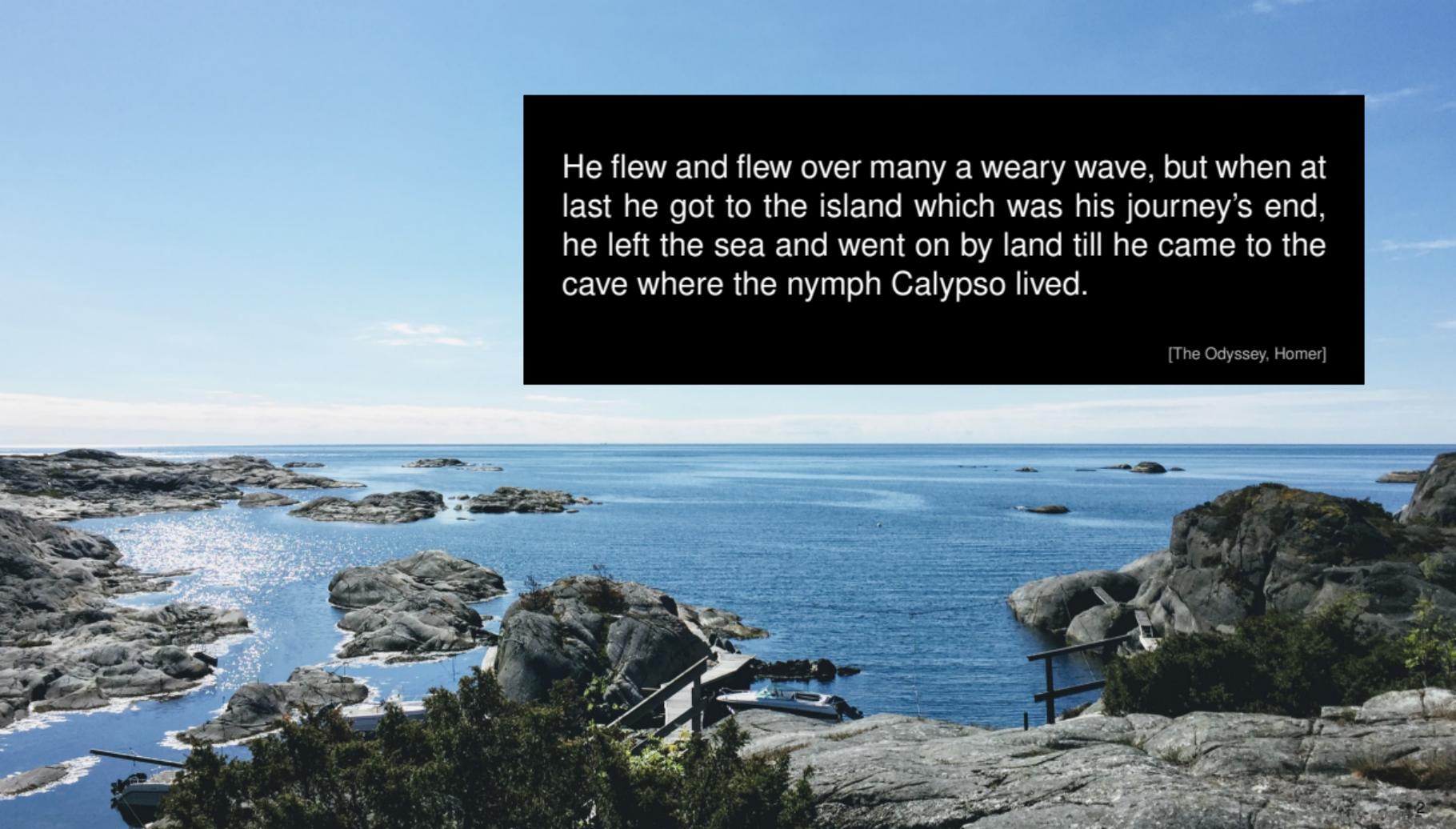
Marie E. Rognes

Department of Numerical Analysis and Scientific Computing
Simula Research Laboratory, Oslo, Norway

K. G. Jebsen Centre for Brain Fluid Research





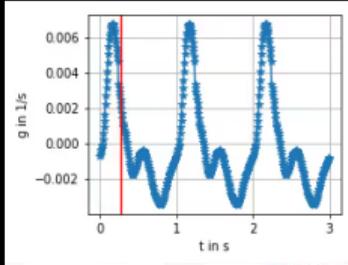


He flew and flew over many a weary wave, but when at last he got to the island which was his journey's end, he left the sea and went on by land till he came to the cave where the nymph Calypso lived.

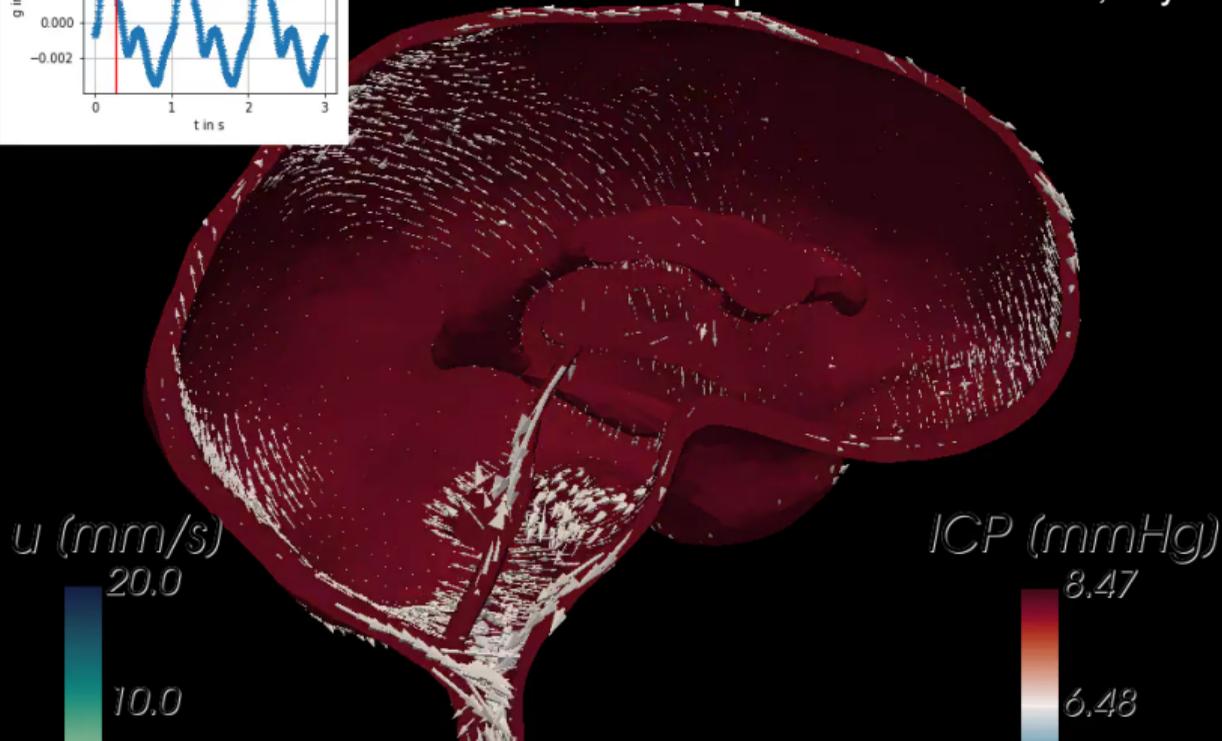
[The Odyssey, Homer]

The brain and its cerebrospinal fluid (CSF) environment pulsates in synchrony with the cardiac and respiratory cycles

Causemann et al. [2022]

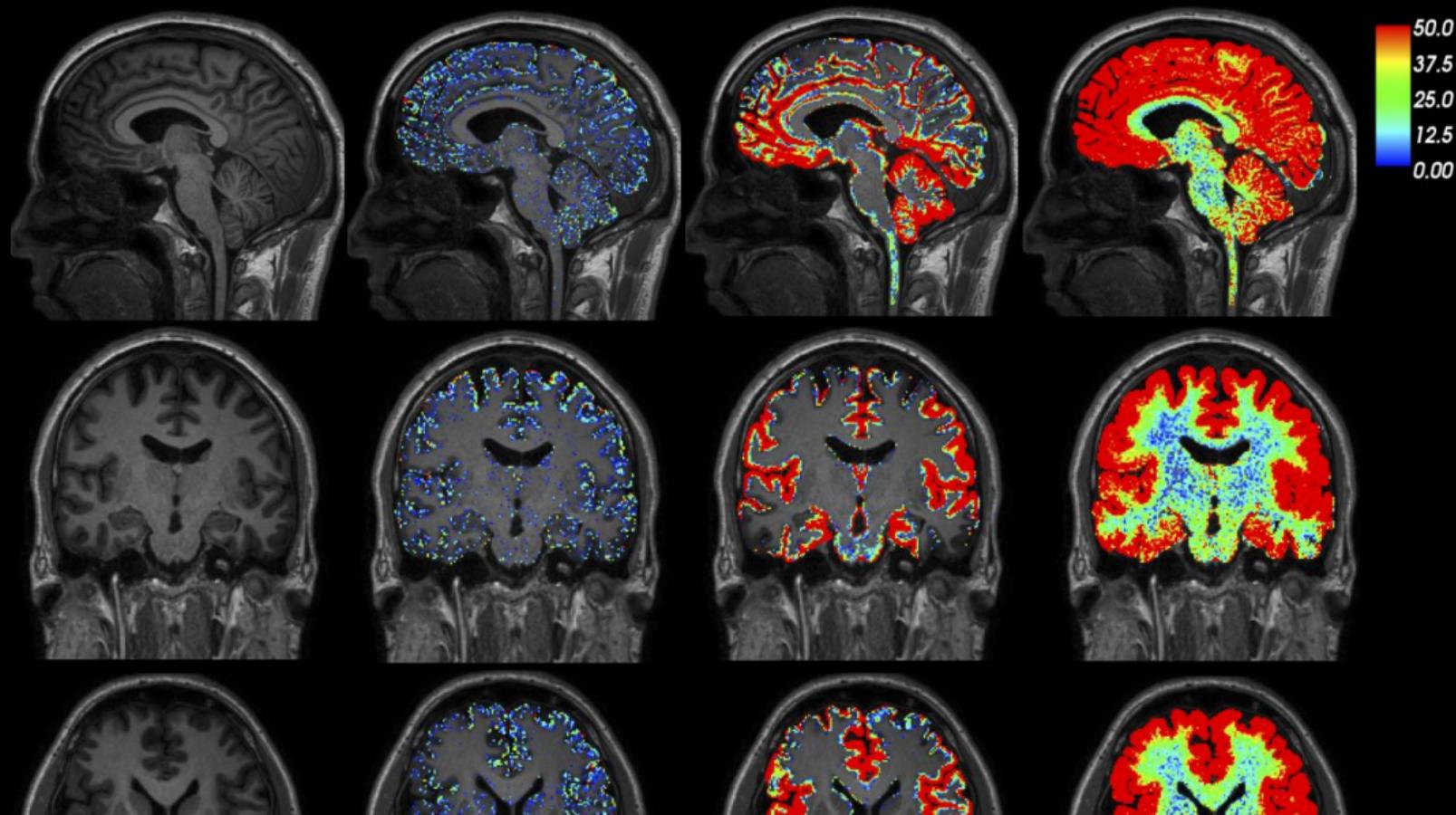


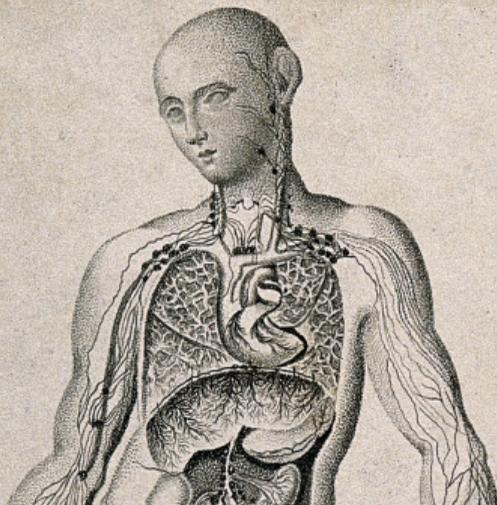
Coupled Biot & Stokes equations (Brain & CSF)
Total pressure formulation, Taylor–Hood elements



MRI reveals human brain-wide tracer enhancement and clearance

Ringstad et al. [2017, 2018]





This Figure is copied from the late M. Cruikshanks's, but 'twice half the size, it is supposed to be in a manner transparent except a few of the principal vessels, in the Thorax and Stomach, left with a view to show their absorbents. The whole from Injections made by



Fig. 5.

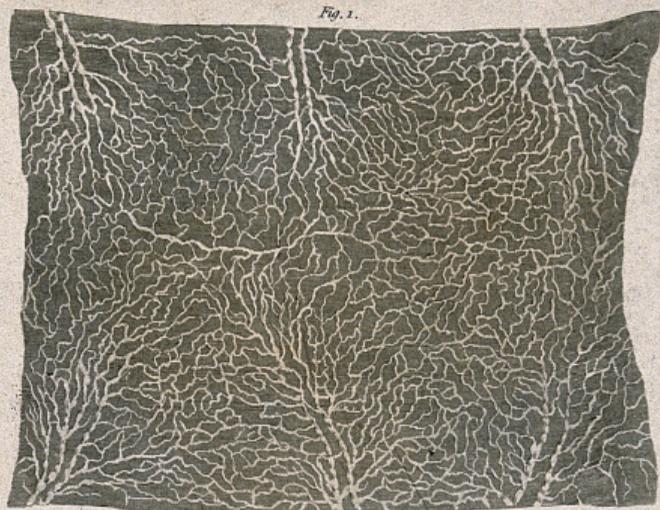


Fig. 1.

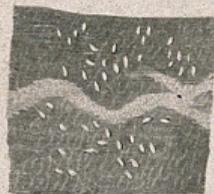


Fig. 2.

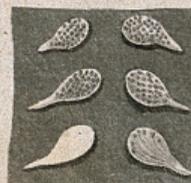


Fig. 3.

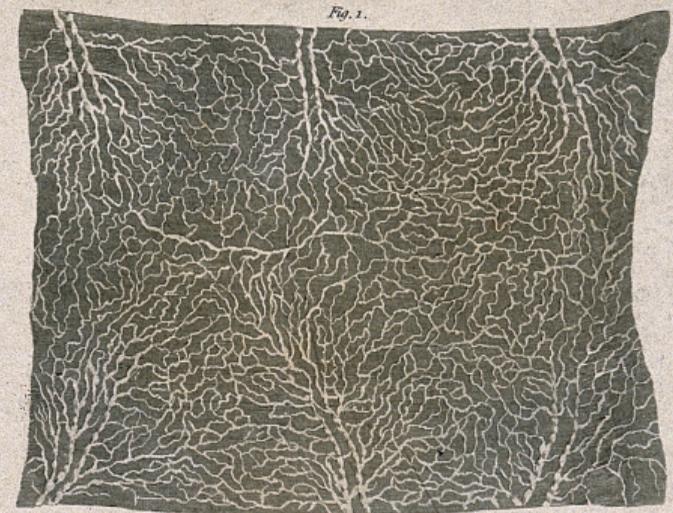
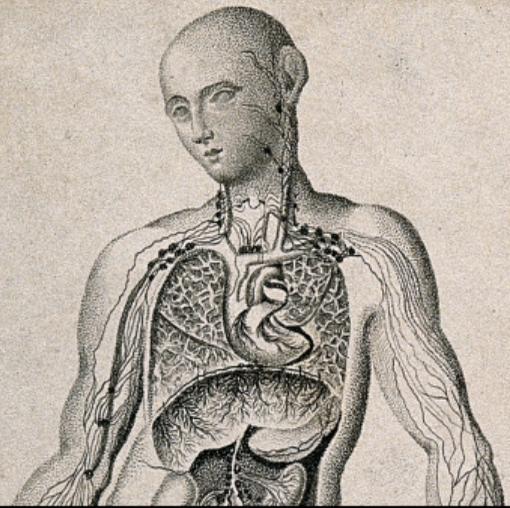


Fig. 4.

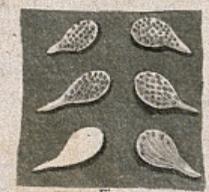
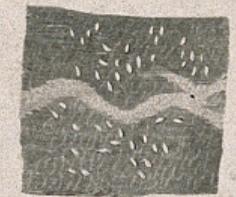
D. Baillie on the absorbent Vessels 1. & 2. Lectures, Windmill Street.

The Mark explained over leaf to be Pl. IV.





Where are the lymph vessels of the brain?

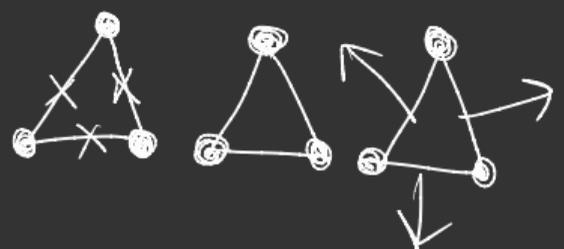


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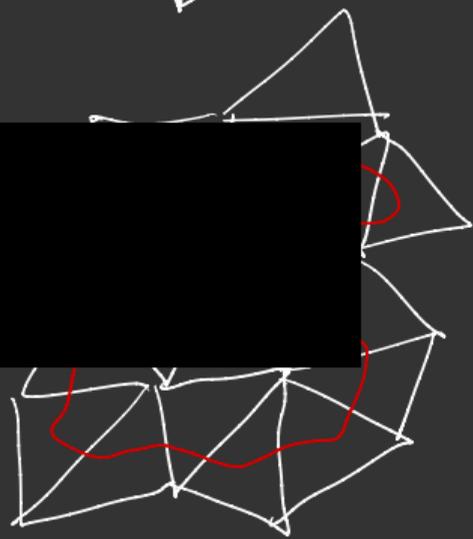
$C_m v = \pm I_m \pm \text{ker}(v)$
 where I_m are subject to modelling



Denote \mathcal{S}_T
 $\text{div } u - \alpha \cdot p$

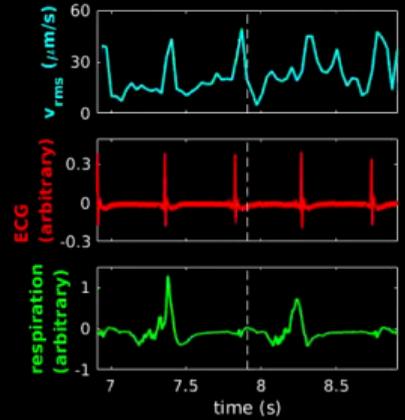
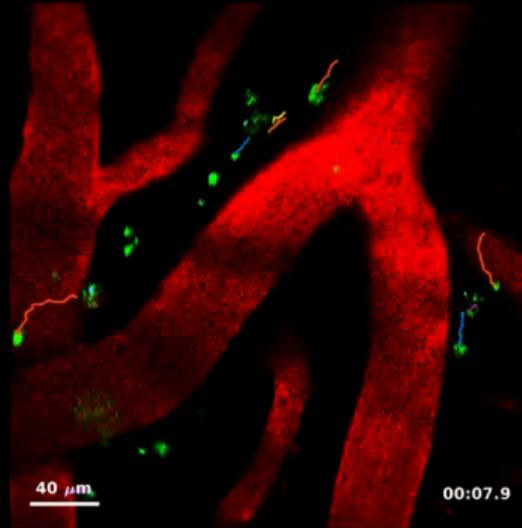
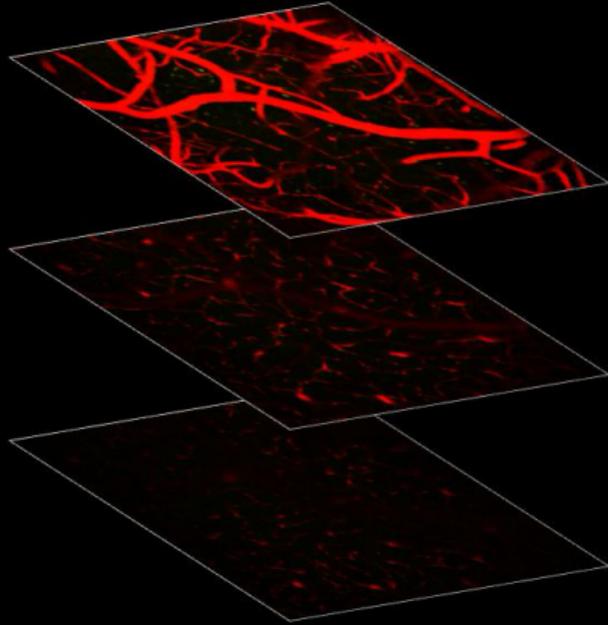
I. How do solutes travel into the brain?

with $E = -\text{div } \mathbf{z}$
 yielding the operator $-\text{div } \mathbf{z} u$
 $\text{div } \mathbf{z} u$
 $\mathcal{H} \rightarrow \mathcal{H} \rightarrow \mathcal{H}$
 $\mathcal{H} \rightarrow \mathcal{H} \rightarrow \mathcal{H}$
 $\mathcal{H} \rightarrow \mathcal{H} \rightarrow \mathcal{H}$
 The bilinear form is symmetric



Lemma:

Solutes travel via preferential perivascular pathways – driven by ...?

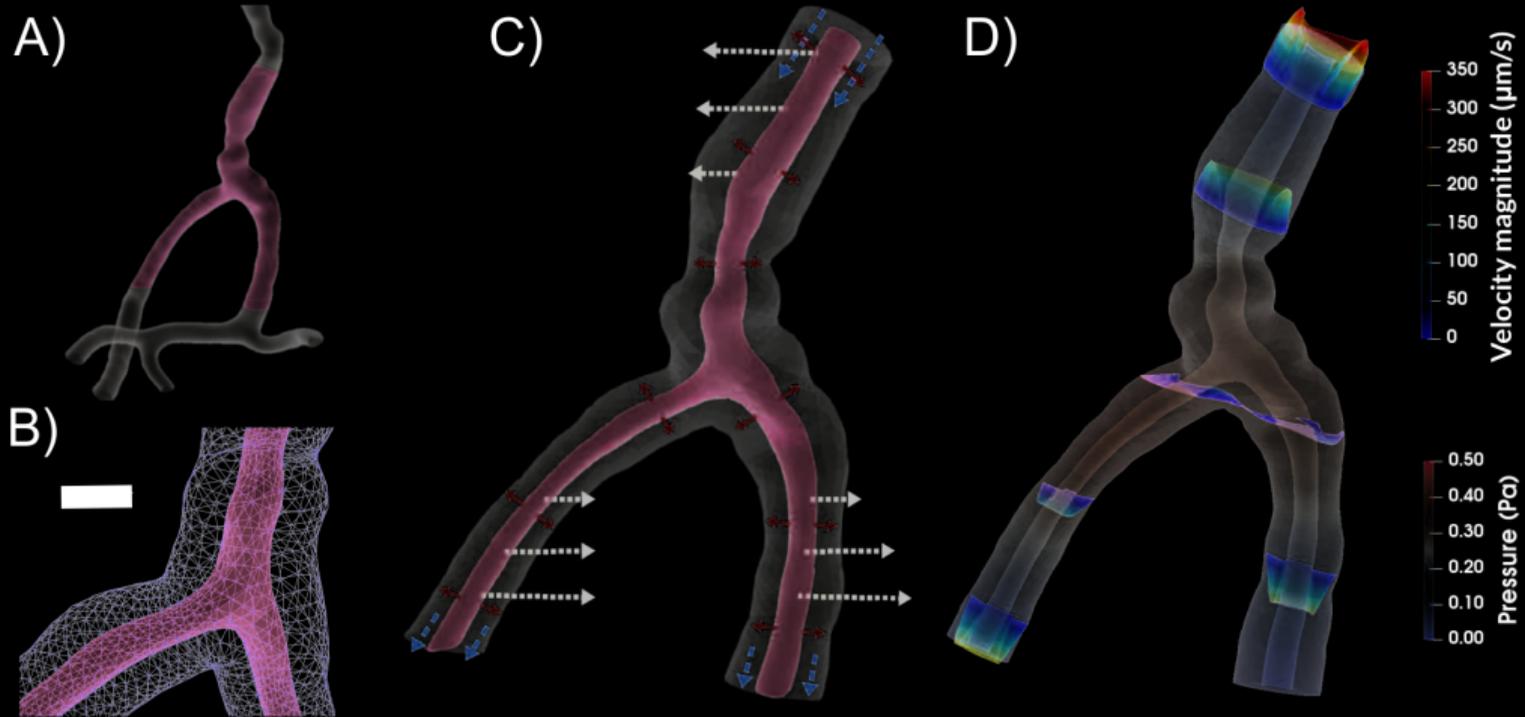


[Illiff et al, Sci. Transl. Med, 2012 (Movie S1)]

[Mestre et al, Nat. Comms, 2018 (Movie S2)]

What mechanisms drive perivascular flow and transport?

Daversin-Catty et al. [2020]



Incompressible Stokes flow (low Reynolds, low Womersley numbers)

Model length and wave speed modulate PVS velocity and net flow

Daversin-Catty et al. [2020]

PVS thought example:

Annular cylinder L (mm) long

Wave speed $c = 1000$ mm/s

Frequency $f = 10$ Hz = 10 /s

Wave length λ is speed
divided by frequency:

$$\lambda = c/f = 100 \text{ mm}$$

For instance:

$$L = 1 \text{ mm} = 0.01 \lambda$$

$$L = 50 \text{ mm} = 0.5 \lambda$$

$$L = 100 \text{ mm} = 1 \lambda$$

Model length and wave speed modulate PVS velocity and net flow

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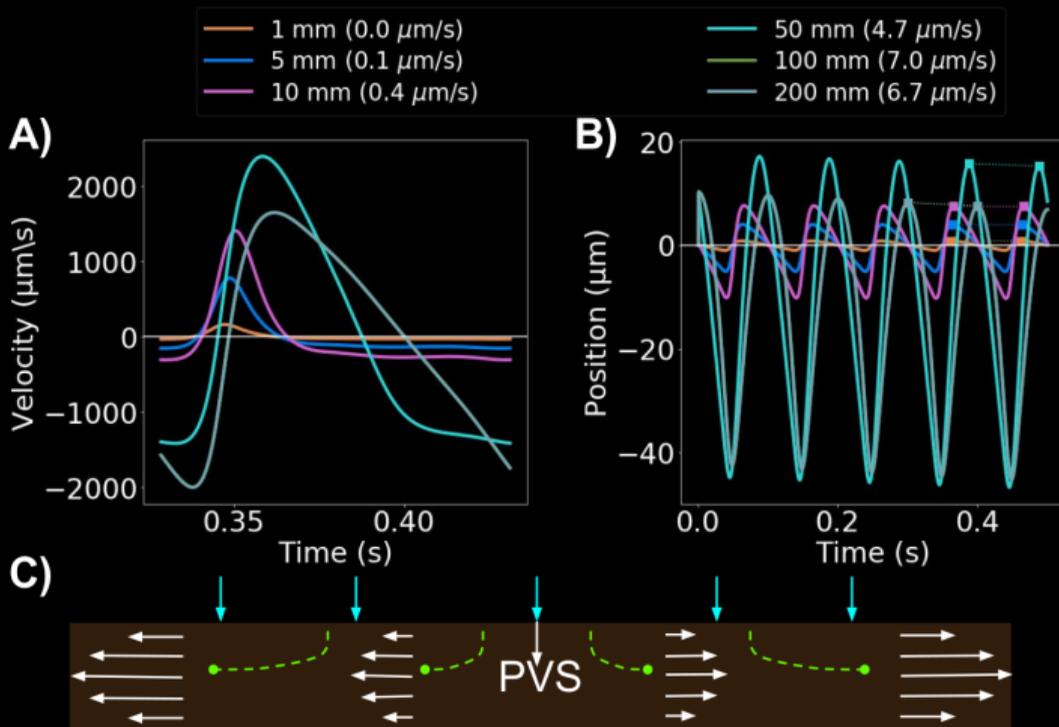
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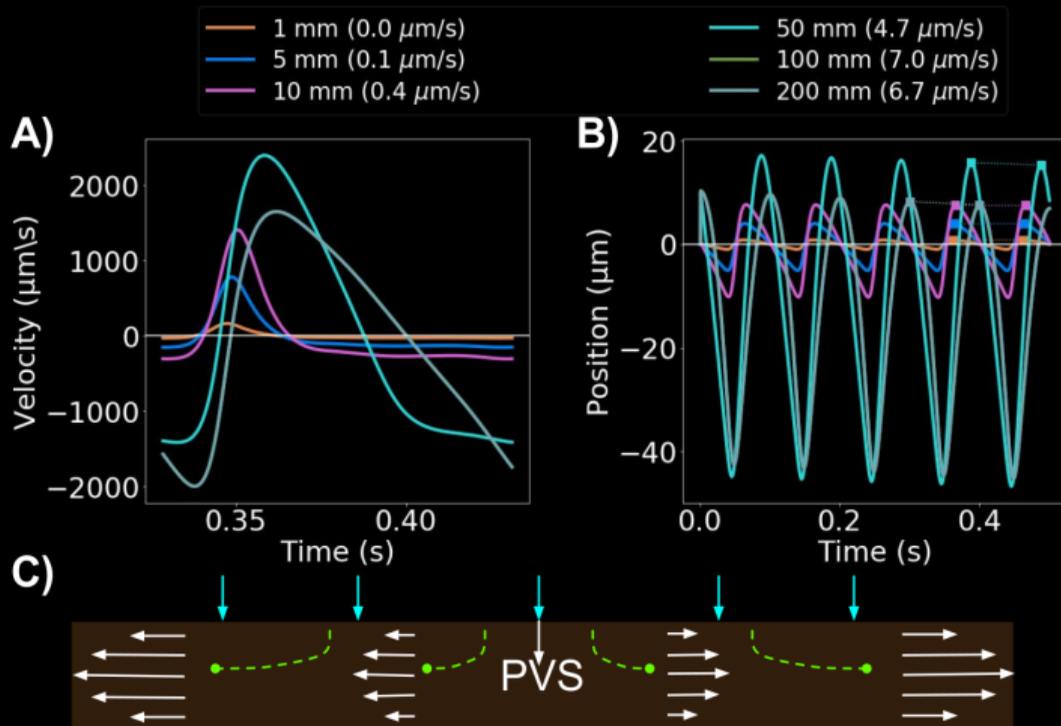
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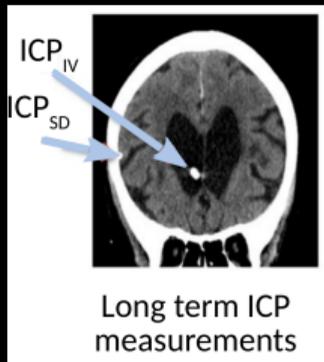
$L = 100$ mm = 1λ



[Wang and Olbricht (2011), Thomas (2019), Carr et al (2021): $L \gg \lambda$]

ICP (gradients) pulsate in sync with cardiac and respiratory cycles

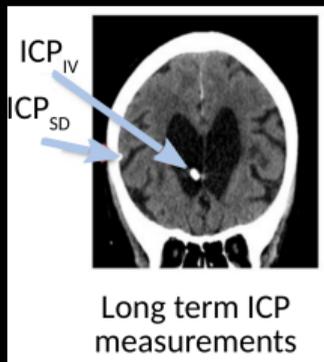
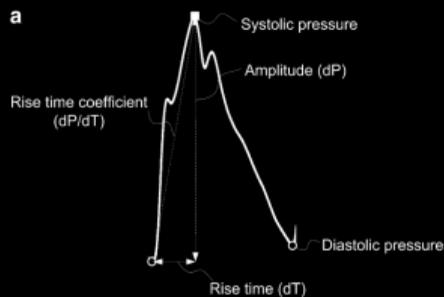
Vinje et al. [2019]



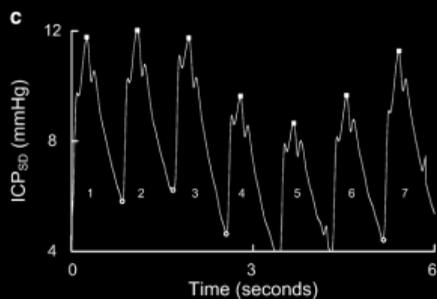
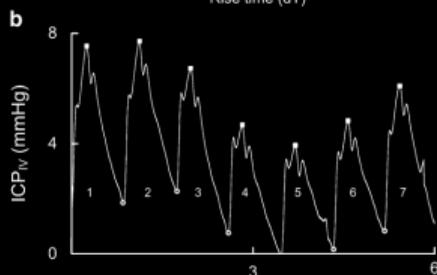
[Eide and Sæhle (2010)]

ICP (gradients) pulsate in sync with cardiac and respiratory cycles

Vinje et al. [2019]

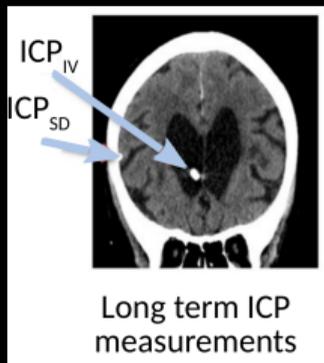
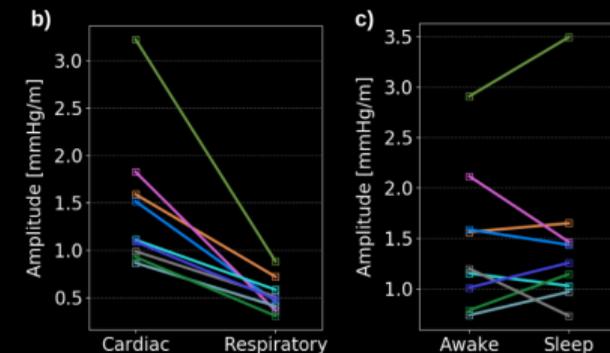
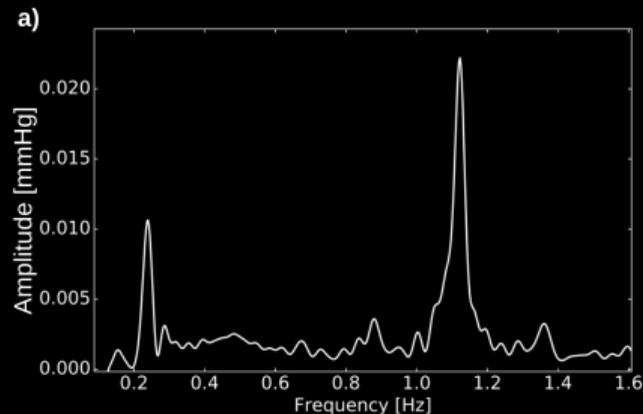
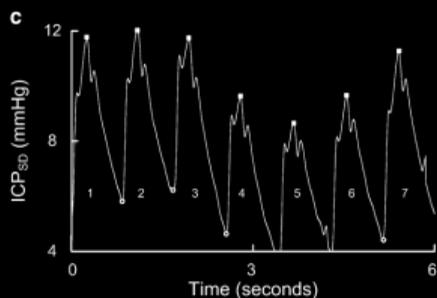
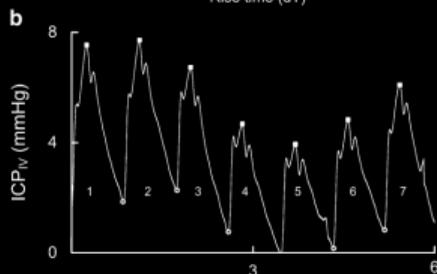
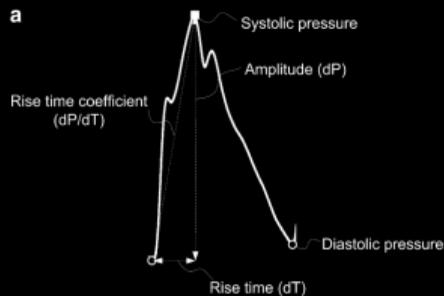


[Eide and Sæhle (2010)]



ICP (gradients) pulsate in sync with cardiac and respiratory cycles

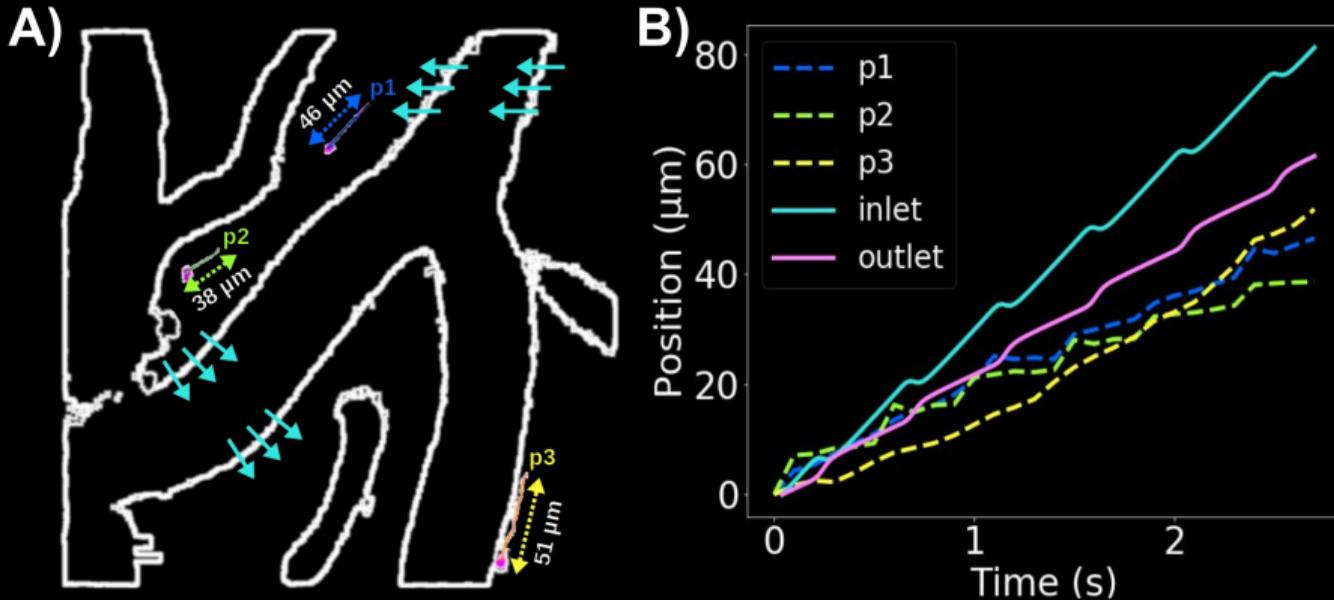
Vinje et al. [2019]



[Eide and Sæhle (2010)]

$$dICP(t) \approx a_c \sin(2\pi f_c t) + a_r \sin(2\pi f_r t)$$

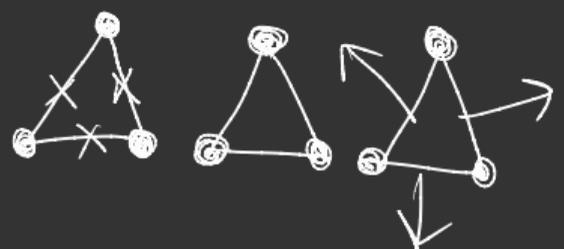
Rigid motions, arterial wall pulsations and a static pressure gradient induced oscillatory PVS flow in agreement with experimental findings



Wall pulsation frequency: 2.2 Hz. Static pressure gradient: 1.46 mmHg.



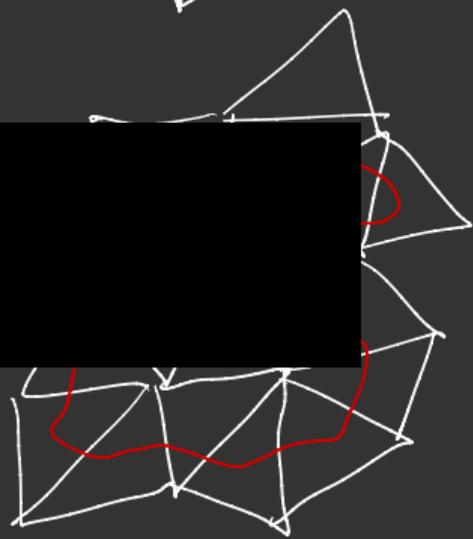
$C_m v = \pm I_m \pm \text{ker}(v)$
 where I_m are subject
 to modelling



Denote $\frac{\partial}{\partial x}$
 $\text{div } u = \text{d.o.P}$
 Poisson

II. Where do solutes travel into and out of the brain?

yielding the operator
 $-\text{div } \mathcal{L} u$
 $\text{div } \mathcal{L} u$
 $\mathcal{L} u = \mathcal{L} \frac{\partial u}{\partial x}$
 $\mathcal{L} u = \mathcal{L} \frac{\partial u}{\partial t}$
 $\mathcal{L} u = \mathcal{L} \frac{\partial u}{\partial t}$

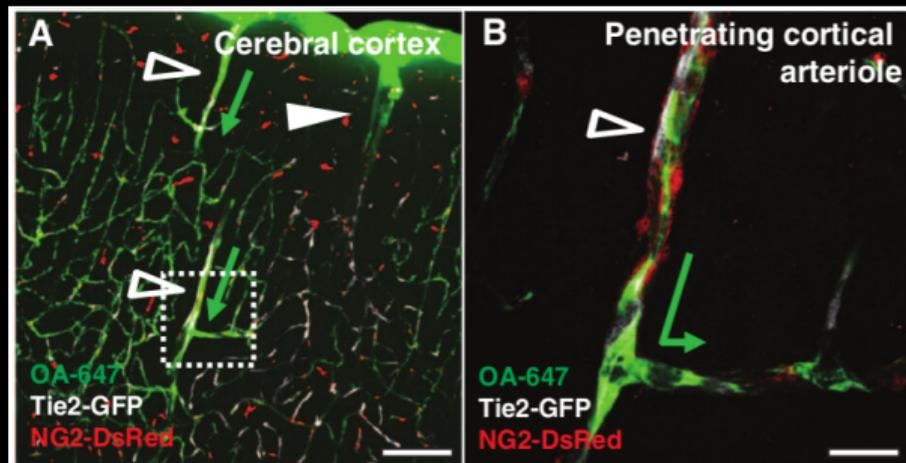


Lemma:

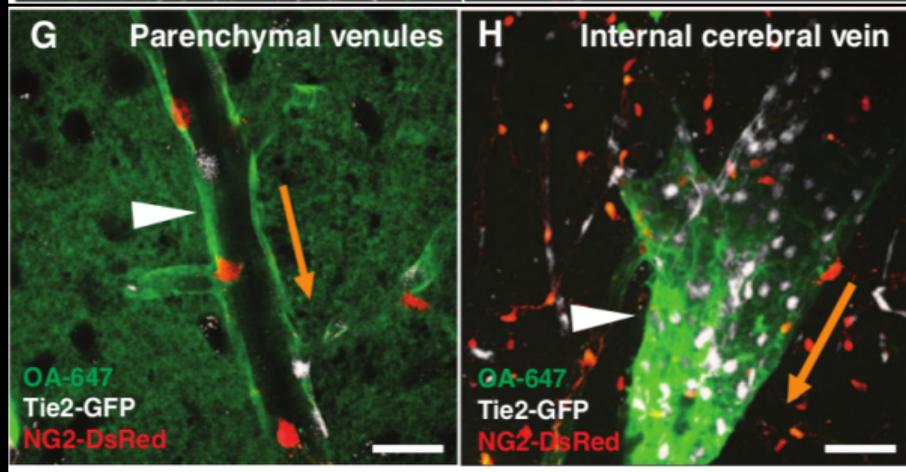
The bilinear form is symmetric

Analysis in \mathbb{R}^d

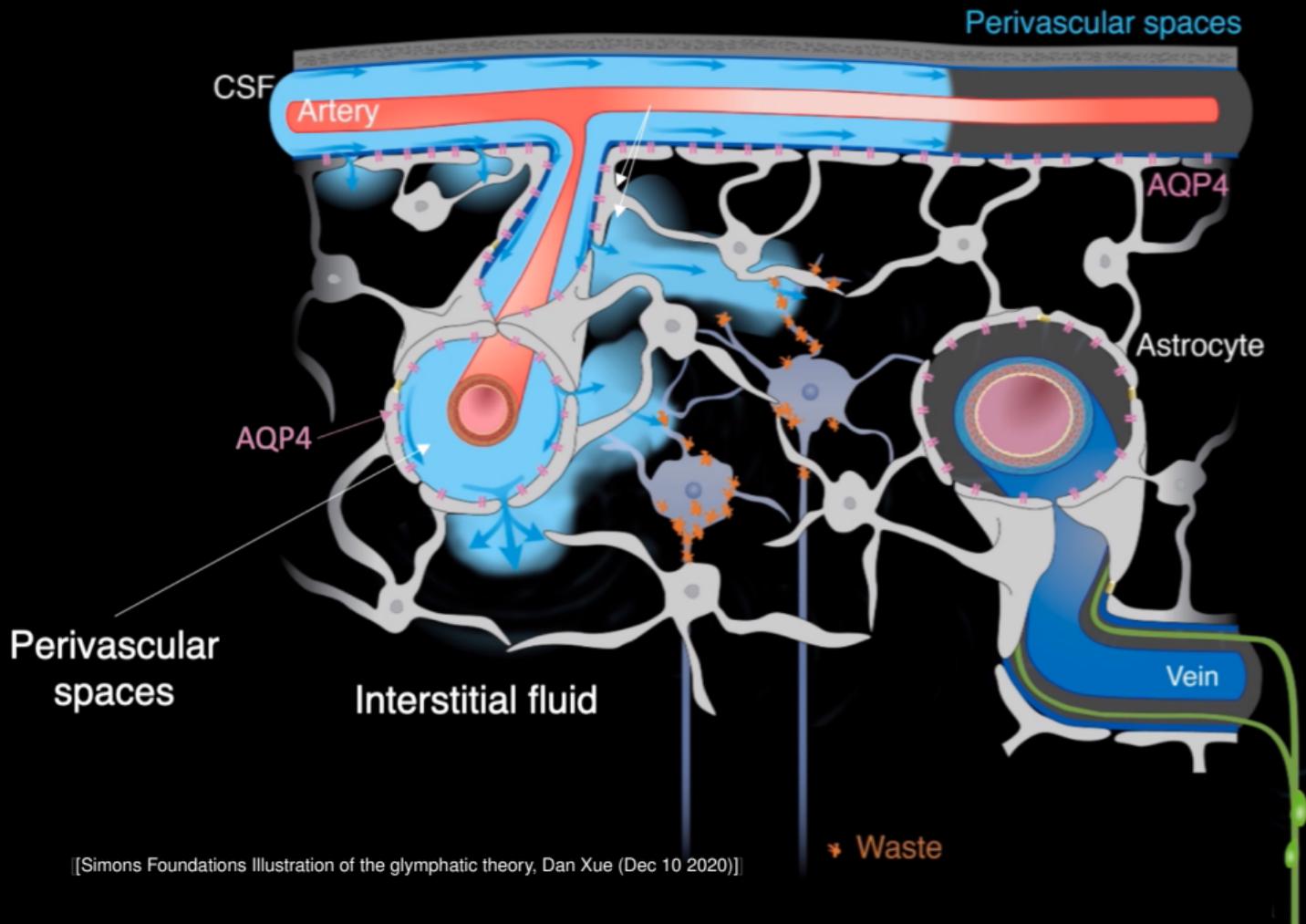
Periarterial entry? (t = 10 min)



Perivenous exit? (t = 180 min)



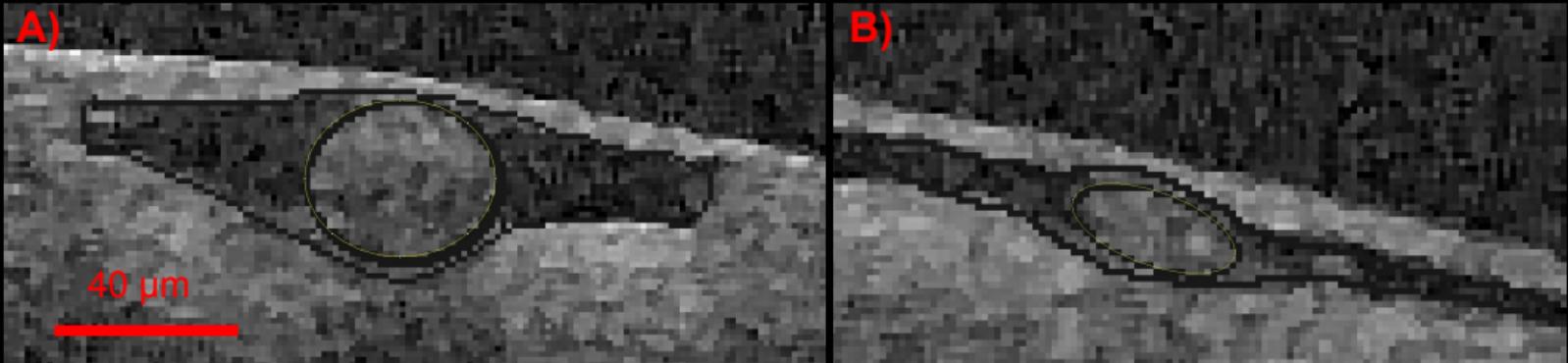
[Ilf et al, Sci. Transl. Med, 2012 (Fig 3)]



[Simons Foundations Illustration of the glymphatic theory, Dan Xue (Dec 10 2020)]

Iliff et al, 2012
Louveau et al., 2015

How do geometrical differences between periarterial and perivenous spaces affect their CSF flow patterns?



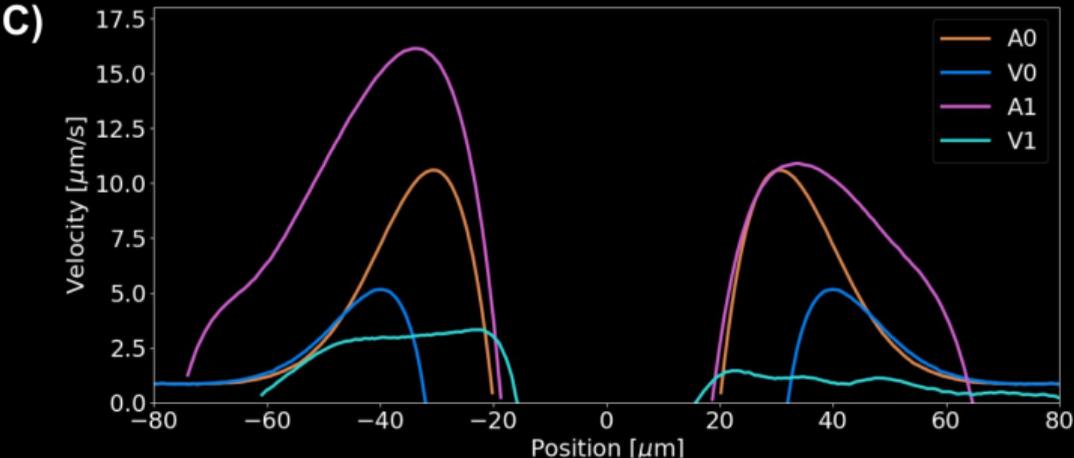
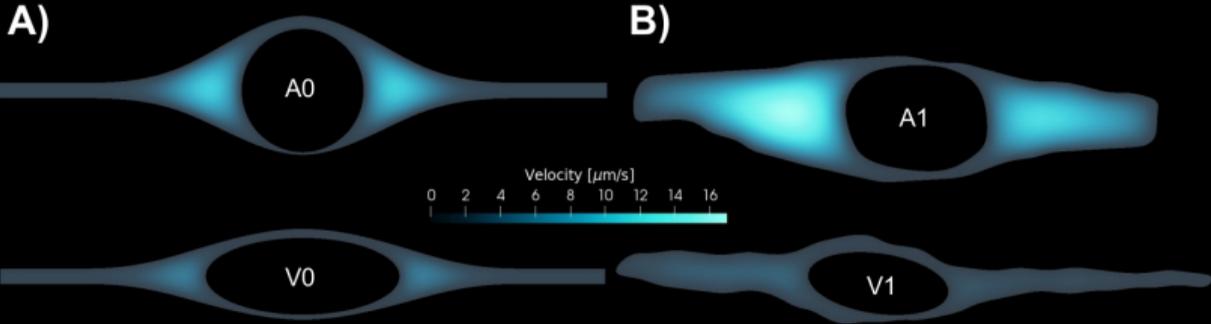
In vivo OCT images of blood vessels taken of the surface of a human brain (courtesy of Erik N. T. P. Bakker and colleagues). Scale after scaling to mouse scale

With these images (and idealized versions) as representative cross-sections, compute the **CSF velocity** and **net flow** along the length of the perivascular space given a static pressure gradient (of 1.46 mmHg/m).

Next, compute **tracer concentration** (2000 kDa) transported by diffusion and convection in the respective PVSs.

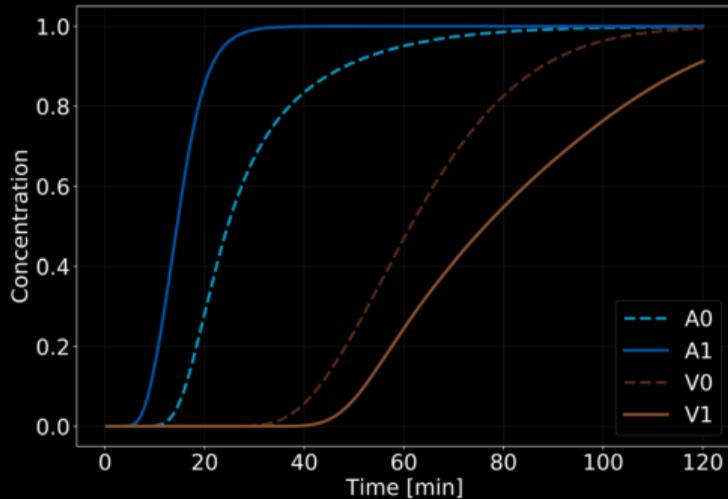
Same pressure gradient induce higher velocities and higher net flow in periarterial than in perivenous spaces

Vinje et al. [2021]

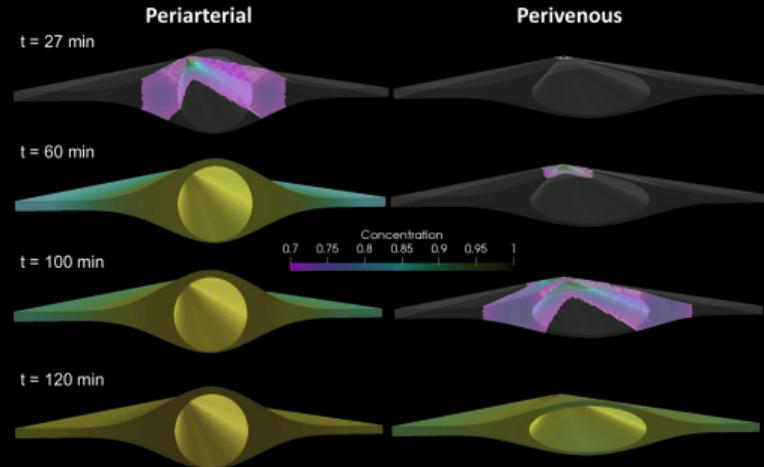


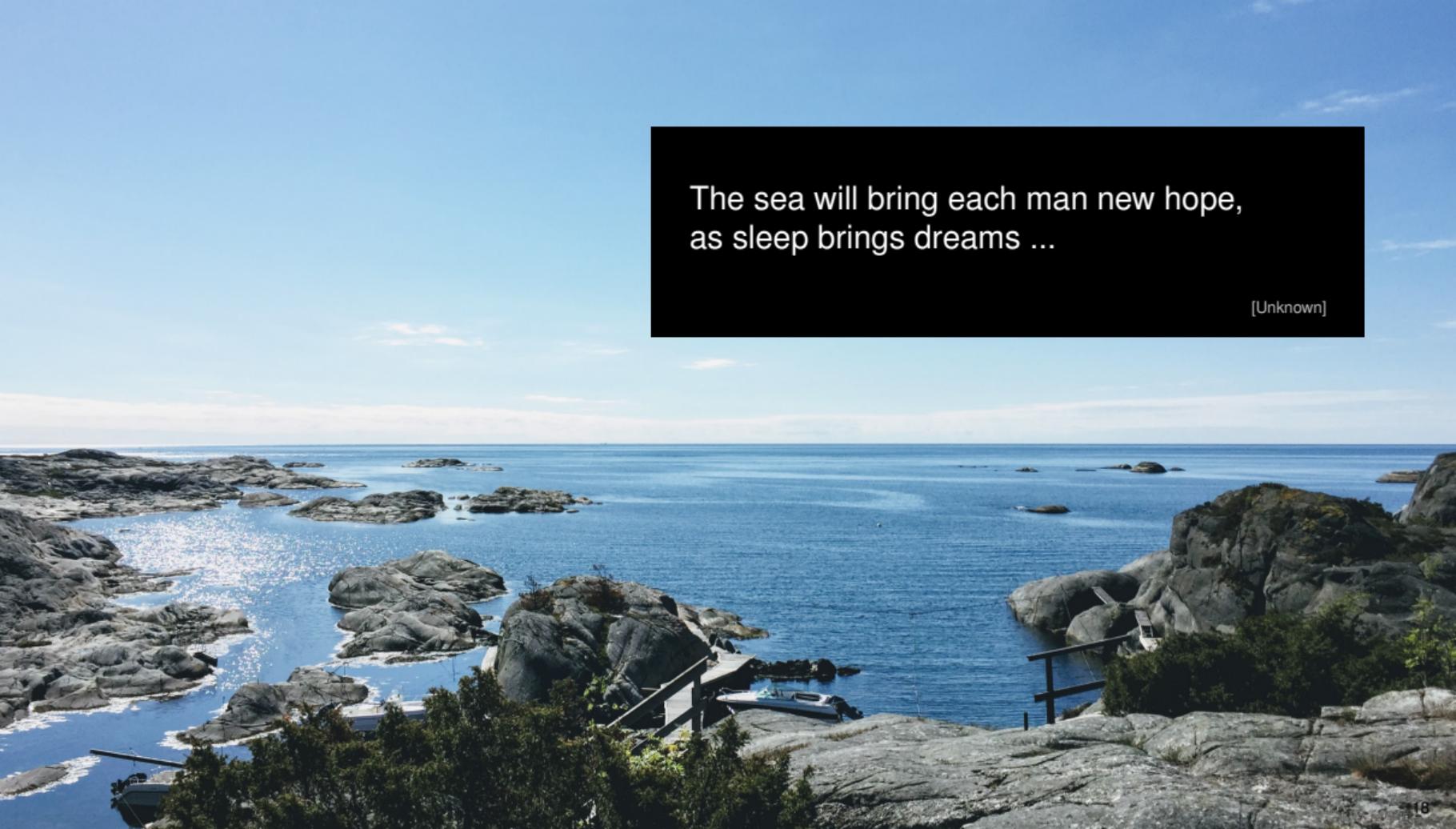
Differences in geometry lead to more rapid tracer transport and earlier arrival times in periarterial compared to perivenous spaces

Vinje et al. [2021]



Concentration at measurement site
(5 mm downstream from injection site)

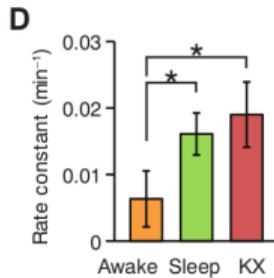
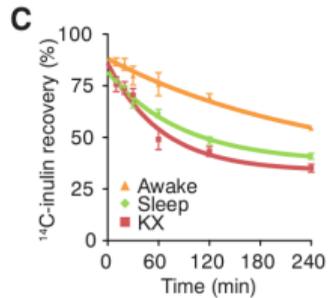
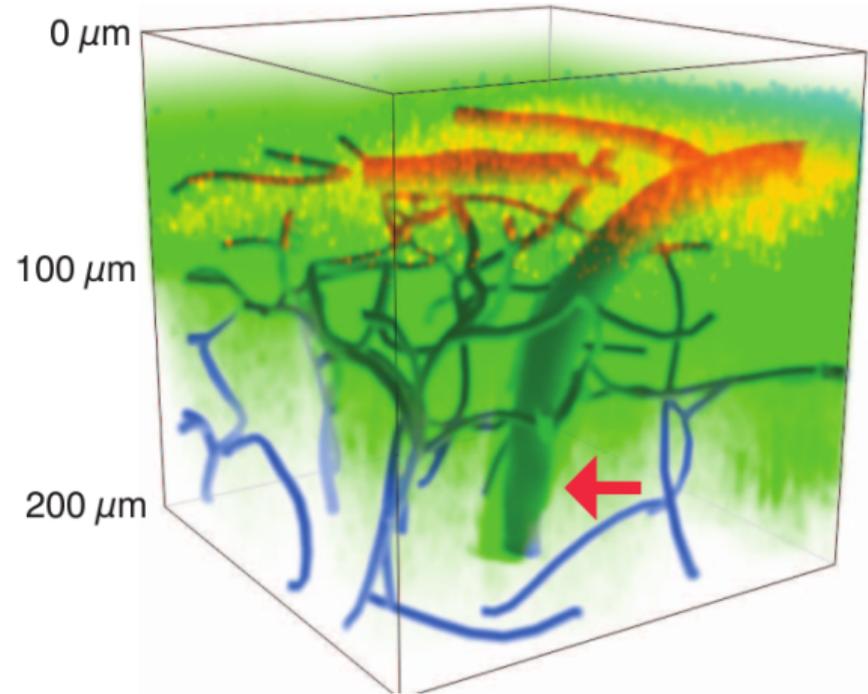
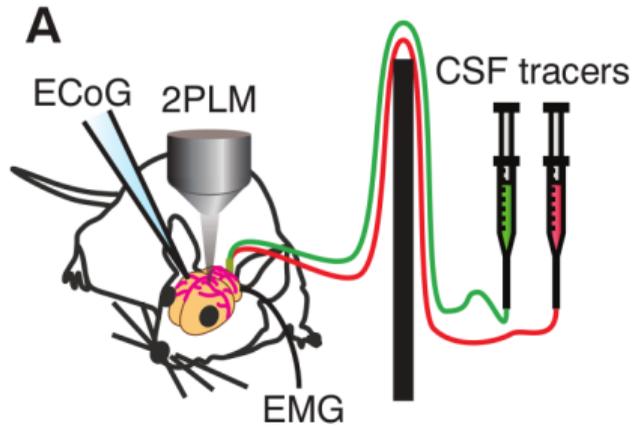




The sea will bring each man new hope,
as sleep brings dreams ...

[Unknown]

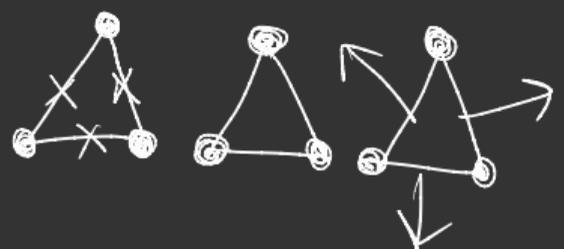
Sleep: a fundamental driver of metabolic clearance from the brain?



Xie et al. [2013], Fultz et al. [2019], Ma et al. [2019], Bojarskaite et al. [2023], Vinje et al. [2023], Miao et al. [2024]



$C_m v = \pm I_m \pm \text{kon}(v)$
 where I_m are subject to modelling



Denote $\frac{\partial}{\partial t}$
 $\text{div } u - \alpha \cdot P$
 Poisson

III. How is solute transport affected by CSF flow during sleep?

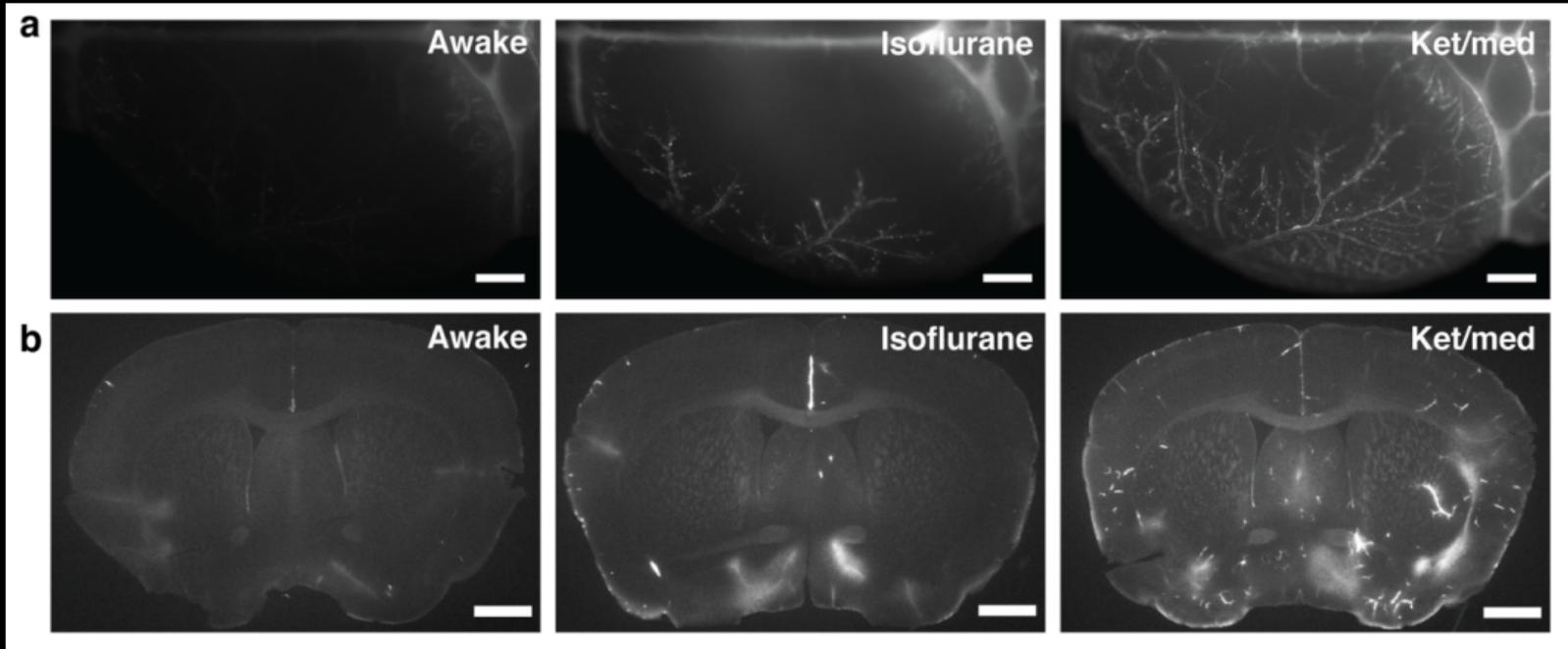
yielding the operator
 $-\text{div } \Sigma u$
 $\text{div } \Sigma u$
 $\frac{\partial}{\partial t}$
 $\frac{\partial}{\partial t}$
 $\frac{\partial}{\partial t}$
 Analysis in Ω_i



Lemma:

The bilinear form is symmetric

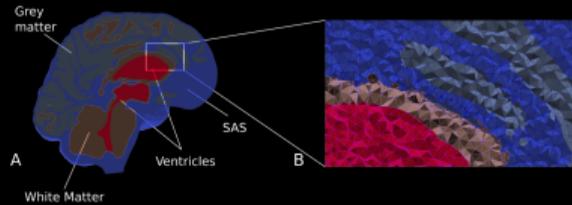
"Sleep" affects CSF outflux and tracer availability at brain surface



"...the spread of tracer to the PVS of the brain surface was directly related to the amount of tracer remaining at the basal cisterns and indirectly proportional to the amount that had reached the systemic blood."

Increased CSF production (as when awake) limits brain tracer influx

[Hornkjøl et al, CSF circulation and dispersion yield rapid clearance from intracranial compartments, Front. Bioeng. Biotechnol, 2022]



Given CSF production g , find the CSF **velocity** u and **pressure** p in Ω_F

$$\mu \nabla^2 u - \nabla p = 0,$$

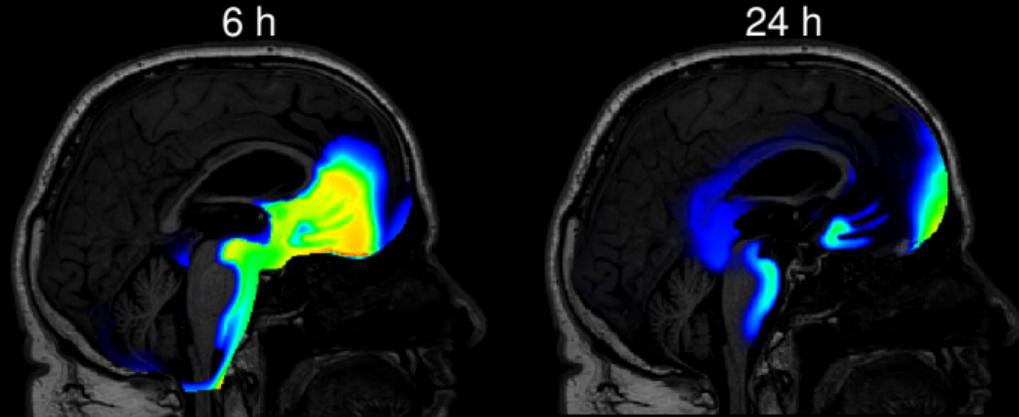
$$\nabla \cdot u = g,$$

with restricted outflux at $\partial\Omega_{\text{out}}$

$$\mu \nabla u \cdot n - pn = -R_0 u \cdot n,$$

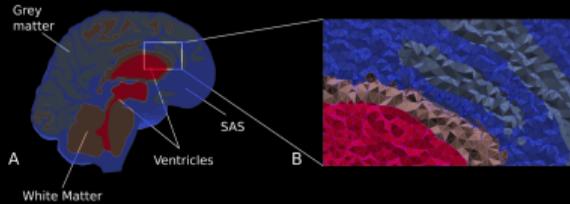
and the **concentration** c in $\Omega_F \cup \Omega_B$

$$\phi \frac{\partial c}{\partial t} + \phi u \cdot \nabla c - \nabla \cdot (\phi \alpha D \nabla c) = 0.$$



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[Hornkjøl et al, CSF circulation and dispersion yield rapid clearance from intracranial compartments, Front. Bioeng. Biotechnol, 2022]



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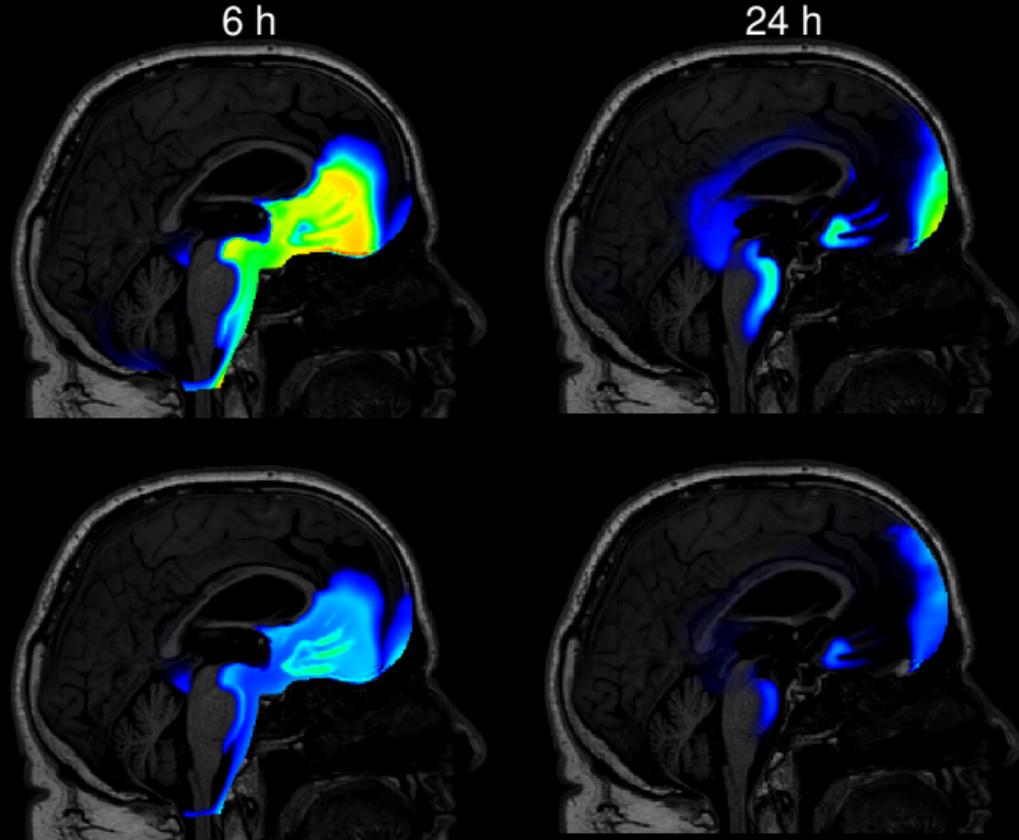
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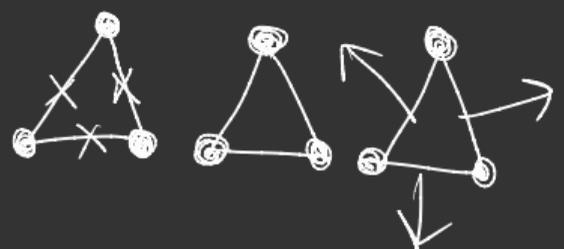
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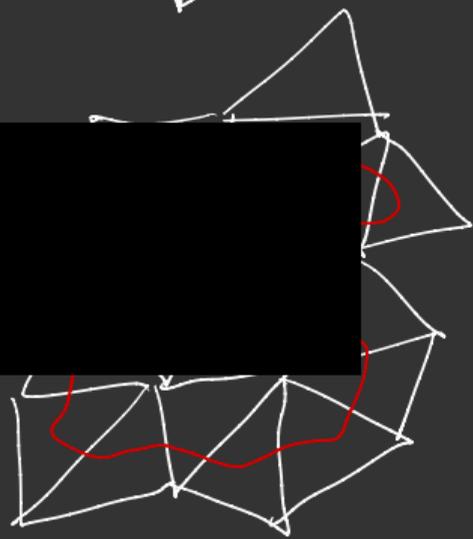
$\text{Curl } v = \pm \text{Im} \pm \text{ker}(v)$
 where Im are subject
 to modelling



$\text{div } u = \text{d.o.P}$
 Denote $\frac{\partial}{\partial t}$

IV. What are the modes of transport in the brain itself?

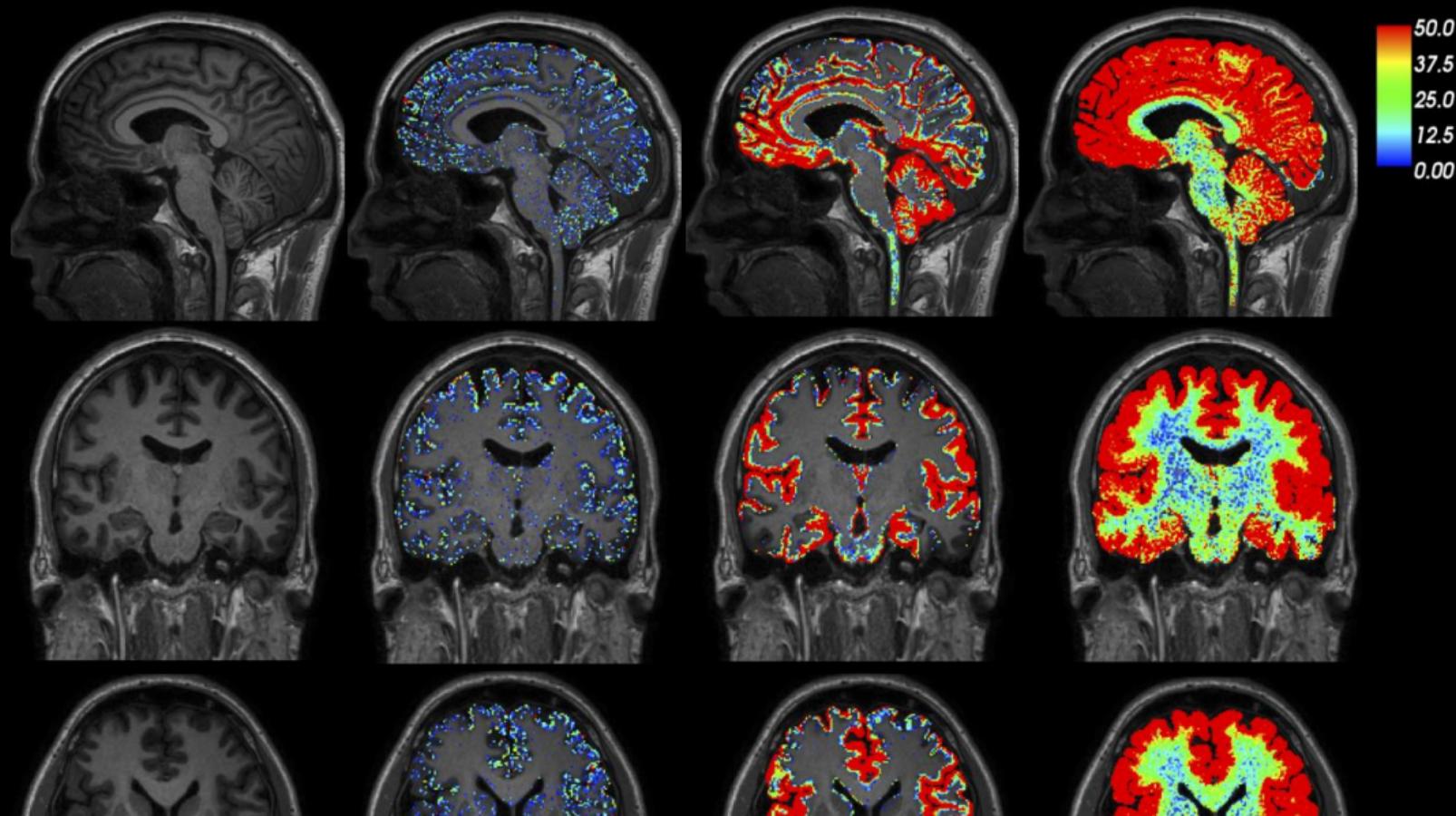
with $E =$
 yielding the operator
 $-\text{div } \nabla u$
 div
 $\frac{\partial}{\partial t}$
 $\frac{\partial}{\partial t}$
 $E + \frac{\partial}{\partial t}$
 The bilinear
 is sum



Lemma:

MRI reveals human brain-wide tracer enhancement and clearance

Ringstad et al. [2017, 2018]



Individualized finite element models of brain molecular transport and clearance

Vinje et al. [2023]



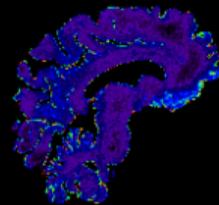
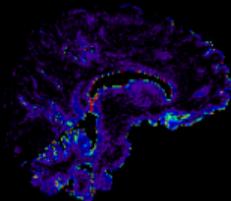
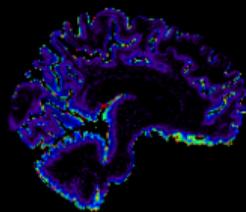
Find $c = c(x, t)$ for $x \in \Omega$,
 $t > 0$:

$$c_t - \operatorname{div} D \operatorname{grad} c = 0 \quad \text{in } \Omega$$
$$c = \mathcal{C}(I) \quad \text{on } \partial\Omega$$

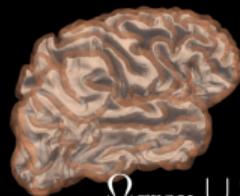
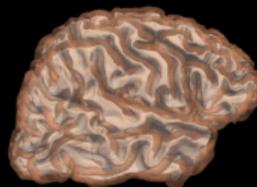
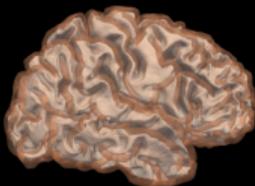
Continuous linear finite
elements

1 – 5M cells:

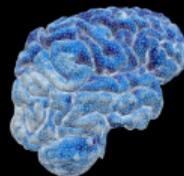
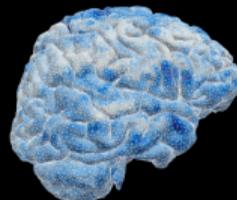
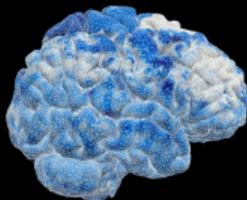
$h \approx 0.2 - 5.6\text{mm}$



$\mathcal{C}(I)$



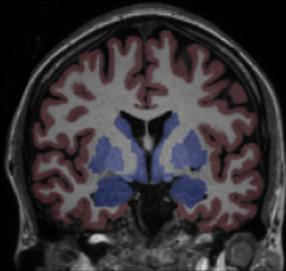
$\Omega_{\text{gray}} \cup \Omega_{\text{white}}$



$\operatorname{tr}(D)$

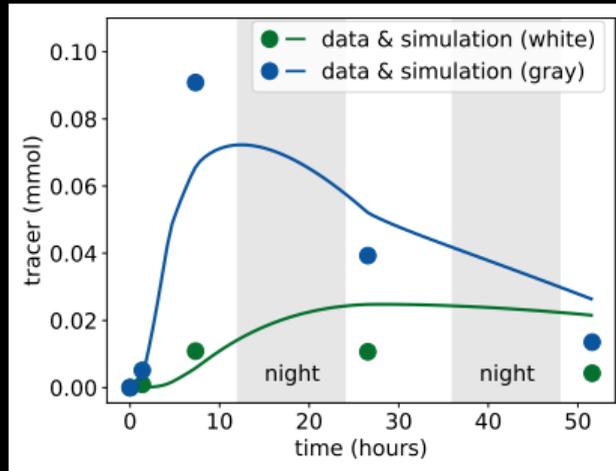
Transport by diffusion and dispersion underestimates molecular brain influx or clearance

Croci et al. [2019], Vinje et al. [2023]



$$\int_{\Omega_{\text{gray}}} c(x, t) dx$$

$$\int_{\Omega_{\text{white}}} c(x, t) dx$$

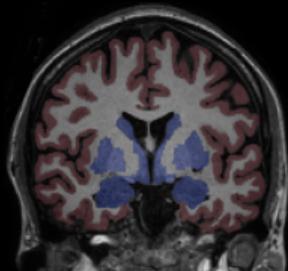


$$c_t - \text{div } D \text{ grad } c = 0$$

Iliff et al. [2012], Smith and Verkman [2019], Ray et al. [2019], Troyetsky et al. [2021], Ray et al. [2021], Hladky and Barrand [2022]

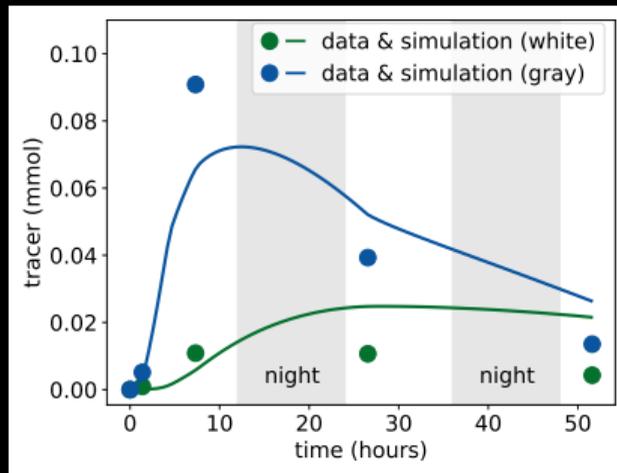
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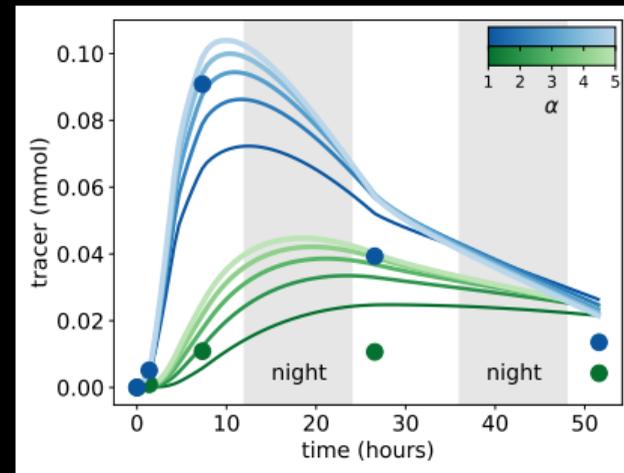


$$\int_{\Omega_{\text{gray}}} c(x, t) dx$$

$$\int_{\Omega_{\text{white}}} c(x, t) dx$$



$$c_t - \text{div } D \text{ grad } c = 0$$



$$c_t - \text{div } \alpha D \text{ grad } c = 0$$

Iliff et al. [2012], Smith and Verkman [2019], Ray et al. [2019], Troyetsky et al. [2021], Ray et al. [2021], Hladky and Barrand [2022]

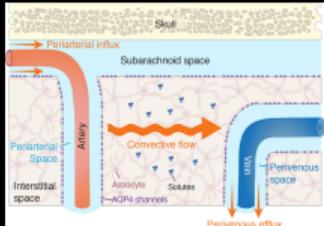
Is there a quantifiable (bulk) flow of interstitial fluid in brain tissue?



[Helen Cserr (credit: R. Cserr)]

Convection of cerebral interstitial fluid and its role in brain volume regulation

H F Cserr, M Depasquale, C S Patlak, R G Pullen



[Kwong et al (Fig 1, 2020)]

[Cserr et al (1986), Hladky and Barrand (2014), Smith et al (2017)]

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The role of brain barriers in fluid movement in the CNS: is there a 'glymphatic' system?

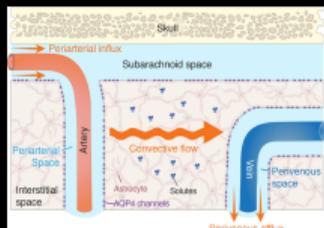
N. Joan Abbott [✉], Michelle E. Pizzo, Jane E. Preston, Damir Janigro & Robert G. Thorne [✉]

The Glymphatic System: A Novel Component of Fundamental Neurobiology

Lauren M. Hablitz and Maiken Nedergaard

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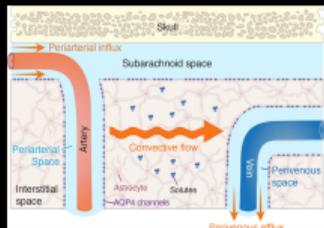


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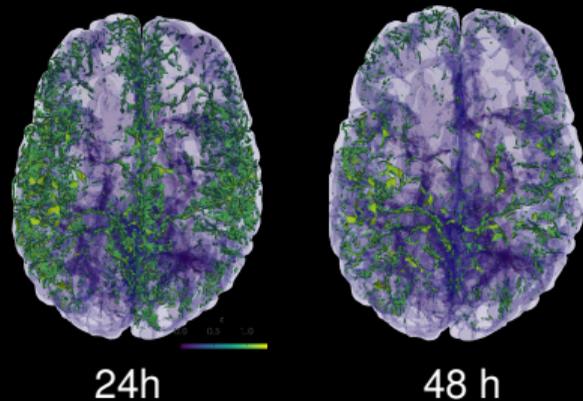
[Abbott et al (2018), Hablitz and Nedergaard (2021), ...]

With a velocity field $\phi : \Omega \rightarrow \mathbb{R}^d$, find $c : \Omega \times [0, T] \rightarrow \mathbb{R}$:

$$c_t + \operatorname{div}(c\phi) - \operatorname{div} D \operatorname{grad} c = 0 \quad \text{in } \Omega,$$

$$c = \mathcal{C}(I) \quad \text{on } \partial\Omega$$

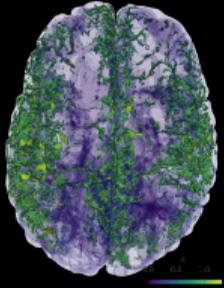
A few observations $\mathcal{C}(I)$ on Ω available



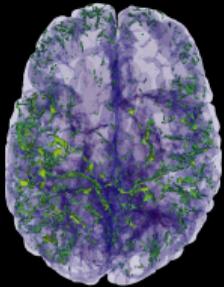
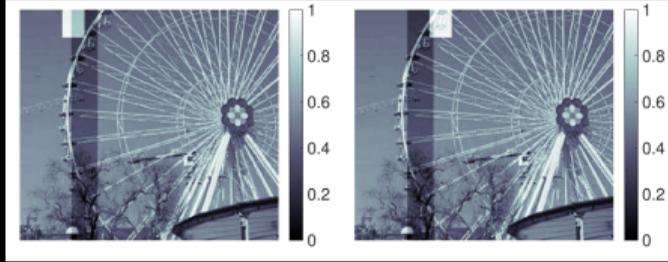
24h

48 h

Determining a fluid flow field from images via optical flow methods



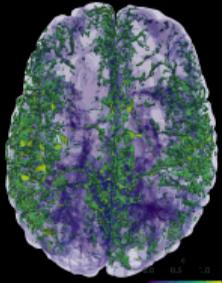
c_1 at t_1



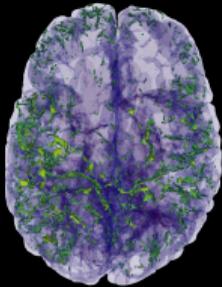
c_2 at t_2

$$\tau = t_2 - t_1$$

Determining a fluid flow field from images via optical flow methods

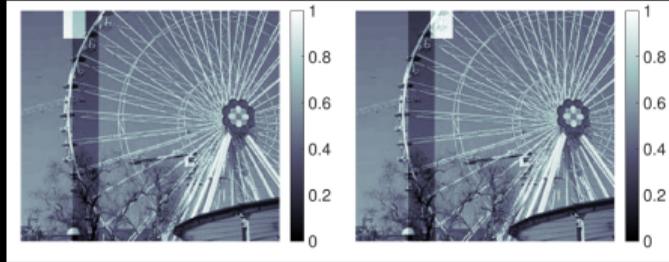


c_1 at t_1



c_2 at t_2

$$\tau = t_2 - t_1$$



Given $c_1, c_2 : \Omega \rightarrow \mathbb{R}$ at t_1, t_2 , $\alpha > 0$, and

$$f = c_t + \phi \cdot \text{grad } c,$$

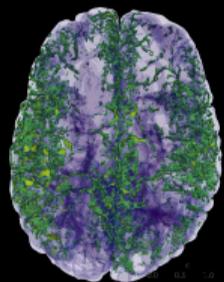
$$R = \|\text{grad } \phi\|_{L^2(\Omega)},$$

find an **optimal** $\phi \in H^1(\Omega; \mathbb{R}^d)$:

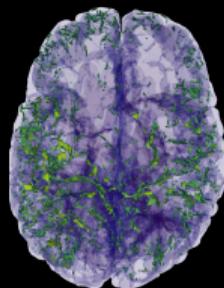
$$\min_{\phi} \int_{t_1}^{t_2} \int_{\Omega} f^2 \, dx \, dt + \alpha^2 R^2,$$

e.g. via the Euler-Lagrange equations.

Determining a fluid flow field from images via optical flow methods

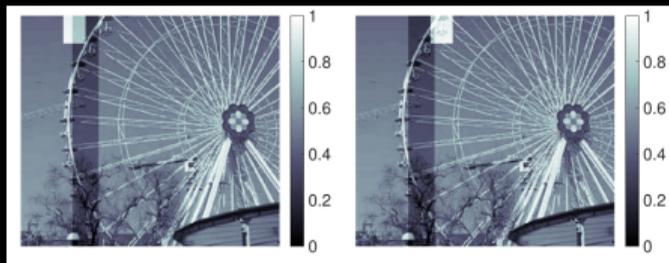


c_1 at t_1



c_2 at t_2

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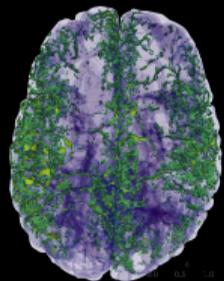
e.g. via the Euler-Lagrange equations.

Monge-Kantorovich mass transfer:

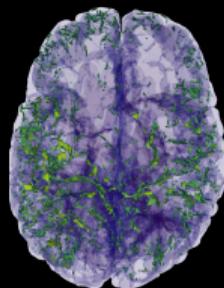
$$R = \|c\phi \cdot \phi\|_{L^1([t_1, t_2]) \times L^1(\Omega)}$$

[..., Benamou and Bernier (2000), Mueller et al (2013), ...]

Determining a fluid flow field from images via optical flow methods

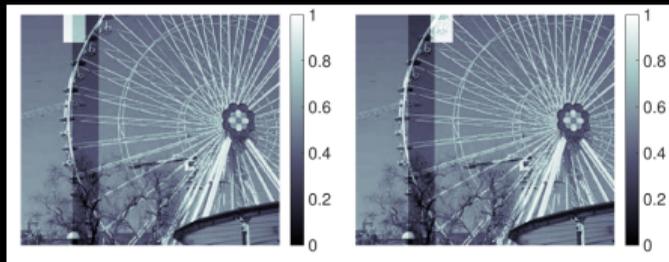


c_1 at t_1



c_2 at t_2

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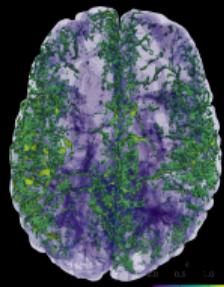
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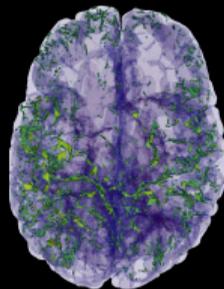
But not a viable approach here!

- ◇ Sensitive to regularization α
- ◇ Discrete derivatives of non-smooth data ($\nabla_h c_1$, $\Delta_h c_1$)
- ◇ Optical flow ignores diffusion

Recovering approximations of fluid flow fields accounting for diffusion



c_1 at t_1



c_2 at t_2

$$\tau = t_2 - t_1$$

Optimal Convection-Diffusion (OCD)

Given $c_1, c_2 : \Omega \rightarrow \mathbb{R}$ at t_1, t_2 , $\alpha > 0$,

optimize

$$\min_{c, \phi} \|c(t_2) - c_2\|_{L^2(\Omega)}^2 + \alpha^2 R^2,$$

subject to $c(t_1) = c_1$ and for $t \in (t_1, t_2]$:

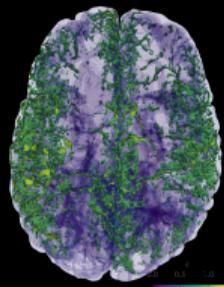
$$c_t + \operatorname{div}(c\phi) - \operatorname{div} D \operatorname{grad} c = 0. \quad (2)$$

[~ Andreev et al (2015), Glowinski et al (2022)]

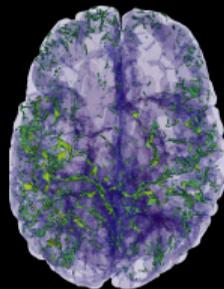
Let $c_t \approx \delta_\tau c \equiv \frac{1}{\tau}(c - c_1)$

[Alnaes et al (2015), Farrell et al (2013), Vinje et al (2023)]

Recovering approximations of fluid flow fields accounting for diffusion



c_1 at t_1



c_2 at t_2

$$\tau = t_2 - t_1$$

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[~ Andreev et al (2015), Glowinski et al (2022)]

Let $c_t \approx \delta_\tau c \equiv \frac{1}{\tau}(c - c_1)$

Iterative optimization approach

Define the reduced functional

$$J : H(\operatorname{div}, \Omega) \rightarrow \mathbb{R}$$

$$J(\phi) = \|c(\phi)(t_2) - c_2\|_{L^2(\Omega)}^2 + \alpha^2 R^2$$

where $\phi \mapsto c(\phi)$ by c solving (2).

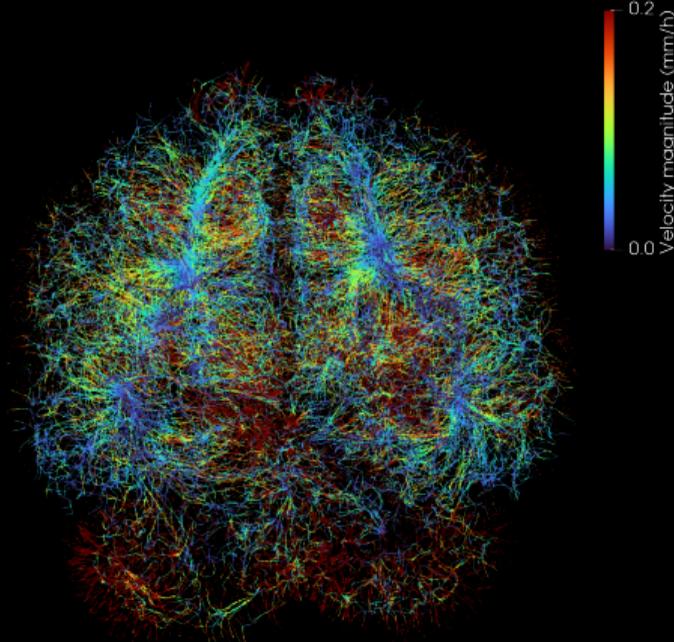
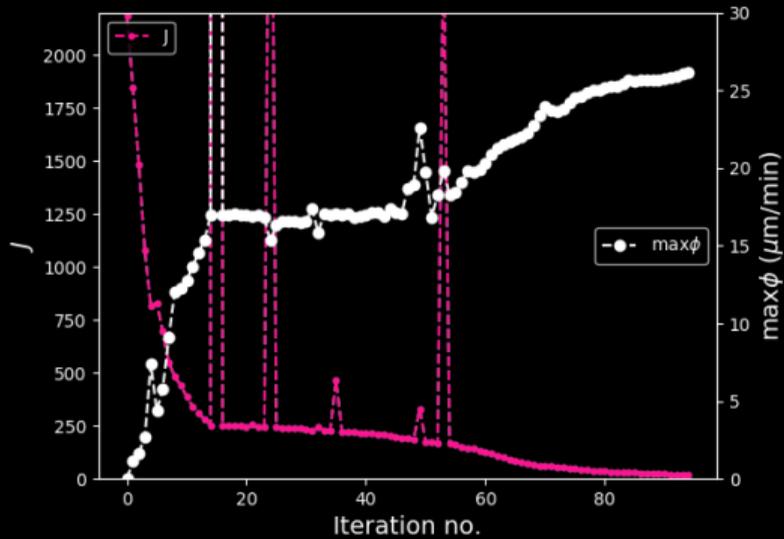
Solve

$$\min_{\phi} J(\phi)$$

via e.g. scipy (L-BFGS), FEniCS, Dolfin-adjoint.

[Alnæs et al (2015), Farrell et al (2013), Vinje et al (2023)]

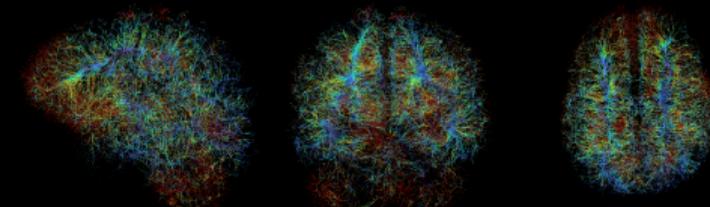
OCD approach yields robust approximation of average velocities



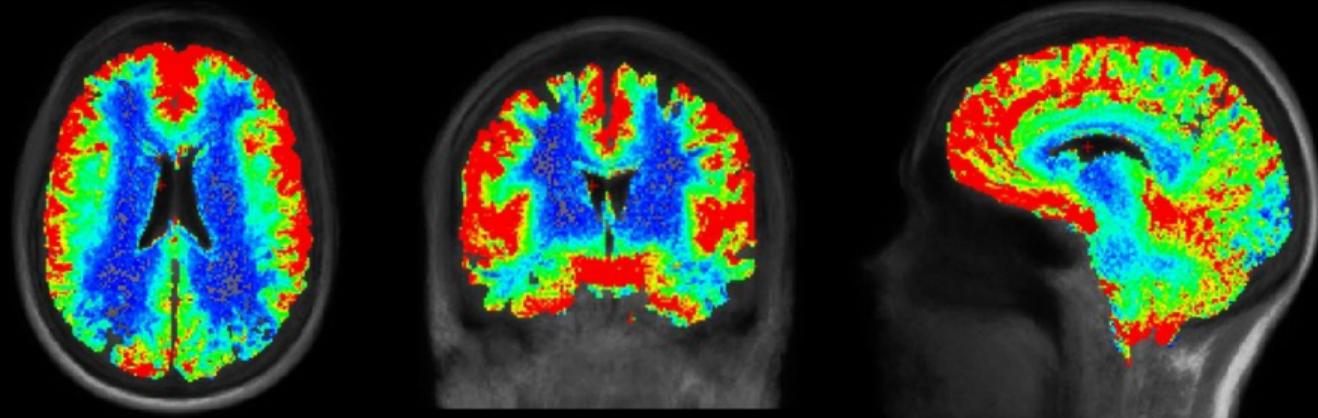
Average speed $\bar{\phi} = \frac{1}{|\Omega|} \int_{\Omega} |\phi| dx$ ($\mu\text{m}/\text{min}$):

[Vinje et al (2023)]

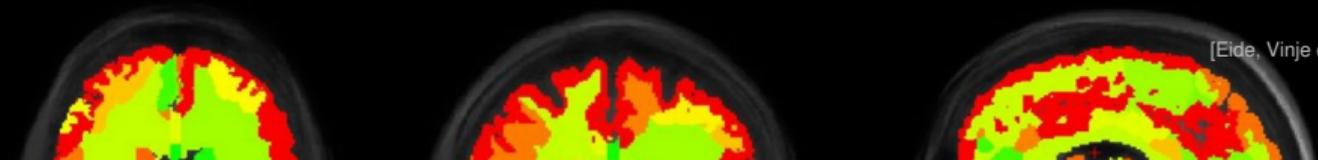
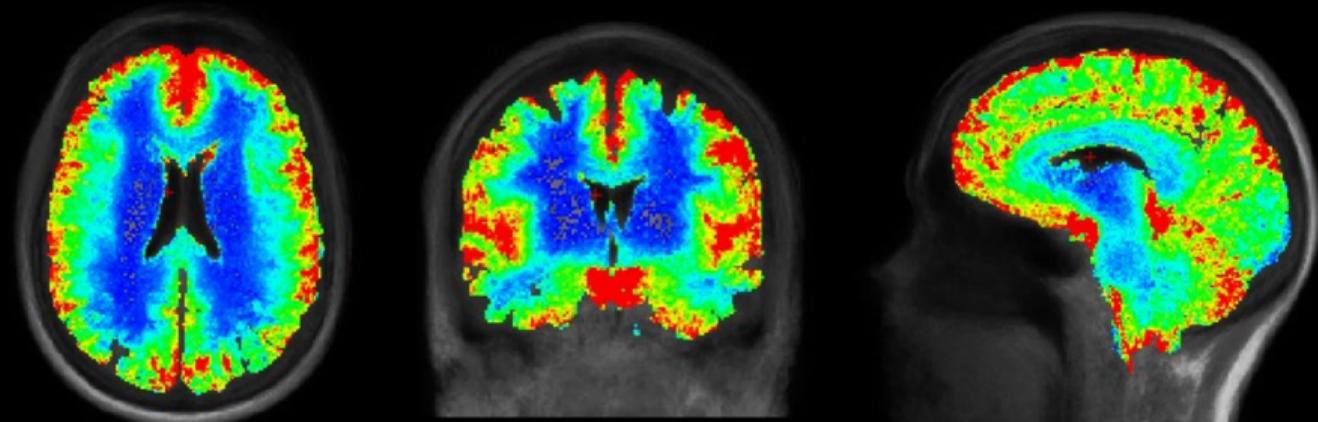
n vs. α^2	10^{-3}	10^{-4}	10^{-5}
16	2.83	3.67	4.00
32	2.33	2.83	2.83



A
Deprivation



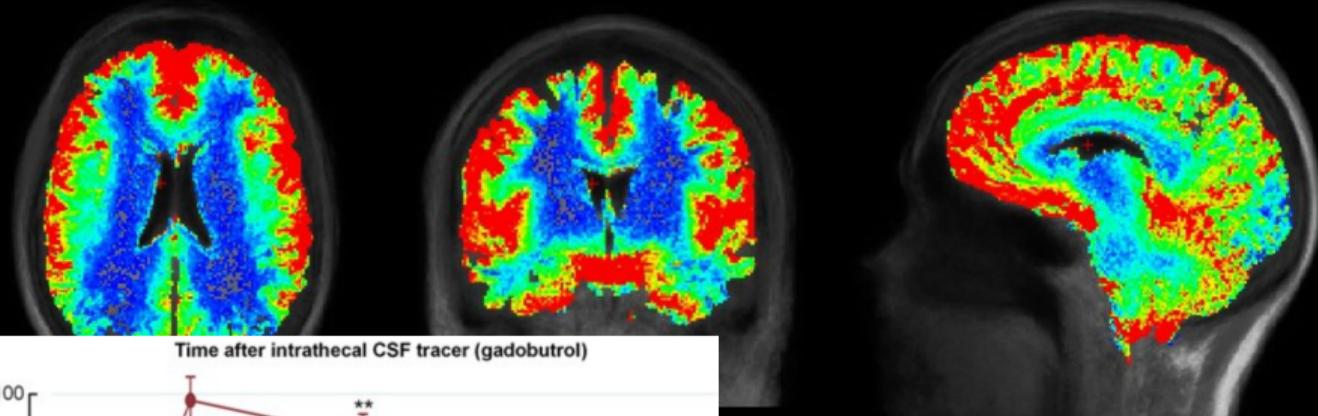
B
Sleep



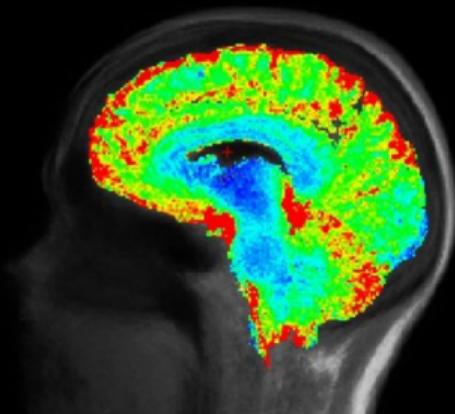
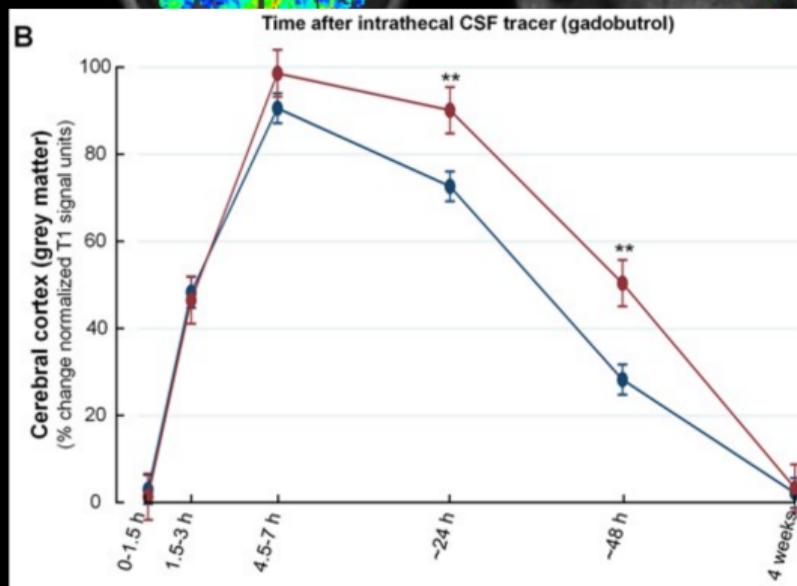
[Eide, Vinje et al (2021)]



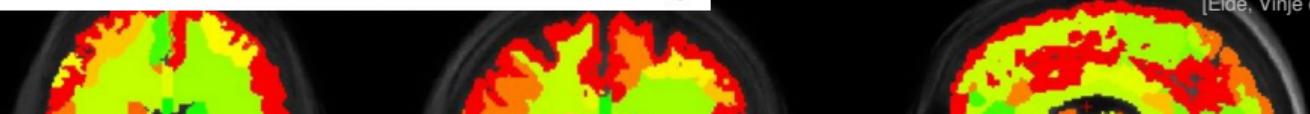
A
Deprivation



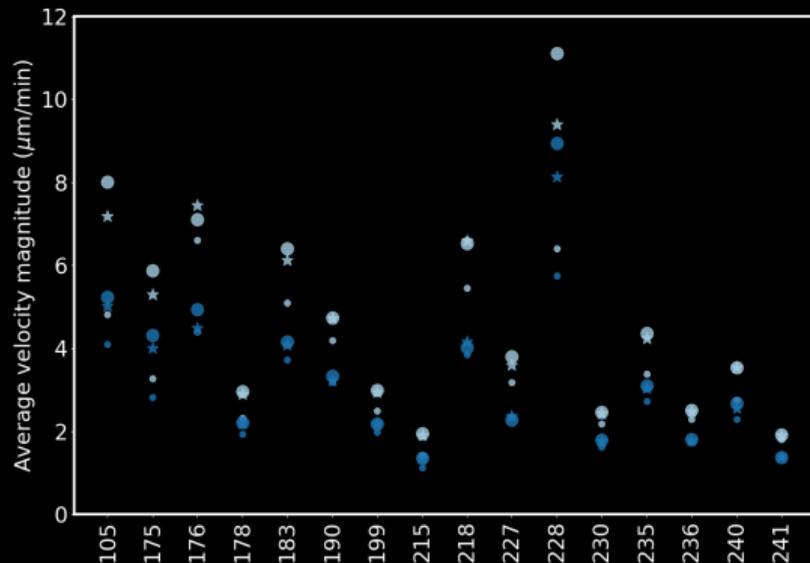
B
Sleep



[Eide, Vinje et al (2021)]



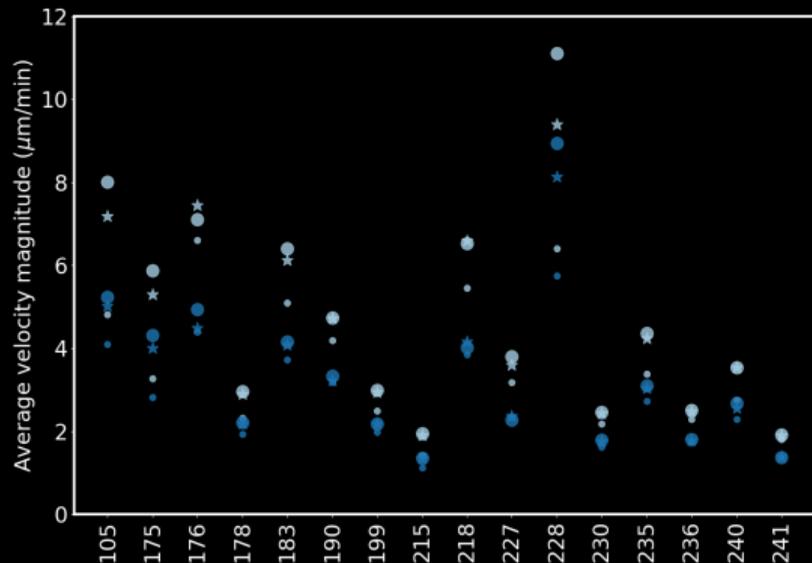
Estimate ϕ between 24h and 48h images for each patient.



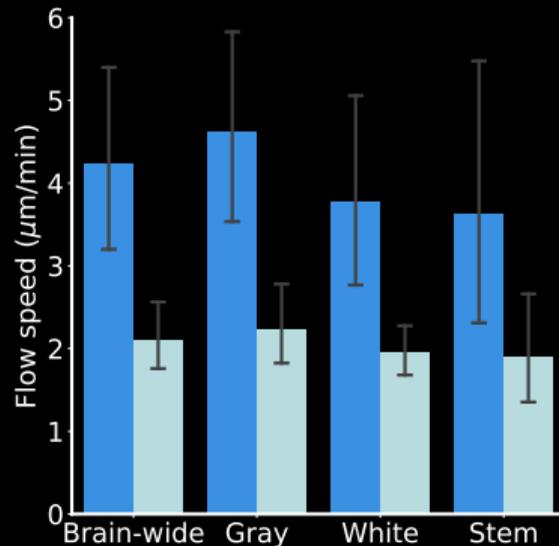
Average flow speed $\bar{\phi}$ for $\alpha^2 = 10^{-3}$ (dots), 10^{-4} (stars), 10^{-5} (circles) for low-res (light blue) and standard meshes (blue).

Convective velocities are reduced (by x2) after sleep-deprivation

Estimate ϕ between 24h and 48h images for each patient.



Average flow speed $\bar{\phi}$ for $\alpha^2 = 10^{-3}$ (dots), 10^{-4} (stars), 10^{-5} (circles) for low-res (light blue) and standard meshes (blue).

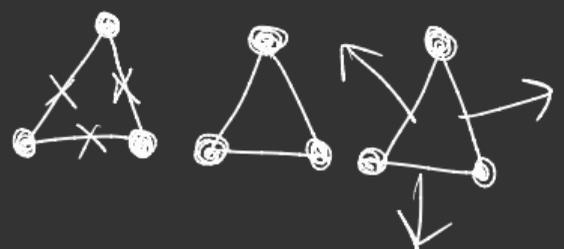


N = 11 + 7

4.23 vs. 2.11 $\mu\text{m}/\text{min}$ ($p=0.0057$)



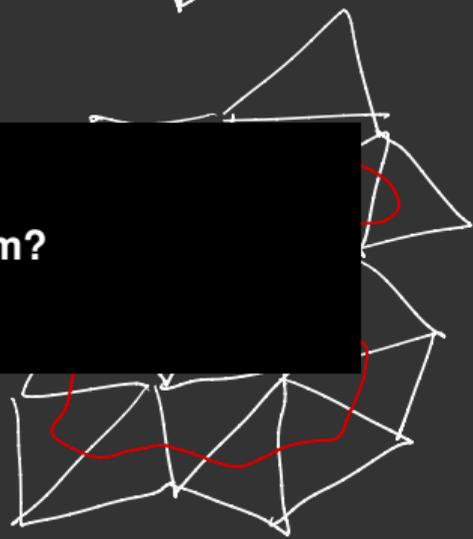
$C_m v = \pm I_m \pm \text{kon}(v)$
 where I_m are subject to modelling



Denote $\frac{\partial}{\partial t}$
 $\text{div } u - \alpha \cdot p$
 Poisson

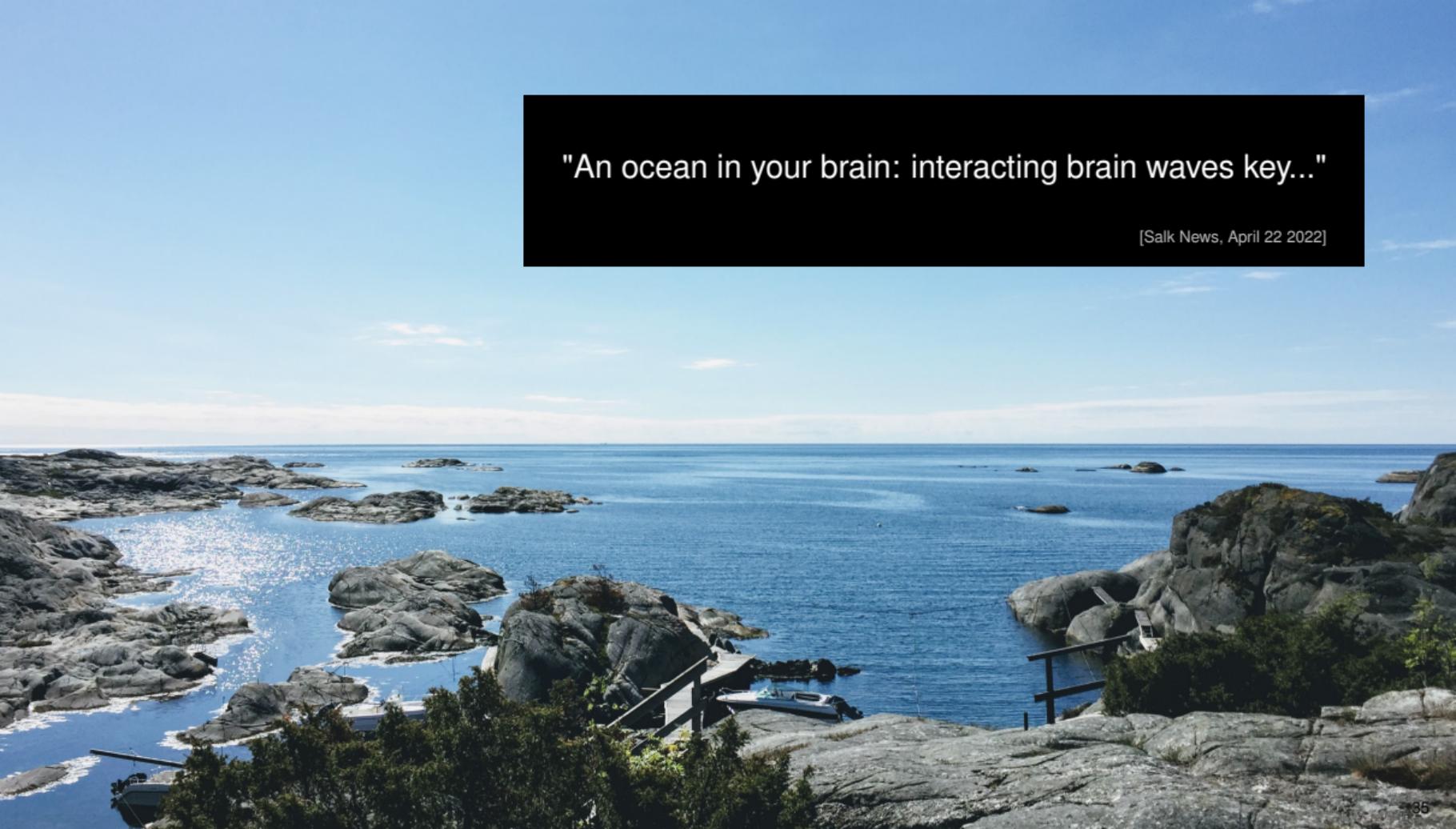
VI. Where does that flow on the order of $\mu\text{m}/\text{min}$ come from?

yielding the operator
 $-\text{div } \Sigma u$
 $\text{div } \Sigma u$
 $\frac{\partial}{\partial t}$
 $\frac{\partial}{\partial t}$
 $\frac{\partial}{\partial t}$
 Analysis in Ω_i



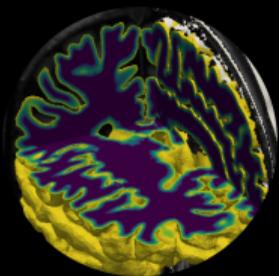
Lemma:

The bilinear form is symmetric

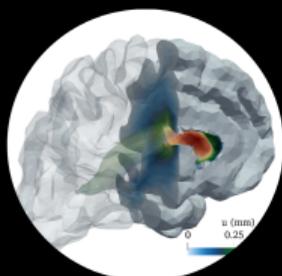


"An ocean in your brain: interacting brain waves key..."

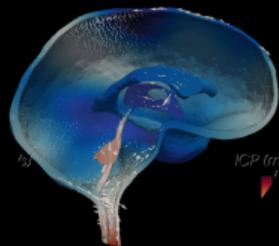
[Salk News, April 22 2022]



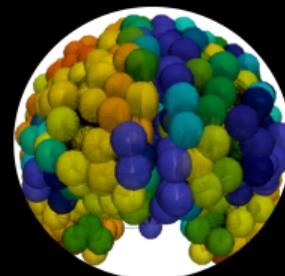
Solute transport and clearance



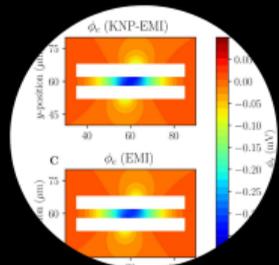
Brain mechanics



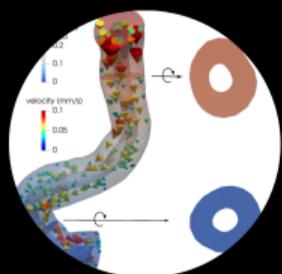
Cerebrospinal fluid flow and pulsatility



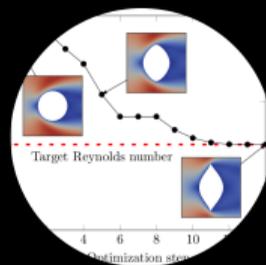
Neurodegeneration



Ions and osmosis



Mixed-dimensional PDEs

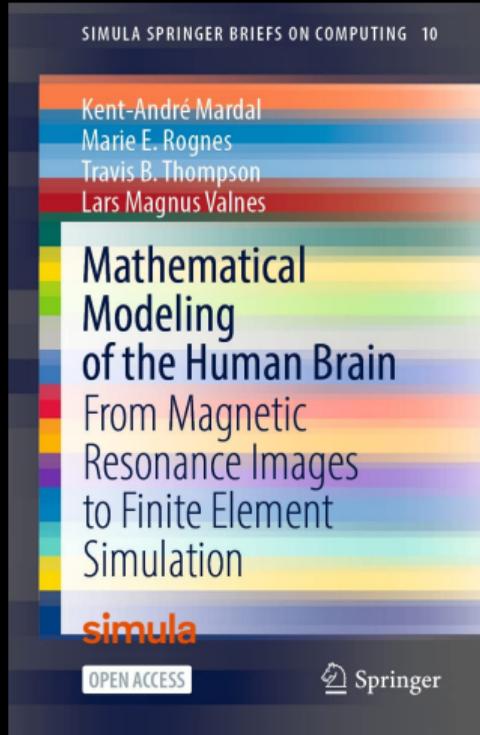


Optimization



Simulation technology

Mathematical modeling of the human brain: from MRI to FEM



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<https://link.springer.com/book/10.1007/978-3-030-95136-8>

[<https://github.com/kent-and/mri2fem>]

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Core message

Mathematical models can give new insight into medicine, – and the human brain gives an extraordinary rich setting for mathematics and numerics!

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