

Fluid-structure interaction problems in the cardiovascular system

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INSTITUT NATIONAL
DE RECHERCHE
EN INFORMATIQUE
ET EN AUTOMATIQUE

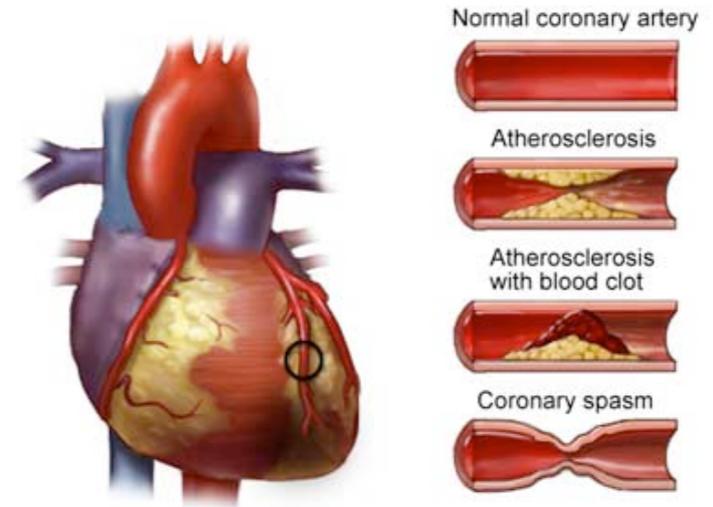


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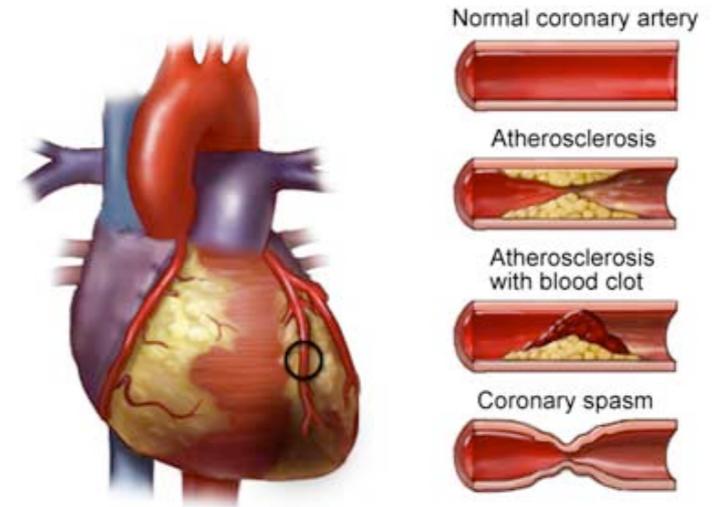
Cardiovascular system modelling ???

- **Blood flows** and **arteries** are much more complicated than what will be presented in this talk !

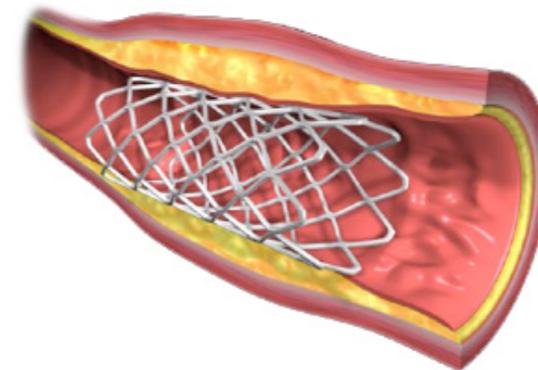


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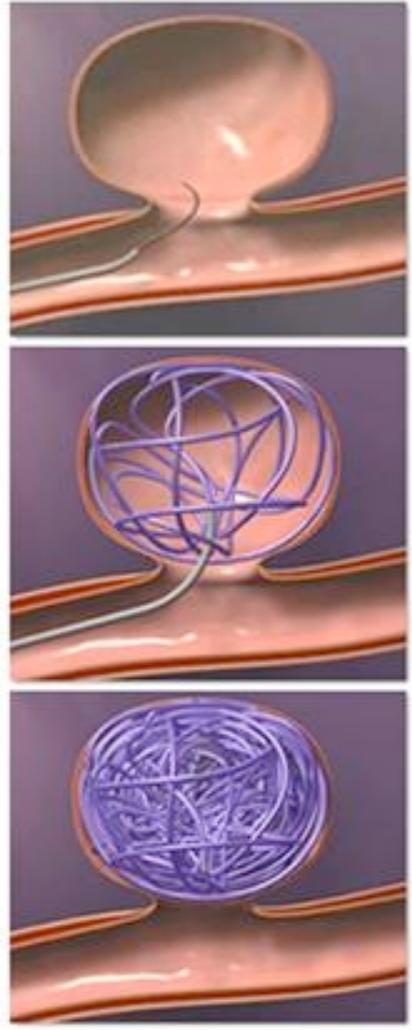
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- Nevertheless : even with simplified models, mathematical modelling may help to improve some therapies or medical devices

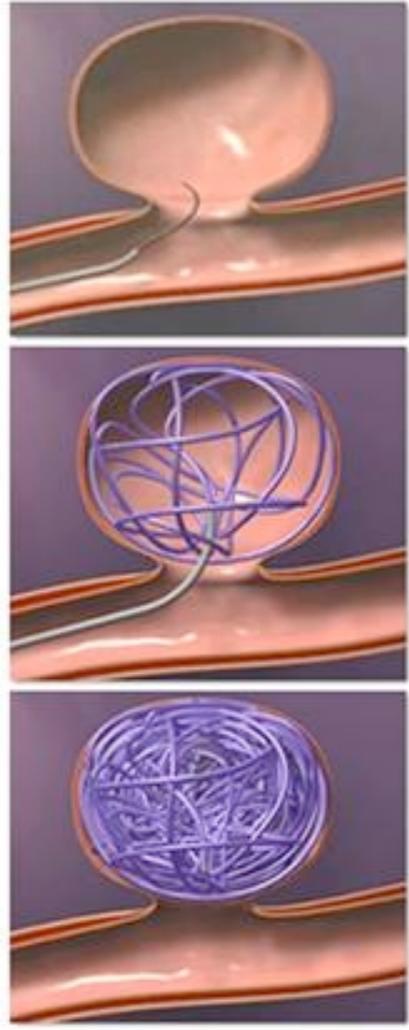


Ex 1: Stents and aneurisms



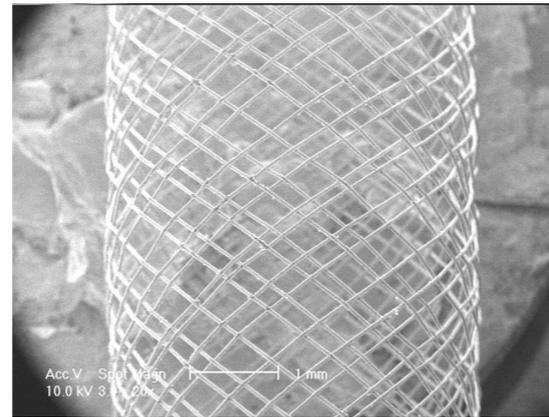
Coils

Ex I: Stents and aneurysms



Coils

Cardiatis stent

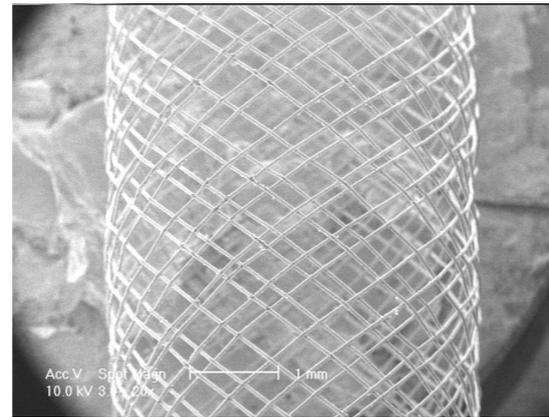


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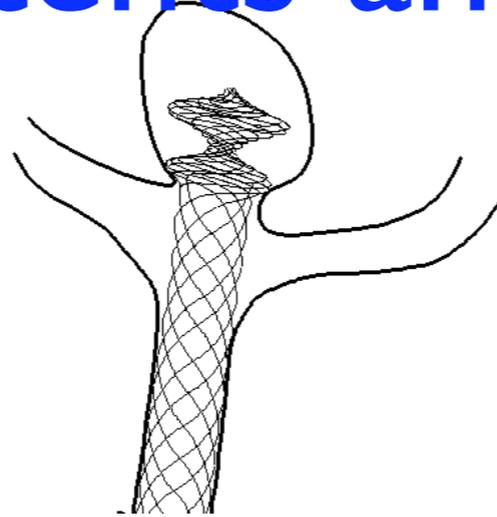


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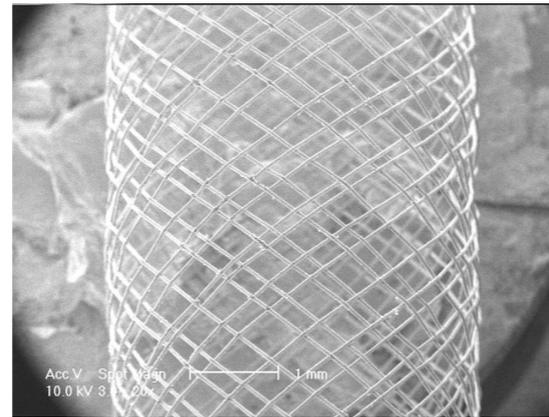
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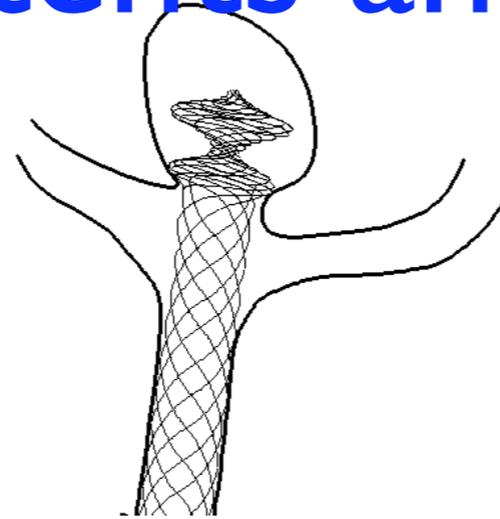


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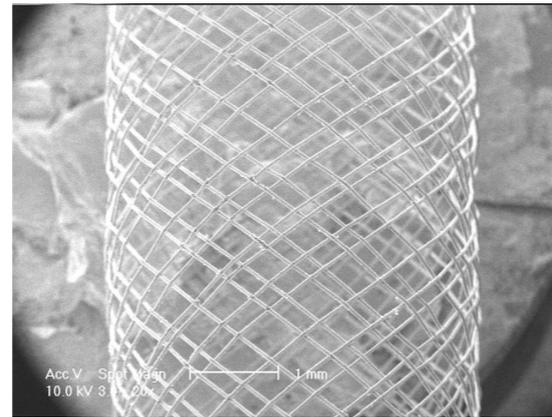
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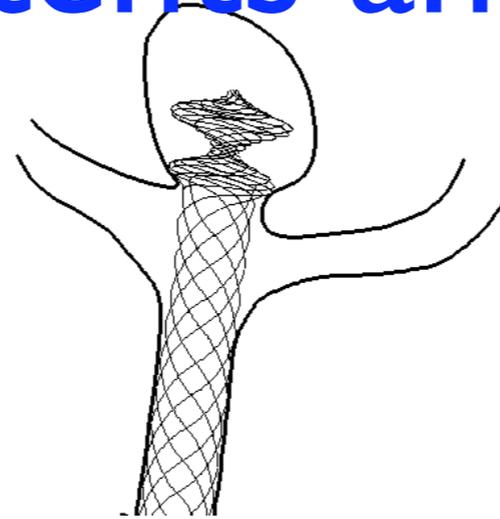


In vivo experiments
(Cardiatix /INRA)

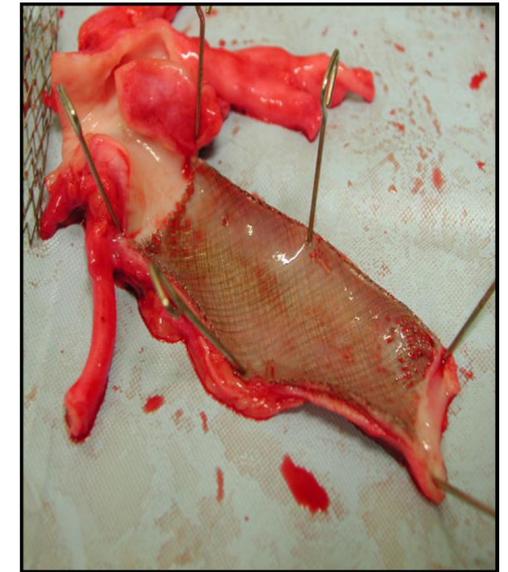
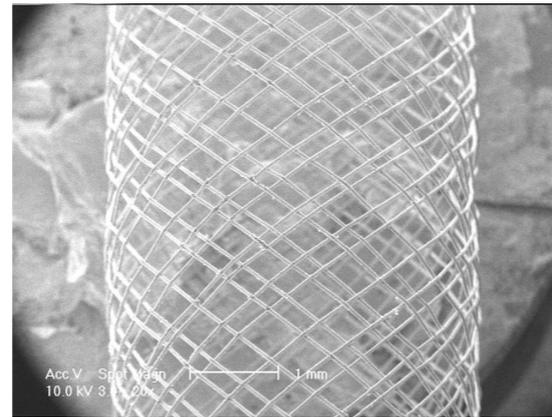
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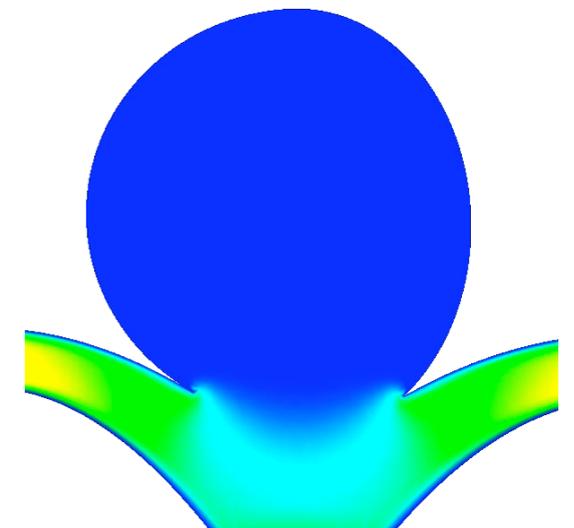
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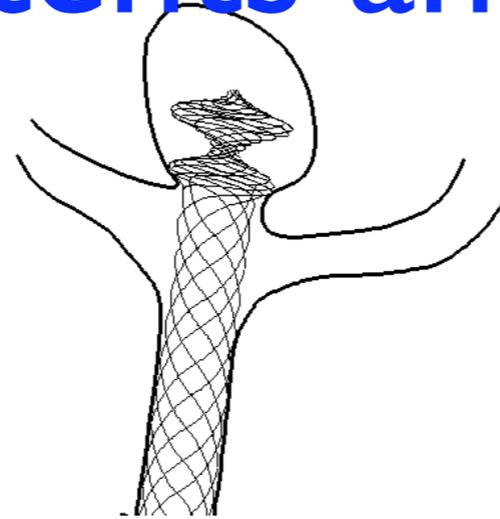


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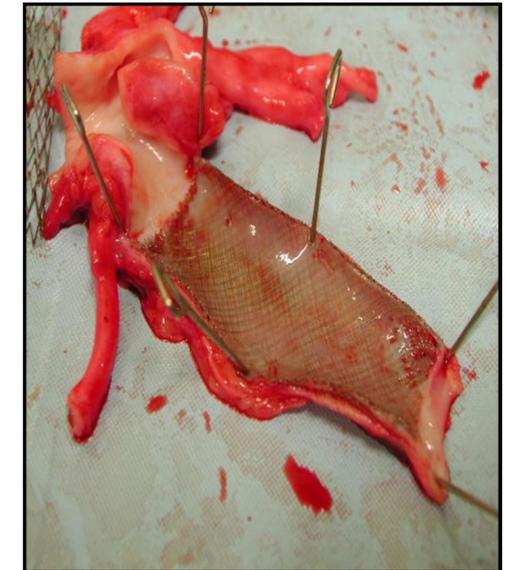
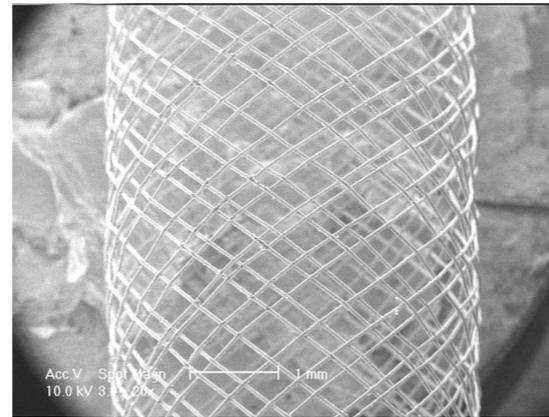
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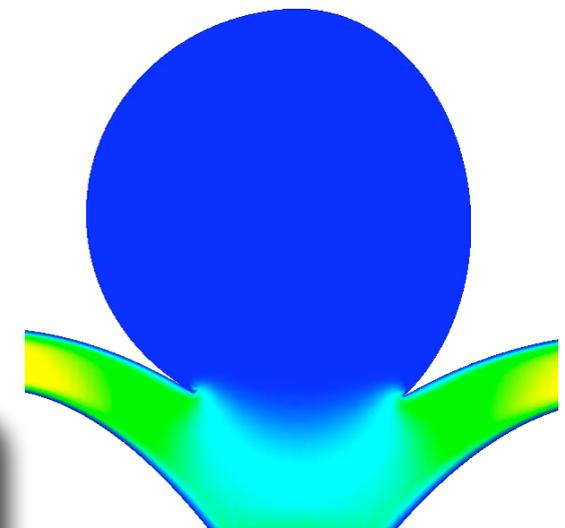
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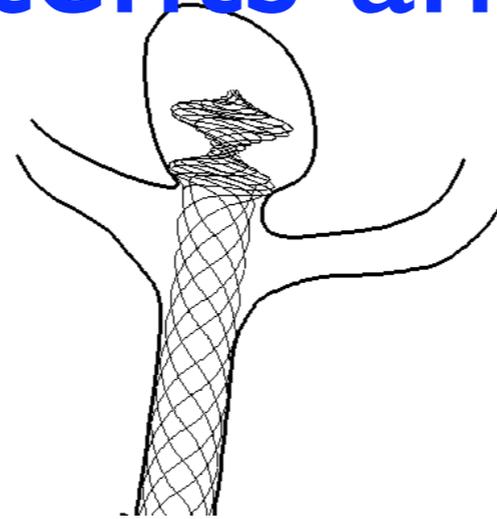
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- stent permeability/colateral arteries blood

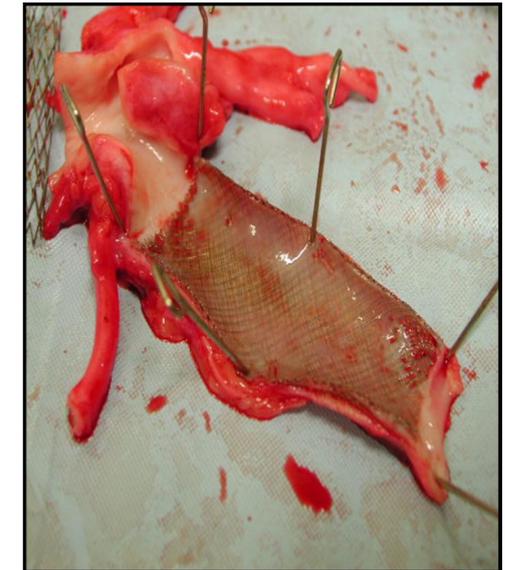
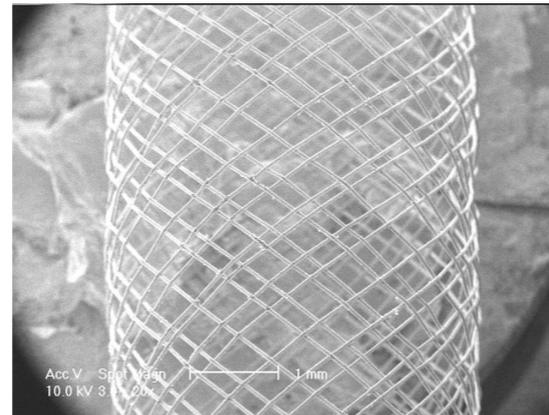
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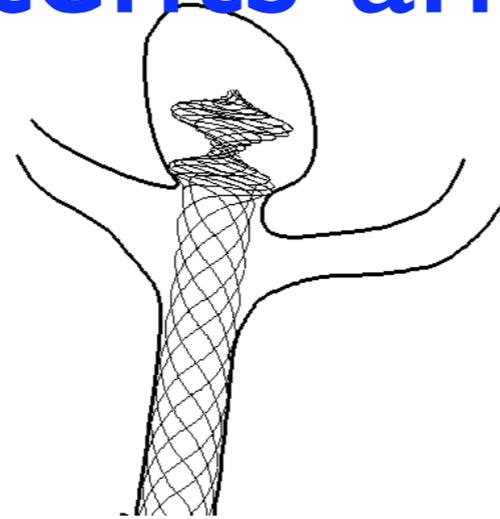
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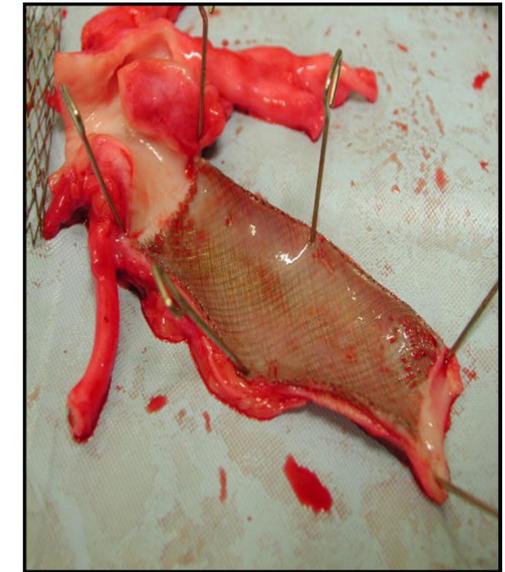
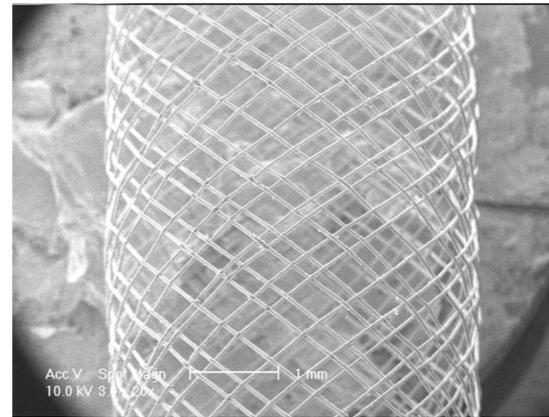
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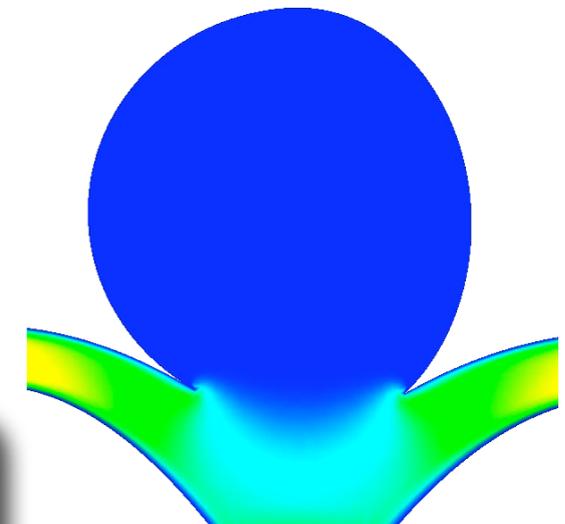
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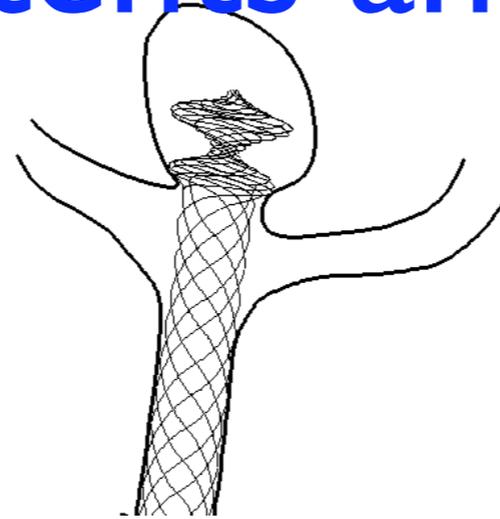
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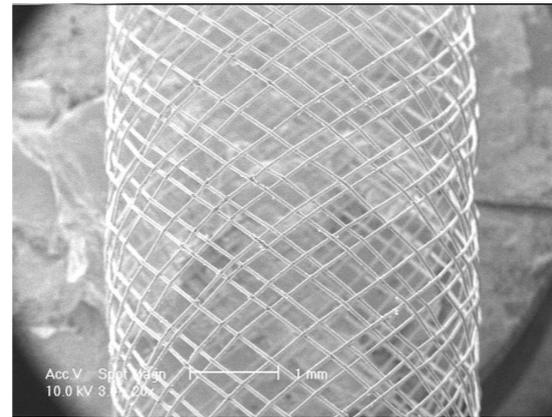
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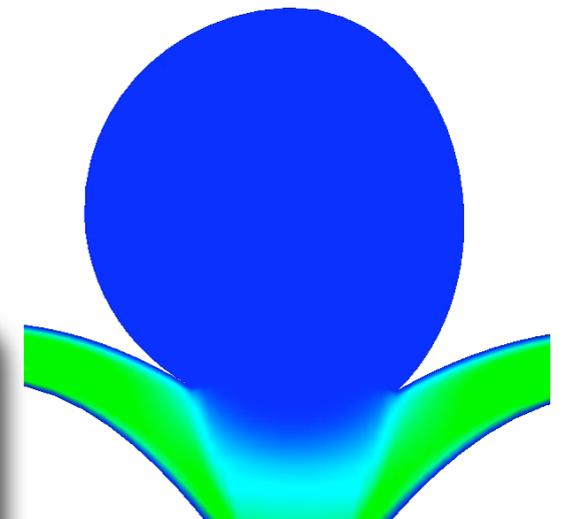
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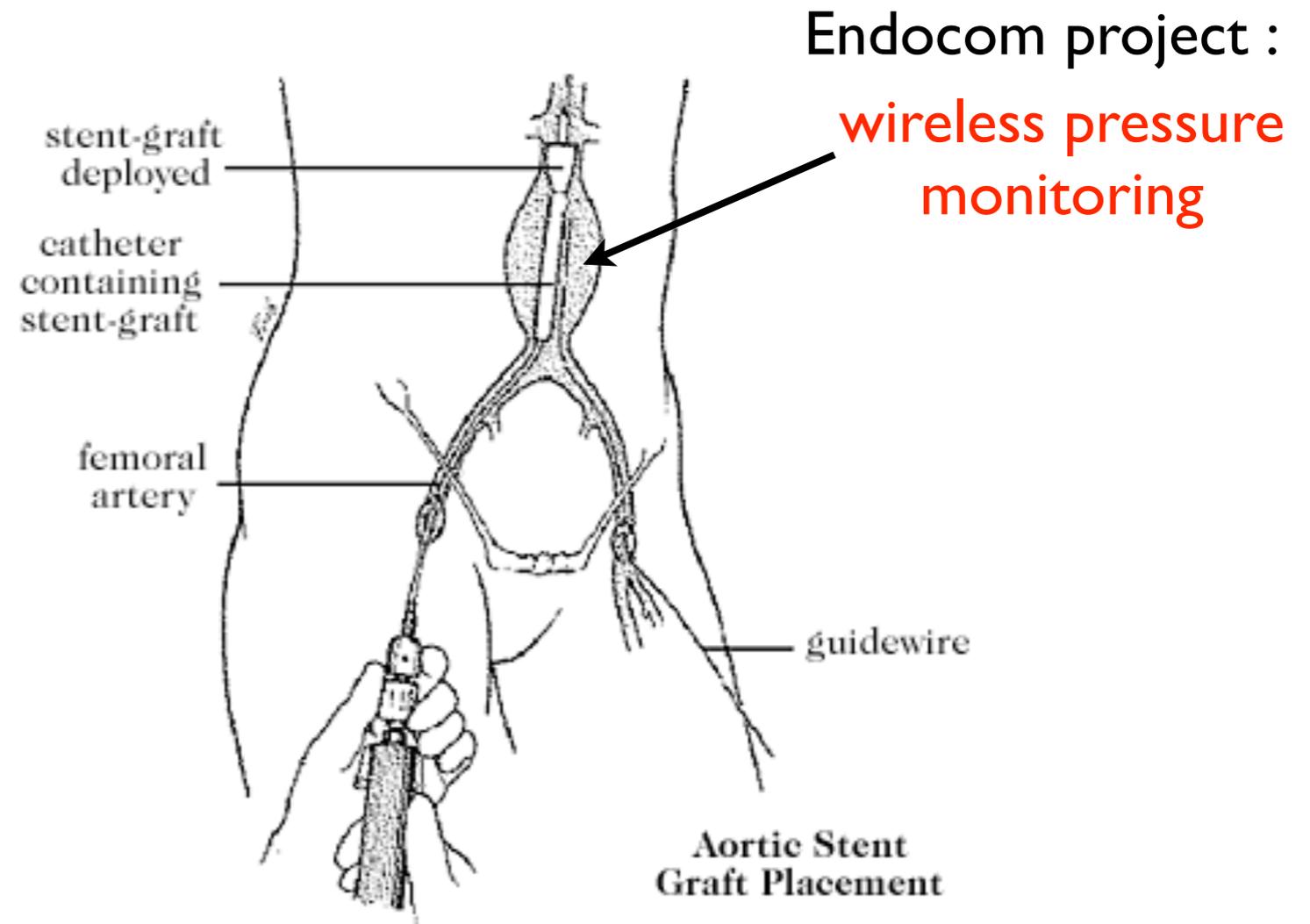
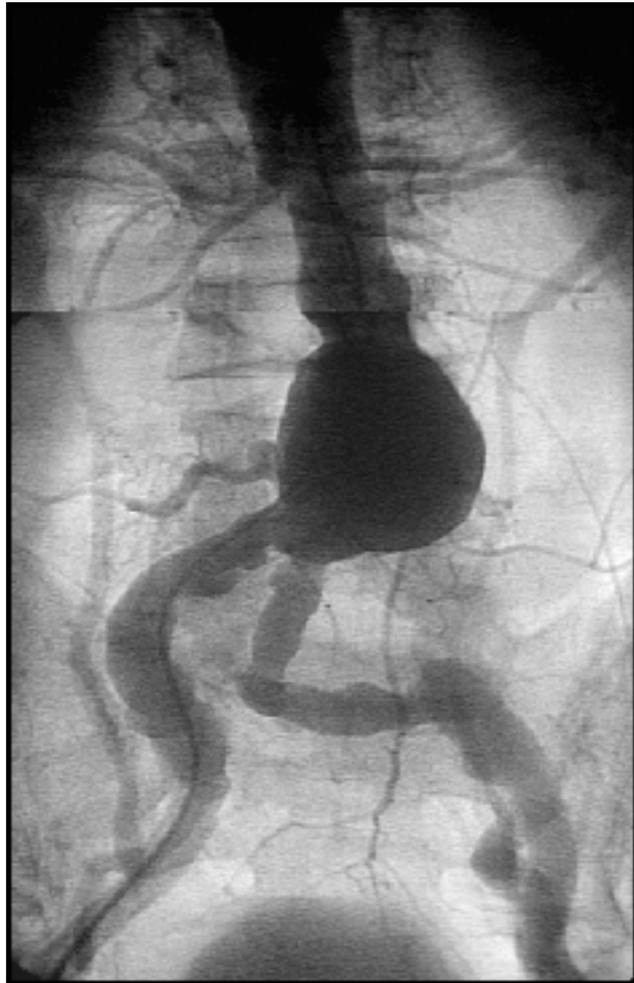
« In silico » experiment
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With stent

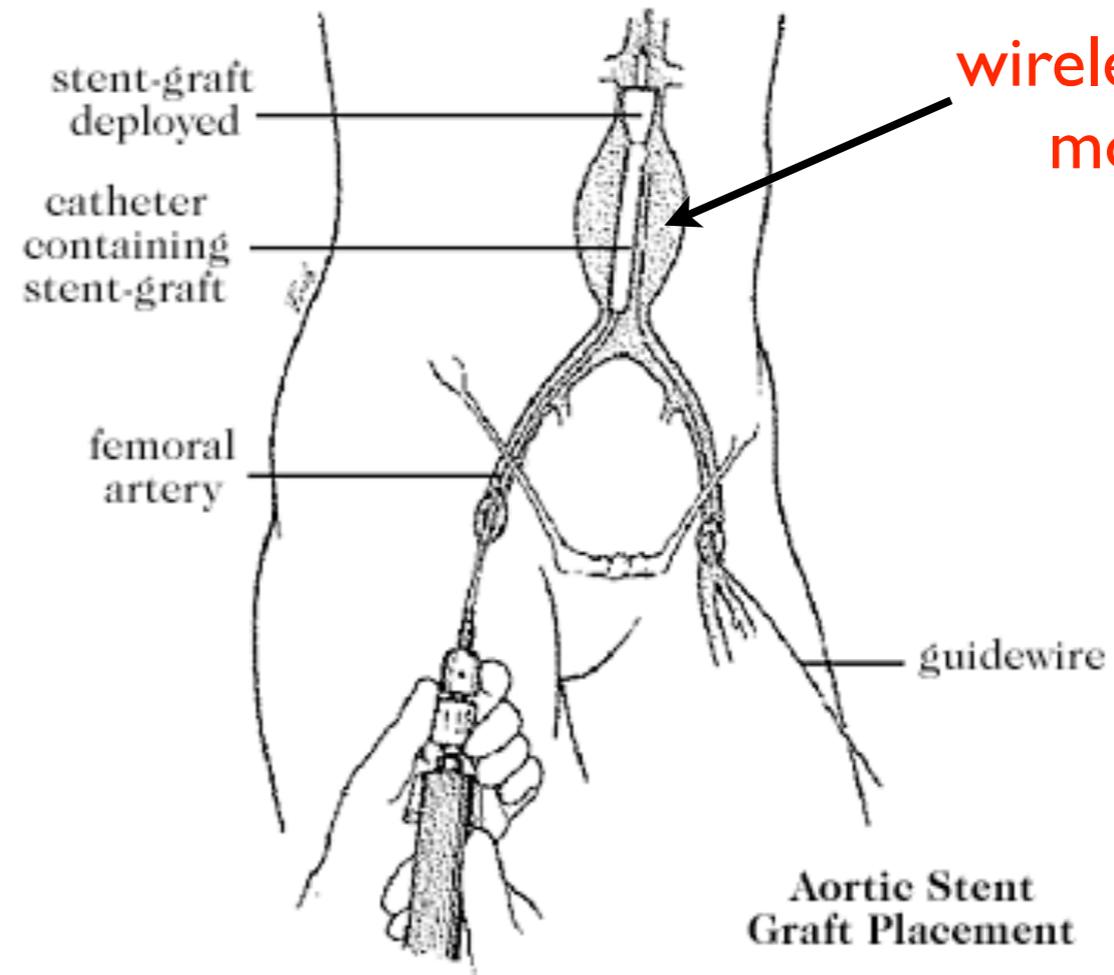
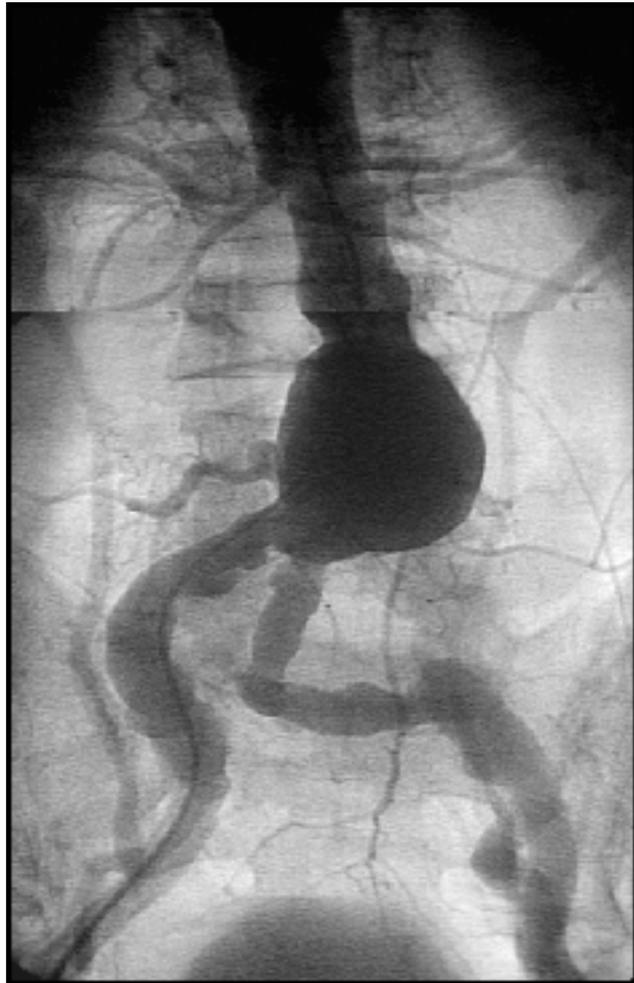
Numerical simulation:

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Ex 2: Abdominal Aortic Aneurysm



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Endocom project :

wireless pressure monitoring

Numerical simulation:

- optimal position of the sensor

Focus of this talk : fluid-structure interaction

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- **Challenging problems** for scientific computing :
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Focus of this talk : fluid-structure interaction

- **Fluid-structure interaction** : interaction with vessel, heart muscle, valves, *etc.*
- **Challenging problems** for scientific computing :
 - Efficiency & stability
 - Moving domain: geometrical non-linearities, topological change (contact)
 - Boundary conditions

Outline

- Fluid-structure interaction in arteries
 - Stability issues - Strongly couple schemes
 - A stable weakly coupled scheme
- Fluid-structure interaction with valves
 - Fictitious domain method
 - FSI and Contact management

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Fluid-structure interaction in arteries



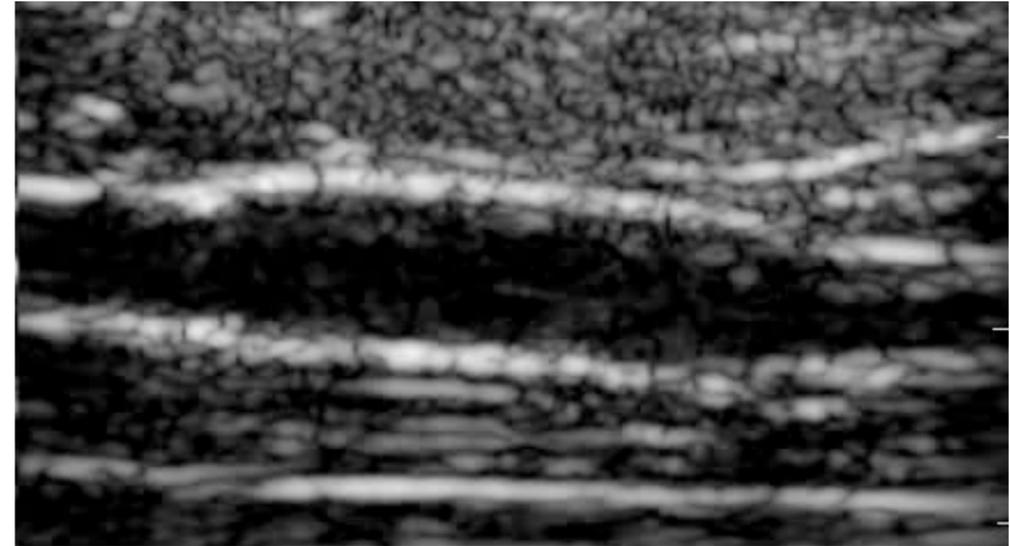
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Fluid-structure interaction in arteries



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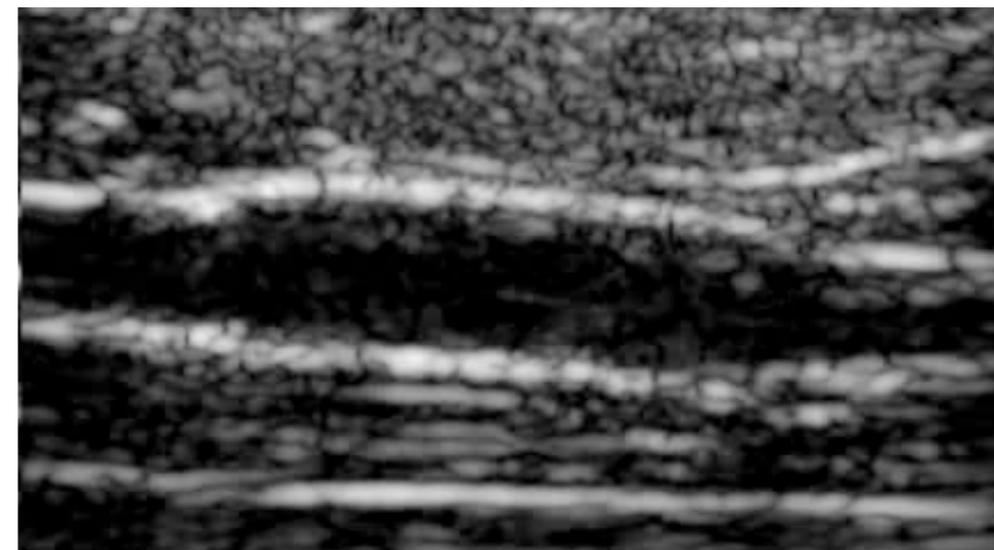


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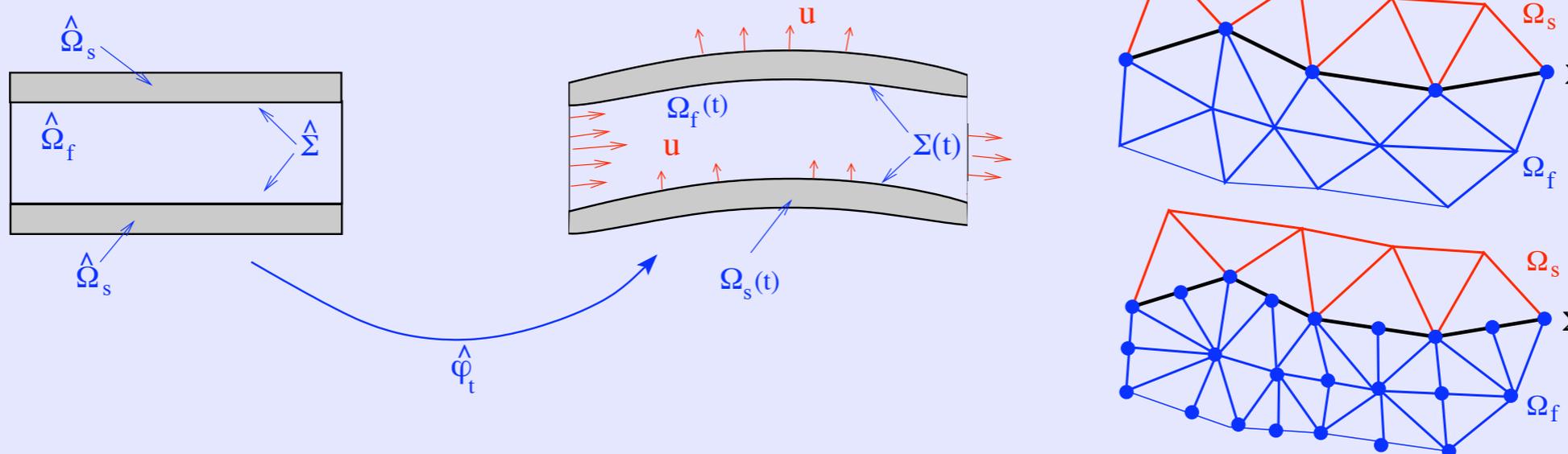


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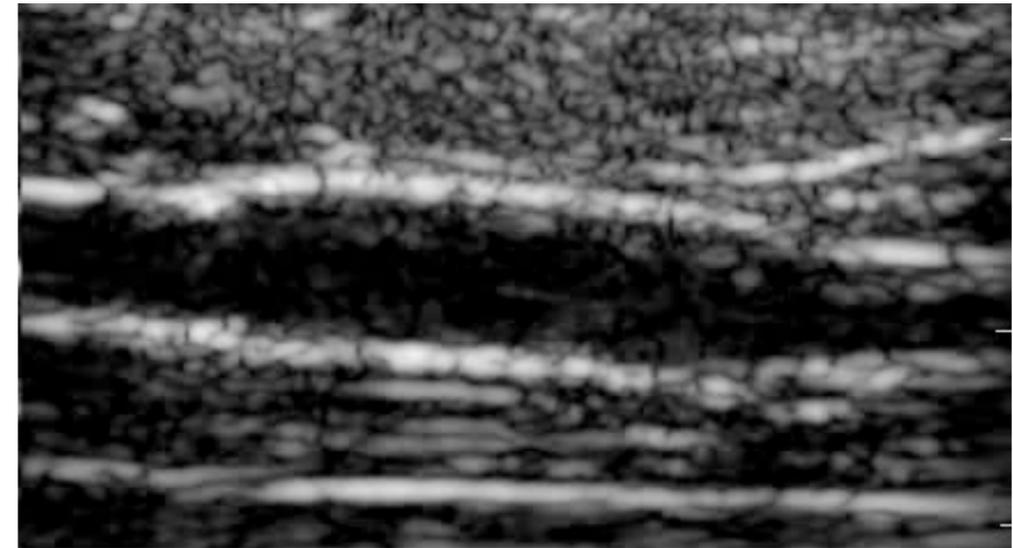
Wall : Arbitrary Lagrangian Eulerian (ALE)



Fluid-structure interaction in arteries

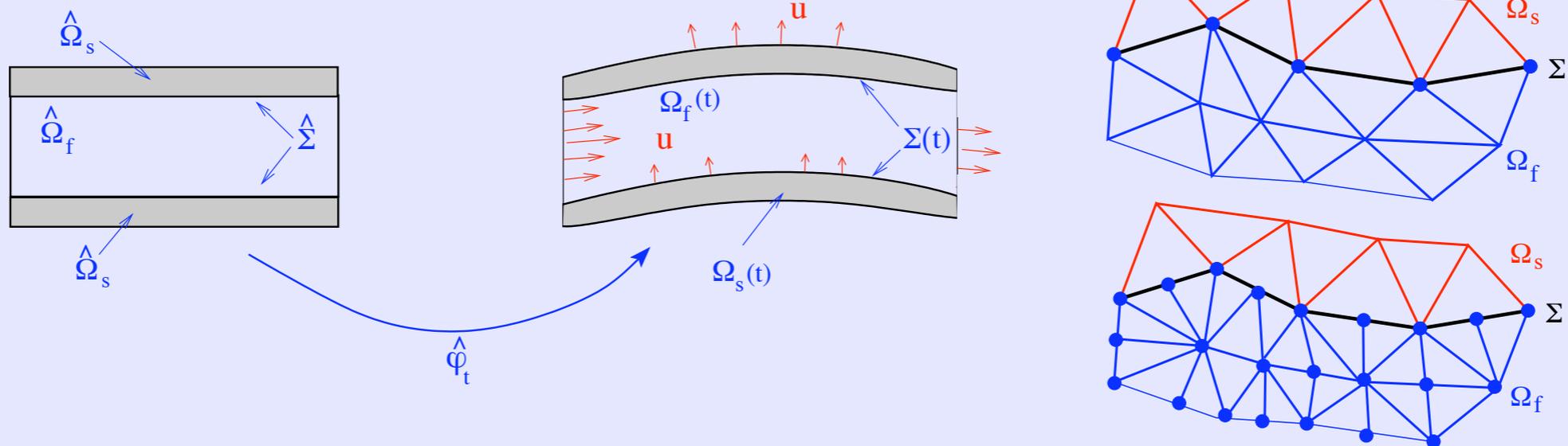


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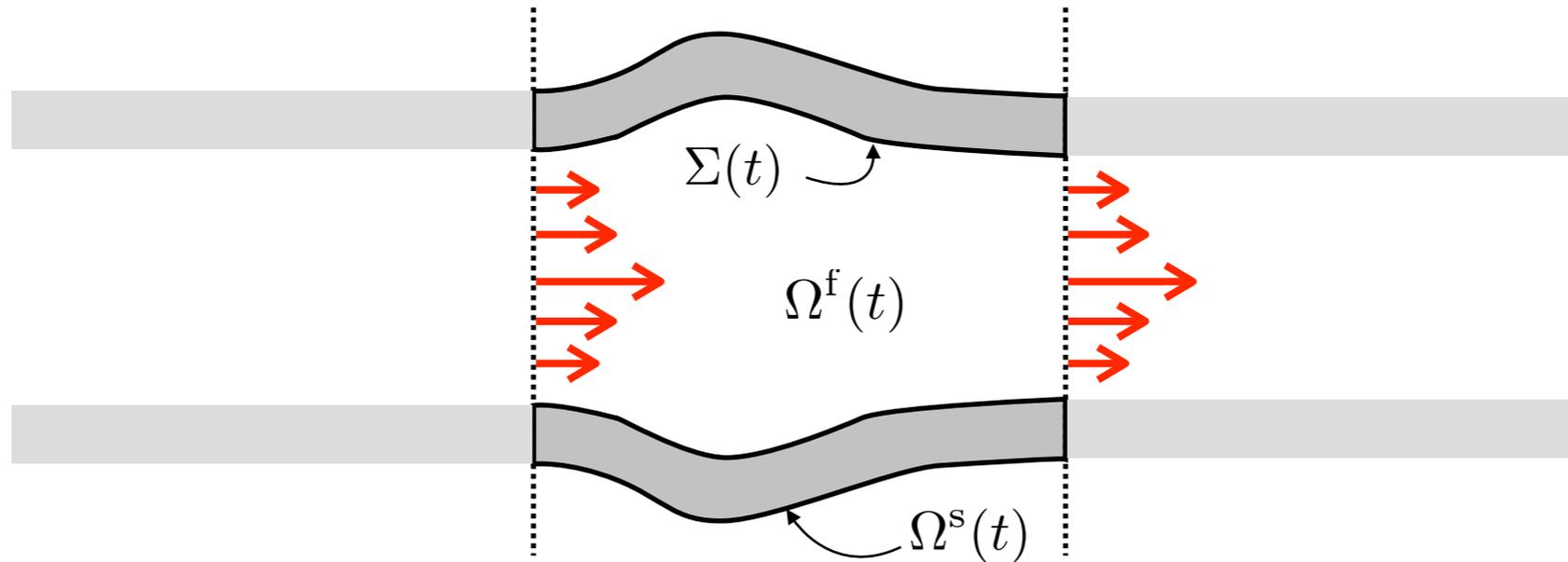


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Wall : Arbitrary Lagrangian Eulerian (ALE)



Geometrical description



$\Omega^f(t)$: **moving fluid domain** (filled with a viscous fluid : blood)

$\Omega^s(t)$: **solid current** configuration (artery wall)

$\Sigma(t)$: **fluid-solid interface**, where we enforce

- continuity of velocity
- continuity of stress

The fluid-structure problem:

Determine $\Omega^f(t)$, velocity and stress within the fluid and solid

The coupled problem

- Fluid equations:

$$\rho^f \left(\frac{\partial \mathbf{u}}{\partial t} \Big|_{\hat{\mathbf{x}}} + (\mathbf{u} - \mathbf{w}) \cdot \nabla \mathbf{u} \right) - 2\mu \operatorname{div} \epsilon(\mathbf{u}) + \nabla p = \mathbf{0}, \quad \text{in } \Omega^f(t)$$

$$\operatorname{div} \mathbf{u} = 0, \quad \text{in } \Omega^f(t)$$

$$\boldsymbol{\sigma}(\mathbf{u}, p) \mathbf{n} = \mathbf{g}, \quad \text{on } \Gamma_N^f$$

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- Solid equations:

$$\rho^s \frac{\partial^2 \mathbf{d}}{\partial t^2} - \operatorname{div}(\mathbf{F}(\mathbf{d}) \mathbf{S}(\mathbf{d})) = \mathbf{0}, \quad \text{in } \hat{\Omega}^s$$

$$\mathbf{d} = \mathbf{0}, \quad \text{on } \hat{\Gamma}_D^s$$

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- Coupling conditions:

$$\mathbf{d}^f = \operatorname{Ext}(\mathbf{d}|_{\hat{\Sigma}}), \quad \mathbf{w}(\mathbf{d}^f) = \frac{\partial \mathbf{d}^f}{\partial t} \quad \text{in } \hat{\Omega}^f, \quad \Omega^f(t) = (I + \mathbf{d}^f)(\hat{\Omega}^f), \quad (\text{geometry})$$

$$\mathbf{u} = \mathbf{w}(\mathbf{d}^f), \quad \text{on } \Sigma(t), \quad (\text{velocity})$$

$$\mathbf{F}(\mathbf{d}) \mathbf{S}(\mathbf{d}) \hat{\mathbf{n}} = J(\mathbf{d}^f) \boldsymbol{\sigma}(\mathbf{u}, p) \mathbf{F}(\mathbf{d}^f)^{-T} \hat{\mathbf{n}}, \quad \text{on } \hat{\Sigma}, \quad (\text{stress})$$

Remark: alternatives

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- ID models

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- 1D models
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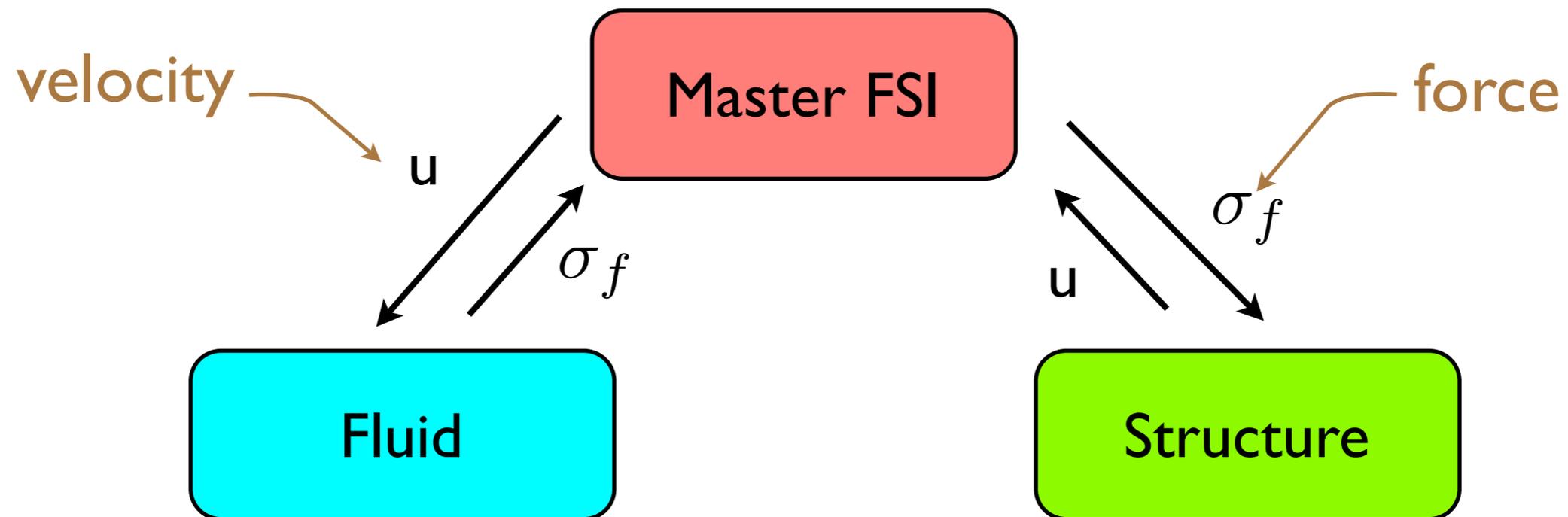
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 - if the stress within the wall is required
 - for valves

Implementation issues

- Use independent solvers for fluid and structure :
 - Advantage: re-usability of state-of-the-art algorithms
 - Difficulties: possible troubles with the coupling algorithms

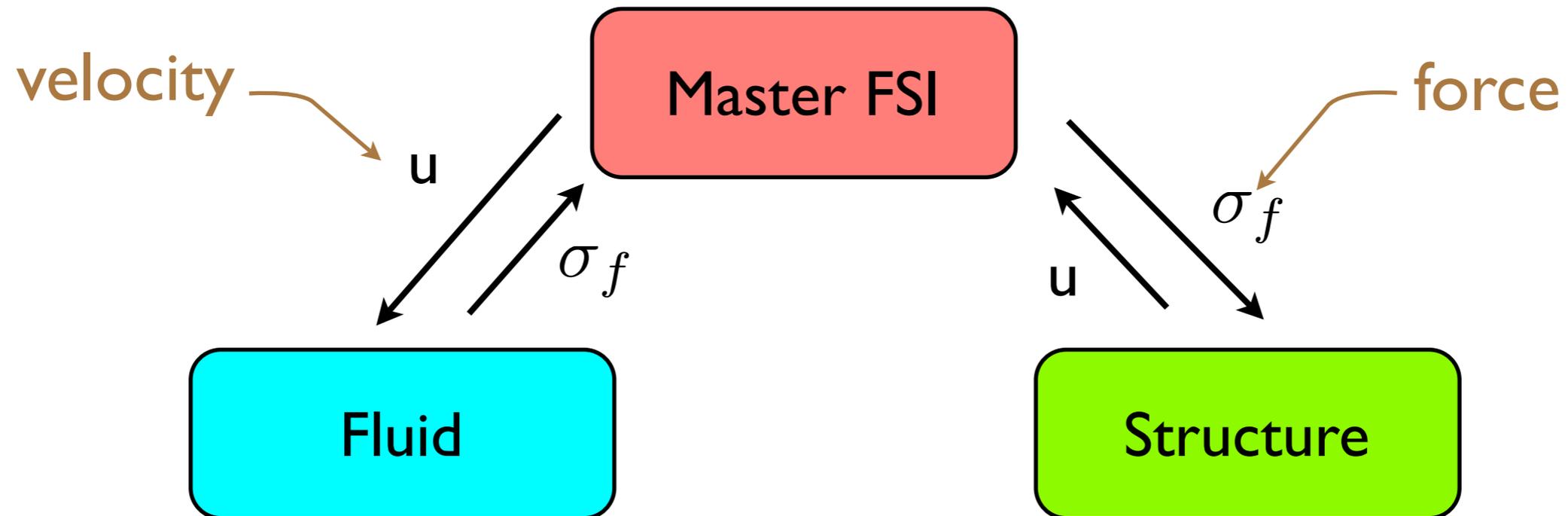
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- **Strong** coupling: sub-iterations at each time step
- **Weak** coupling : 1 or 2 iterations per time step

Example: Dirichlet-Neumann

- Fluid sub-problem: $(\mathbf{d}^{\text{f},n+1}, \mathbf{u}^{n+1}, p^{n+1}) = \mathcal{F}(\mathbf{d}_{|\hat{\Sigma}}^{n+1})$

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Fixed-point iterations with acceleration

(1) Initialization:

$$\boldsymbol{\lambda}^0 = \mathbf{d}_{|\hat{\Sigma}}^n$$

(2) Until convergence ($k \geq 0$):

(a) Solve fluid and solid:

$$\tilde{\boldsymbol{\lambda}}^{k+1} = (\mathcal{S} \circ \mathcal{F})(\boldsymbol{\lambda}^k)$$

(b) Relaxation:

$$\boldsymbol{\lambda}^{k+1} = \omega_k \tilde{\boldsymbol{\lambda}}^{k+1} + (1 - \omega_k) \boldsymbol{\lambda}^k, \quad \omega_k \in (0, 1]$$

► **Aitken acceleration**(*Wall, Ramm, 2001*):

$$\omega_k = \frac{(\boldsymbol{\lambda}^k - \boldsymbol{\lambda}^{k-1}) \cdot (\boldsymbol{\lambda}^k - \tilde{\boldsymbol{\lambda}}^k - \boldsymbol{\lambda}^{k-1} + \tilde{\boldsymbol{\lambda}}^{k-1})}{|\boldsymbol{\lambda}^k - \tilde{\boldsymbol{\lambda}}^k - \boldsymbol{\lambda}^{k-1} + \tilde{\boldsymbol{\lambda}}^{k-1}|^2}$$

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Domain decomposition

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Option I : decompose first then linearize

- Dirichlet-Neumann
 - Fixed-point : *Le Tallec-Mouro (1999)* *Wall-Ramm (2001)*, ...
 - Newton : *Fernandez-Moubachir (2003)*, ...
 - Inexact Newton: *Matthies-Steindorf (2003)*, *JFG-Vidrascu (2003)*, *Mischler-van Brummelen-de Borst (2005)*, *Vierendeels (2006)*,...
- Neumann - Neumann
 - *Deparis-Discacciati-Quarteroni (2005)*, ...
- Robin - Neumann
 - *Badia-Nobile-Vergara (2007)*

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Domain decomposition

Option 1 : decompose first then linearize

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Common feature:

*These algorithms are strongly coupled, for **stability**.*

Number of sub-iterations : between 10 and 100 !

Explicit coupling: some observations

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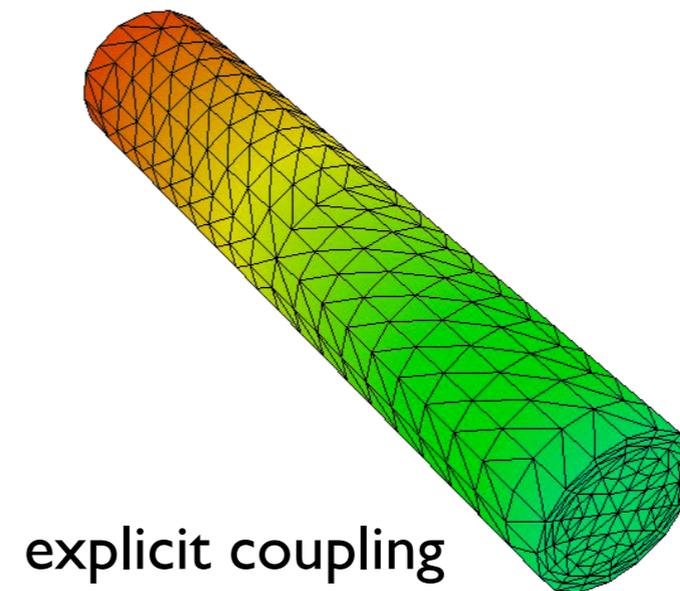
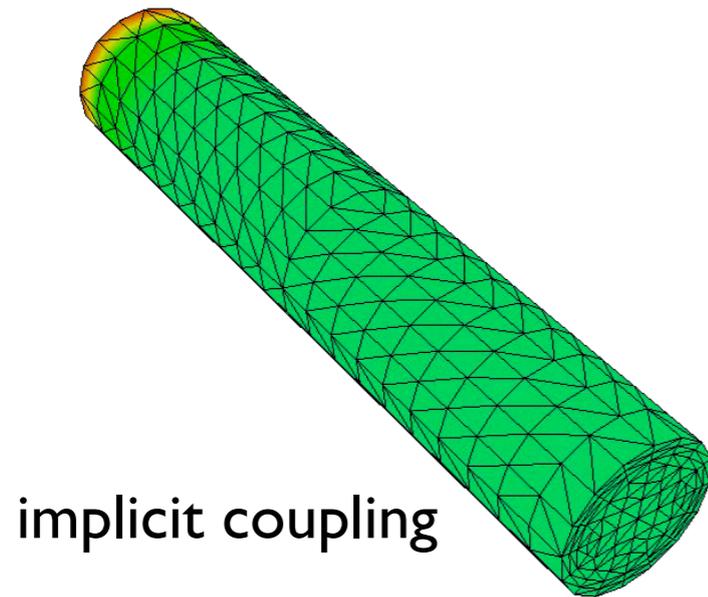
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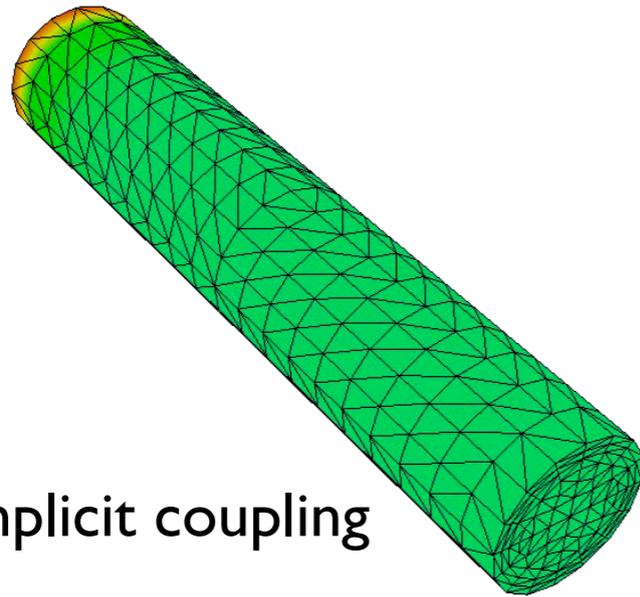


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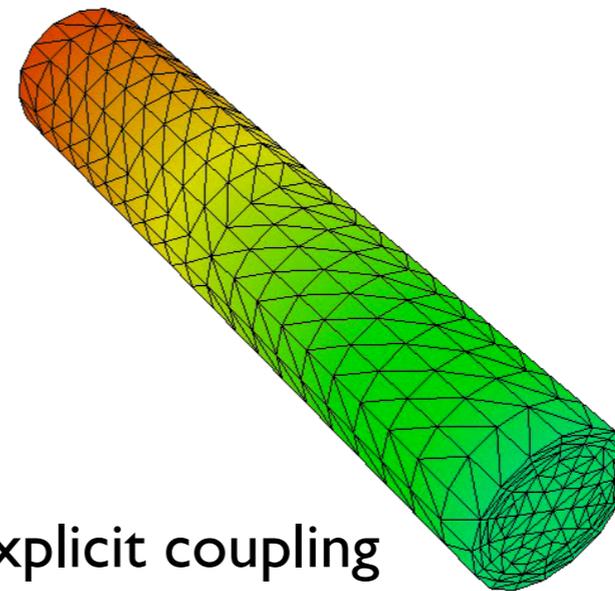
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implicit coupling



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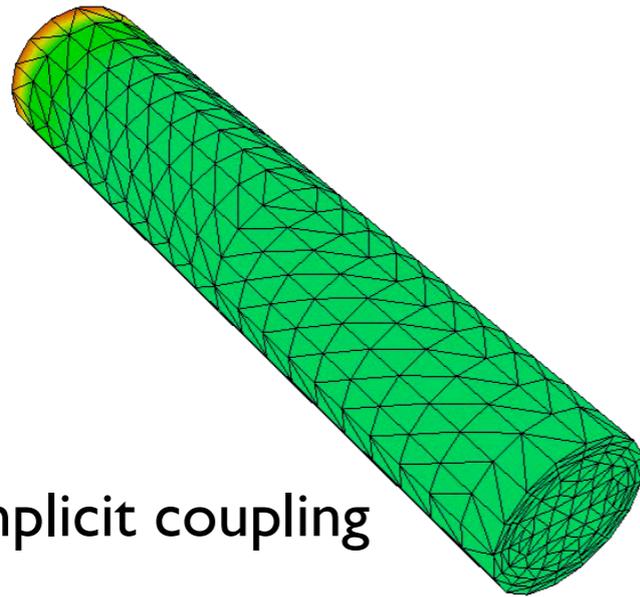
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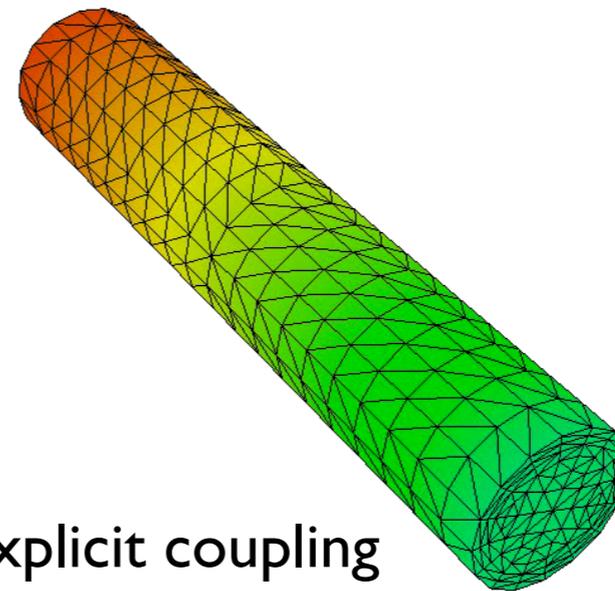
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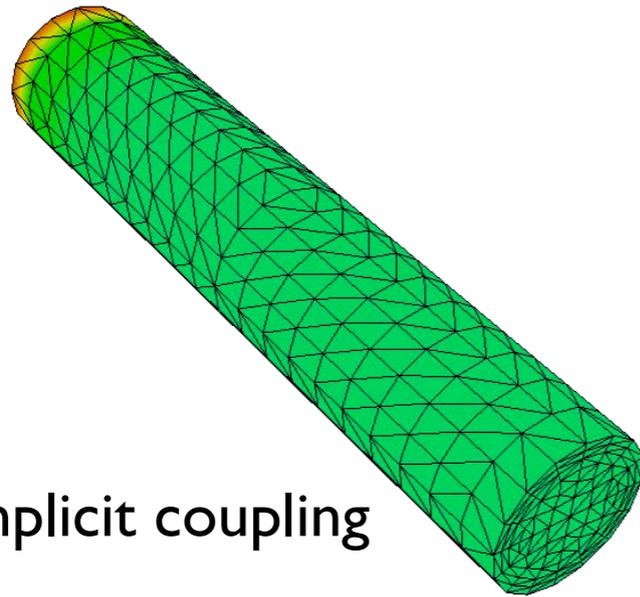
- **Explicit coupling** is **stable** and widely used in **aeroelasticity** !
Ex : *Farhat, van der Zee, Geuzaine, 2006*

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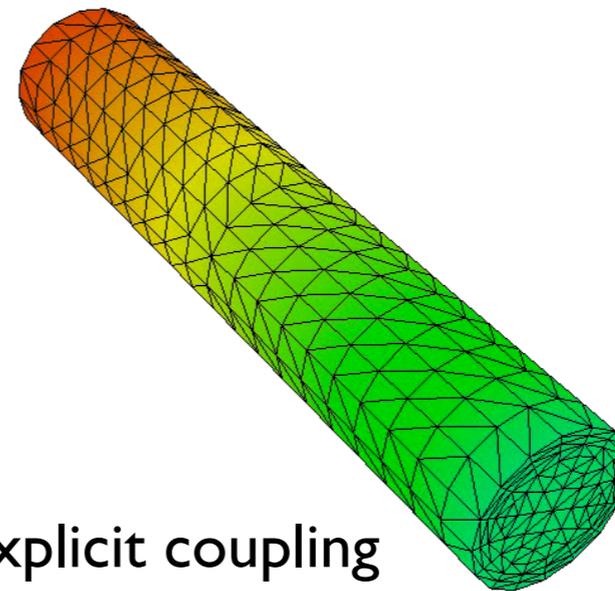
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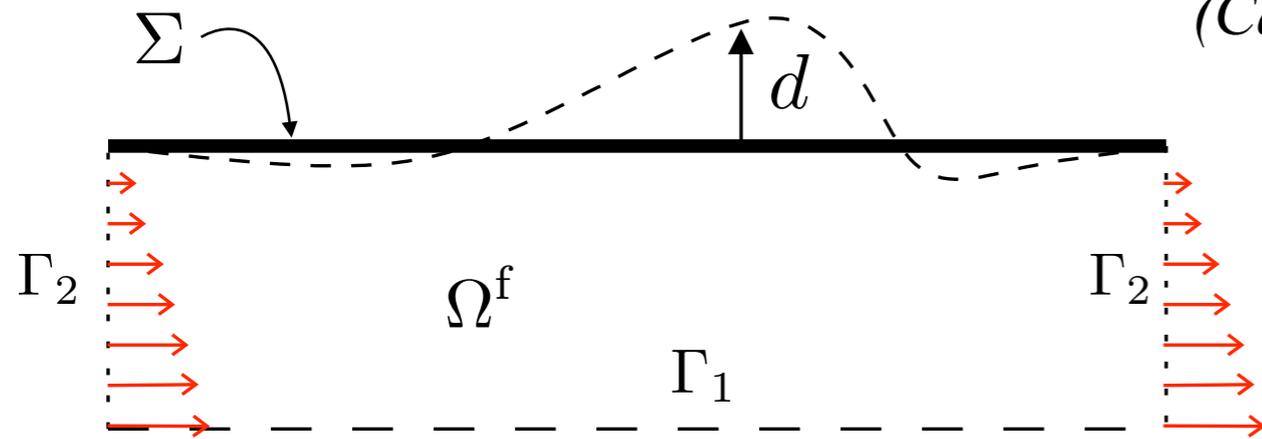
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► What is the **source of instabilities of those schemes in blood flows** ?

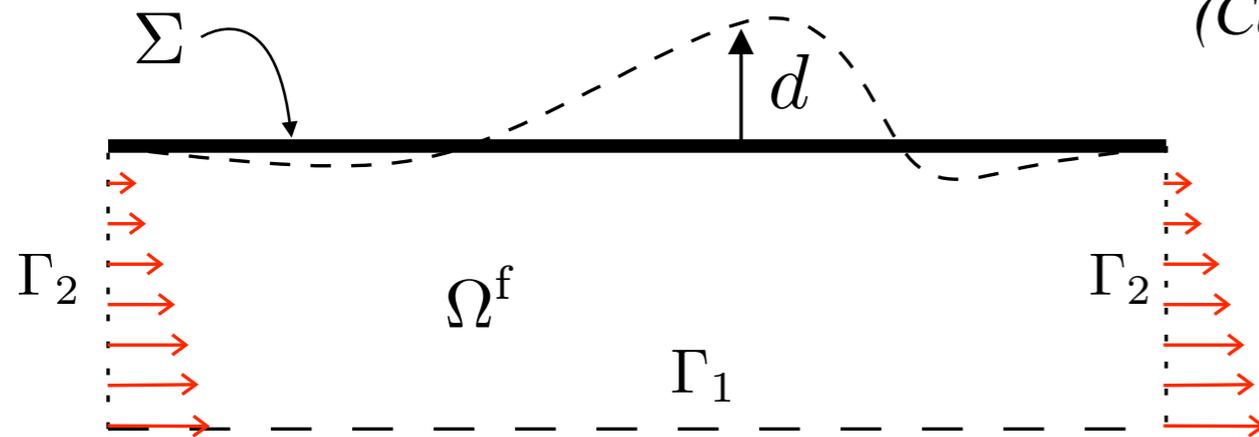
A 2D simplified model

(Causin, JFG, Nobile, 2004)



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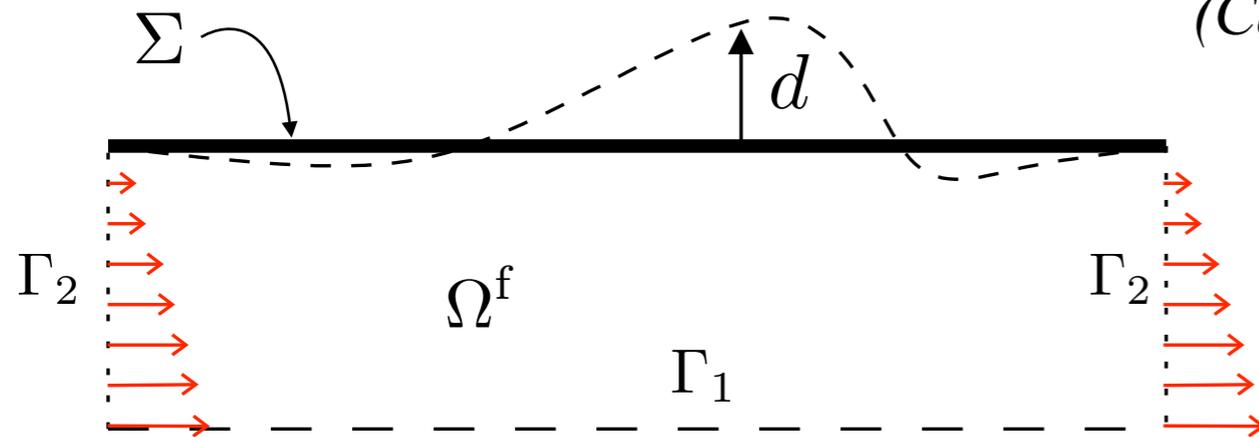
- **Solid:** string model (small displacements)

with
$$\rho^s \varepsilon \ddot{d} + Ld = p|_{\Sigma}, \quad \text{in } \Sigma,$$

- d : vertical displacement
- ε : vessel thickness
- L : linear operator (for instance $L\eta = a\eta - b \frac{\partial^2 \eta}{\partial x^2}$)

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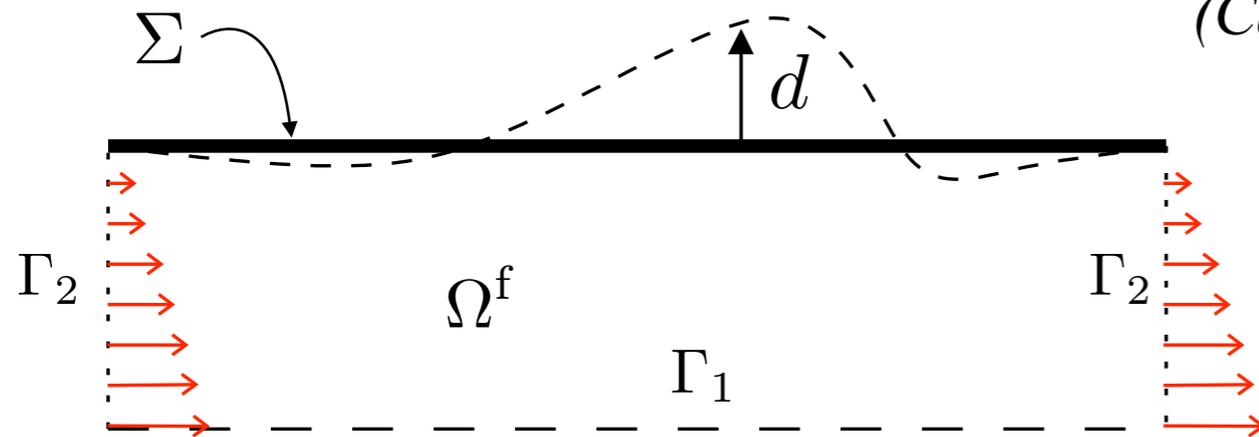
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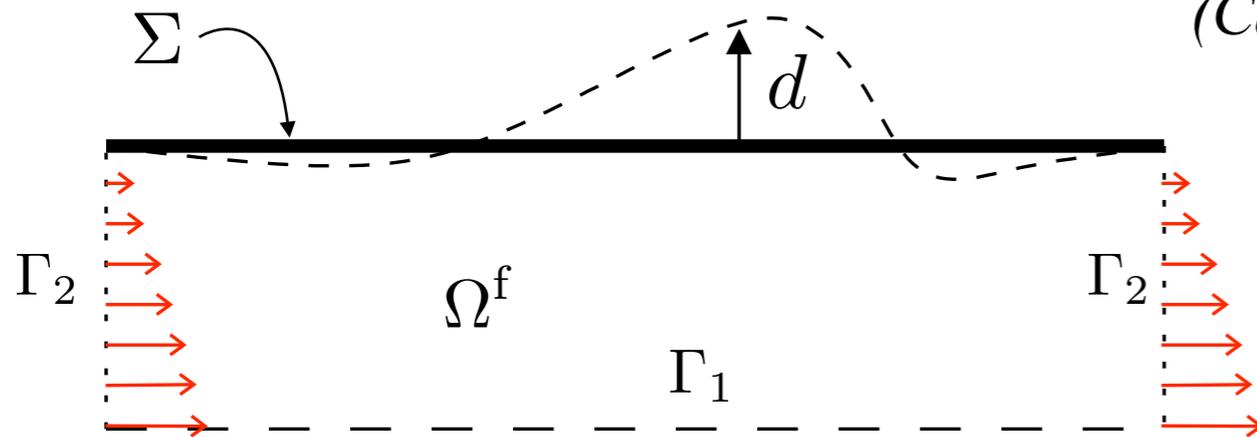
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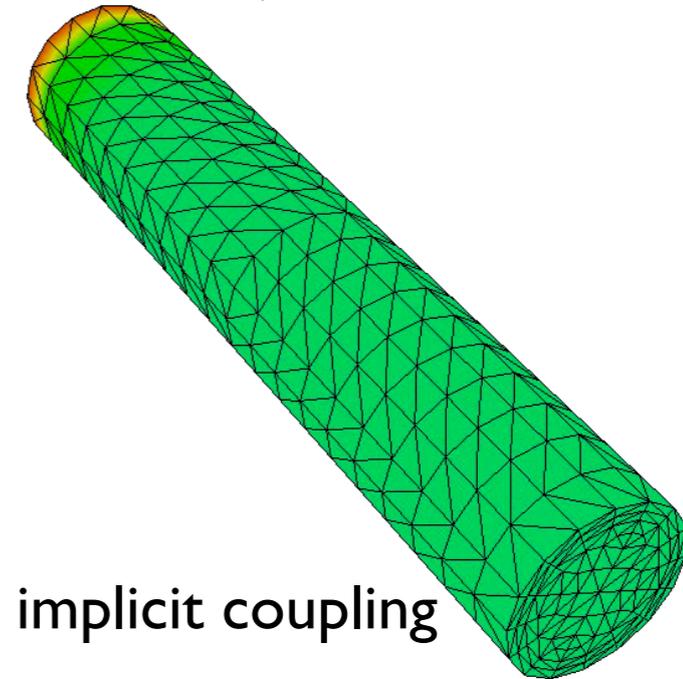
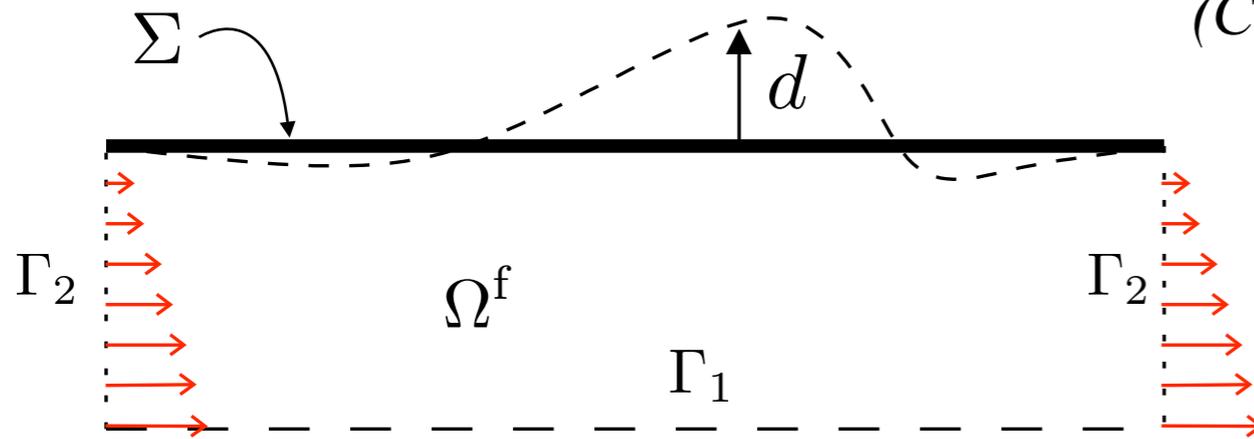
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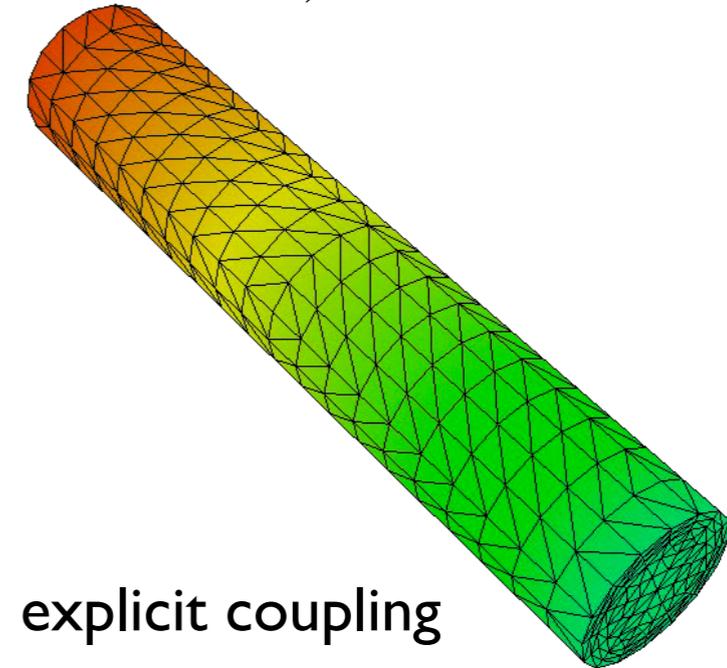
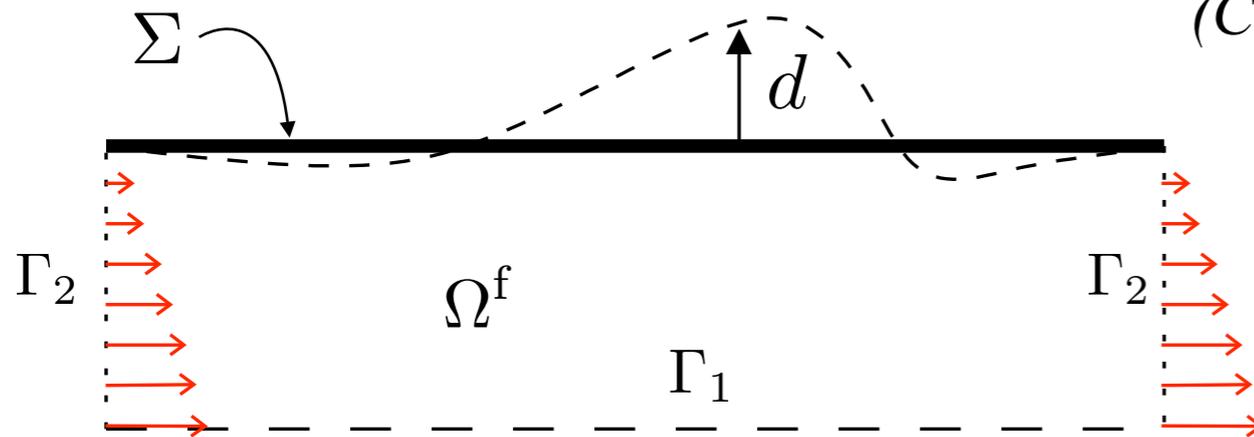
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The added-mass operator

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The operator $\mathcal{M}_A : H^{-\frac{1}{2}}(\Sigma) \rightarrow H^{\frac{1}{2}}(\Sigma)$ defined as: for each $g \in H^{-\frac{1}{2}}(\Sigma)$ we set $\mathcal{M}_A(g) \stackrel{\text{def}}{=} q|_{\Gamma^w}$, where $q \in H^1(\Omega^f)$ solves

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✓ From this definition, we have $p|_{\Sigma} = \mathcal{M}_A(-\rho^f \ddot{d}) = -\rho^f \mathcal{M}_A \ddot{d}$

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Remarks:

- ▶ This equation looks like a structure equation, except for the extra “mass” term
- ▶ The **fluid-structure coupling** can be condensed into an **extra mass** action on the structure (hence the terminology “added-mass effect”)

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Question :

What kind of time integration scheme of (2) arises from the explicit coupling of (1)?

Explicit coupling and added-mass

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Condensed FSI problem:

$$\rho^s \varepsilon \frac{d^{n+1} - 2d^n + d^{n-1}}{\delta t^2} + \rho^f \mathcal{M}_A \frac{d^n - 2d^{n-1} + d^{n-2}}{\delta t^2} + L \eta^{n+1} = 0$$

Explicit coupling and added-mass

$$\text{Fluid: } \left\{ \begin{array}{l} \rho^f \frac{\mathbf{u}^{n+1} - \mathbf{u}^n}{\delta t} + \nabla p^{n+1} = 0 \\ \operatorname{div} \mathbf{u}^{n+1} = 0 \\ \mathbf{u}^{n+1} \cdot \mathbf{n} = \frac{d^n - d^{n-1}}{\delta t} \end{array} \right. \xRightarrow{\operatorname{div}} \left\{ \begin{array}{l} -\Delta p^{n+1} = 0 \\ \frac{\partial p^{n+1}}{\partial \mathbf{n}} = -\rho^f \frac{d^n - 2d^{n-1} + d^{n-2}}{\delta t^2} \end{array} \right.$$

$$\text{Solid: } \rho^s \varepsilon \frac{d^{n+1} - 2d^n + d^{n-1}}{\delta t^2} + L d^{n+1} = p|_{\Sigma}^{n+1} \quad p|_{\Sigma}^{n+1} = -\rho^f \mathcal{M}_A \frac{d^n - 2d^{n-1} + d^{n-2}}{\delta t^2}$$

Condensed FSI problem:

$$\underbrace{\rho^s \varepsilon \frac{d^{n+1} - 2d^n + d^{n-1}}{\delta t^2}}_{\text{implicit}} + \rho^f \mathcal{M}_A \frac{d^n - 2d^{n-1} + d^{n-2}}{\delta t^2} + L d^{n+1} = 0$$

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Observation:

Weak coupling leads to an explicit discretization of the added-mass

An unconditional instability result

Proposition (Causin-JFG-Nobile 04)

Let λ_{\max} be the largest eigenvalue of \mathcal{M}_A and assume that $L\eta = a\eta$. Then, the previous explicit coupling scheme is **unconditionally unstable** whenever

$$\frac{\rho^f \lambda_{\max}}{\rho^s \varepsilon} \geq 1. \quad (1)$$

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Remarks:

- ▶ The instability condition does not depend on the time step
- ▶ The instability condition confirms two numerical observations:
 - Instabilities might occur when the structure is **light, thin and slender**
 - In aeroelasticity $\rho^f \ll \rho^s$, hence weak (*i.e.* explicit) coupling is stable

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Three ideas: (*Fernandez, JFG, Grandmont, 2006*)

- ▶ Treat implicitly the added-mass effect (incompressibility, pressure stress)
- ▶ Treat explicitly the fluid domain motion, convective and viscous effects
- ▶ Perform this using a projection scheme (Chorin-Teman) within the fluid

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$$\rho^f \left(\frac{\partial \mathbf{u}}{\partial t} + \mathbf{u} \cdot \nabla \mathbf{u} \right) - 2\mu \operatorname{div} \epsilon(\mathbf{u}) + \nabla p = \mathbf{0}, \quad \text{in } \Omega^f$$

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Semi-implicit coupling: **explicit** part

- Viscous sub-step:

$$\mathbf{d}^{f,n+1} = \text{Ext}(\mathbf{d}_{|\hat{\Sigma}}^n), \quad \mathbf{w}^{n+1} = \frac{\mathbf{d}^{f,n+1} - \mathbf{d}^n}{\delta t}, \quad \Omega^{f,n+1} = (I + \mathbf{d}^{f,n+1})(\hat{\Omega}^f),$$

$$\rho^f \left(\frac{\tilde{\mathbf{u}}^{n+1} - \mathbf{u}^n}{\delta t} + (\tilde{\mathbf{u}}^{n+1} - \mathbf{w}^{n+1}) \cdot \nabla \tilde{\mathbf{u}}^{n+1} \right) - 2\mu \text{div } \epsilon(\tilde{\mathbf{u}}^{n+1}) = 0, \quad \text{in } \Omega^{f,n+1}$$
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Observation:

- ▶ Fluid domain, viscous and convective effects explicitly treated

Semi-implicit coupling: **implicit** part

- Fluid projection sub-step (in a known domain):

$$\left\{ \begin{array}{l} \rho^f \frac{\mathbf{u}^{n+1} - \tilde{\mathbf{u}}^{n+1}}{\delta t} + \nabla p^{n+1} = 0, \quad \text{in } \Omega^{f,n+1} \\ \operatorname{div} \mathbf{u}^{n+1} = 0, \quad \text{in } \Omega^{f,n+1} \\ \mathbf{u}^{n+1} \cdot \mathbf{n} = \frac{\mathbf{d}^{n+1} - \mathbf{d}^n}{\delta t} \cdot \mathbf{n}, \quad \text{on } \Sigma^{n+1} \end{array} \right.$$

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Observations:

- Projection sub-step in a fixed fluid domain (fixed matrix)

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Observations:

- ▶ Projection sub-step in a fixed fluid domain (fixed matrix)
- ▶ Implicit part solved with cheaper (inner) iterations

A stability result (linear case)

Theorem: (Fernandez-JFG-Grandmont 2006)

Assume the interface matching operator to be L^2 -stable. Then, under condition

$$\rho^s \geq C \left(\rho^f \frac{h}{H^\alpha} + 2 \frac{\mu \delta t}{h H^\alpha} \right), \quad \text{with} \quad \alpha \stackrel{\text{def}}{=} \begin{cases} 0, & \text{if } \overline{\Omega^s} = \Sigma, \\ 1, & \text{if } \overline{\Omega^s} \neq \Sigma, \end{cases}$$

the following discrete energy inequality holds:

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Therefore, the **semi-implicit coupling** scheme is **conditionnally stable** in the energy norm.

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$$\begin{aligned} \frac{1}{\delta t} \left[\frac{\rho^f}{2} \|\mathbf{u}_h^{n+1}\|_{0,\Omega^f}^2 - \frac{\rho^f}{2} \|\mathbf{u}_h^n\|_{0,\Omega^f}^2 + \frac{\rho^s}{2} \left\| \frac{\mathbf{d}_H^{n+1} - \mathbf{d}_H^n}{\delta t} \right\|_{0,\Omega^f}^2 - \frac{\rho^s}{2} \left\| \frac{\mathbf{d}_H^n - \mathbf{d}_H^{n-1}}{\delta t} \right\|_{0,\Omega^f}^2 \right] \\ + \frac{1}{2\delta t} [a^s(\mathbf{d}_H^{n+1}, \mathbf{d}_H^{n+1}) - a^s(\mathbf{d}_H^n, \mathbf{d}_H^n)] + \mu \|\epsilon(\tilde{\mathbf{u}}_h^{n+1})\|_{0,\Omega^f}^2 \leq 0 \end{aligned}$$

Therefore, the **semi-implicit coupling** scheme is **conditionnally stable** in the energy norm.

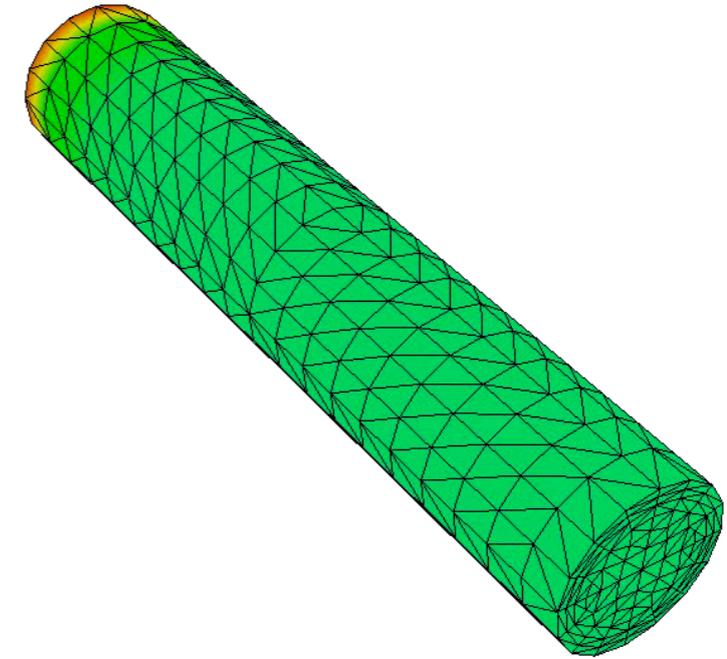
Remark: this semi-implicit algorithm has been extended by [Badia, Quarteroni, Quaini, 2007](#) to other projection schemes.

3D Navier-Sokes / Non-linear Shell coupling

- Straight cylinder: 50 time steps of length $\delta t = 2 \times 10^{-4} s$

COUPLING	ALGORITHM	CPU time
Implicit	FP-Aitken	24.86
	quasi-Newton	6.05
	Newton	4.77
Semi-Implicit	Newton	1

← 2001
← 2003
← 2006

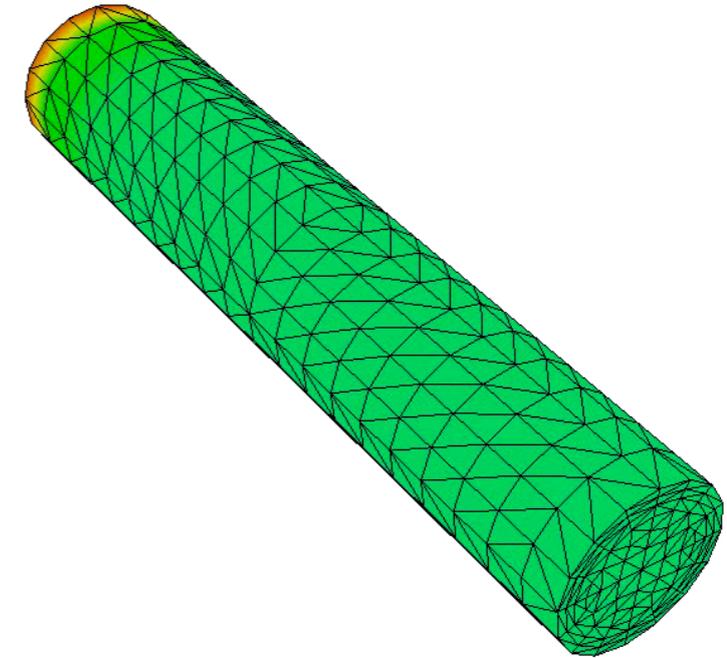


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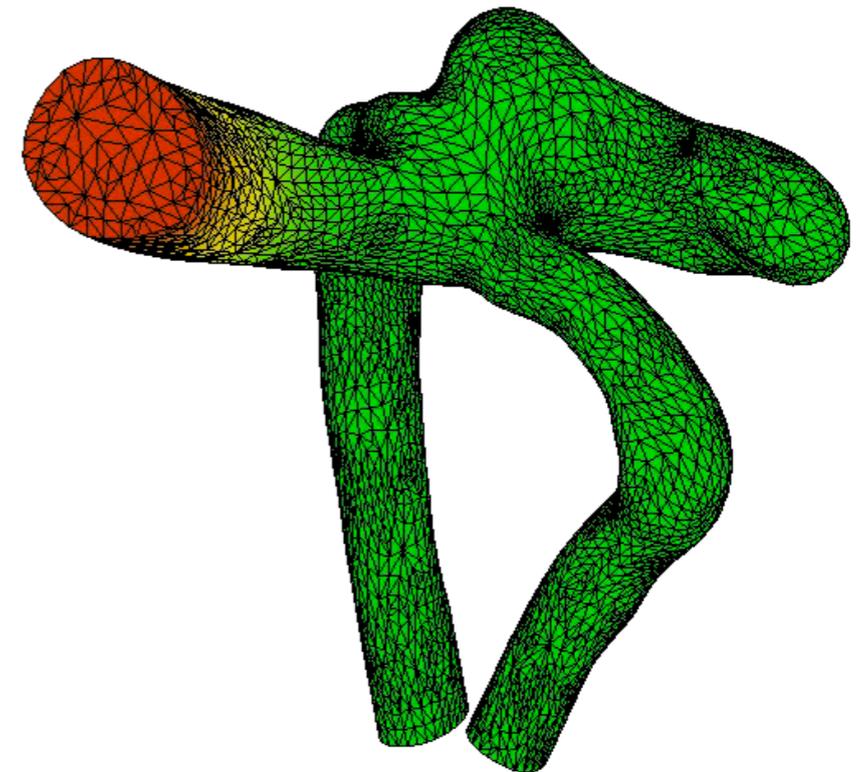
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	quasi-Newton	6.05
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Semi-Implicit	Newton	1

← 2001
 ← 2003
 ← 2006



- Cerebral aneurysm: 20 time steps of length $\delta t = \times 10^{-3} s$

COUPLING	CPU time
Implicit	4.70
Semi-Implicit	1



3D Navier-Sokes / Non-linear Shell coupling

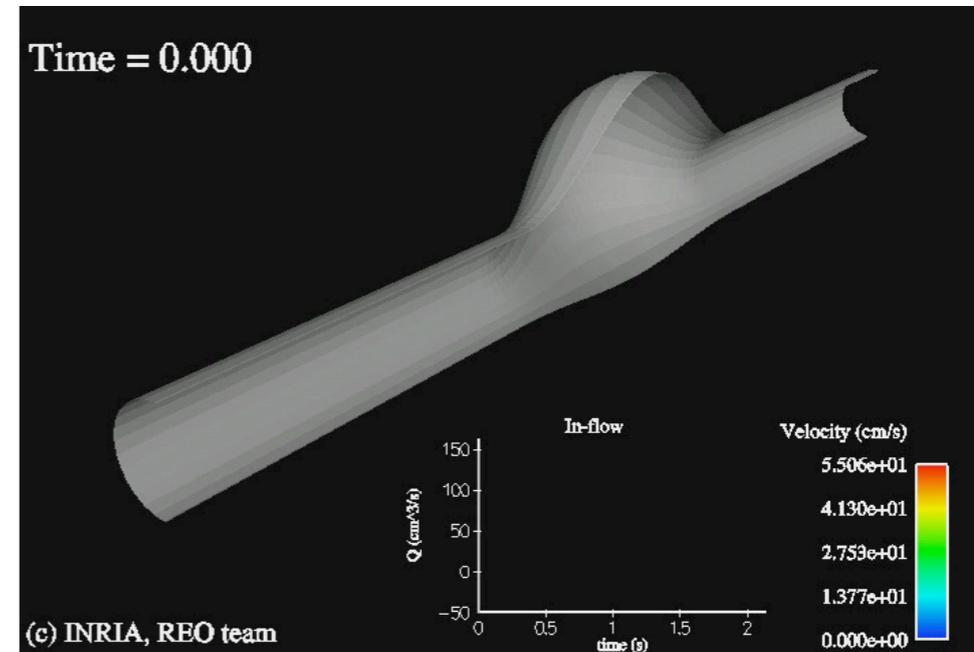
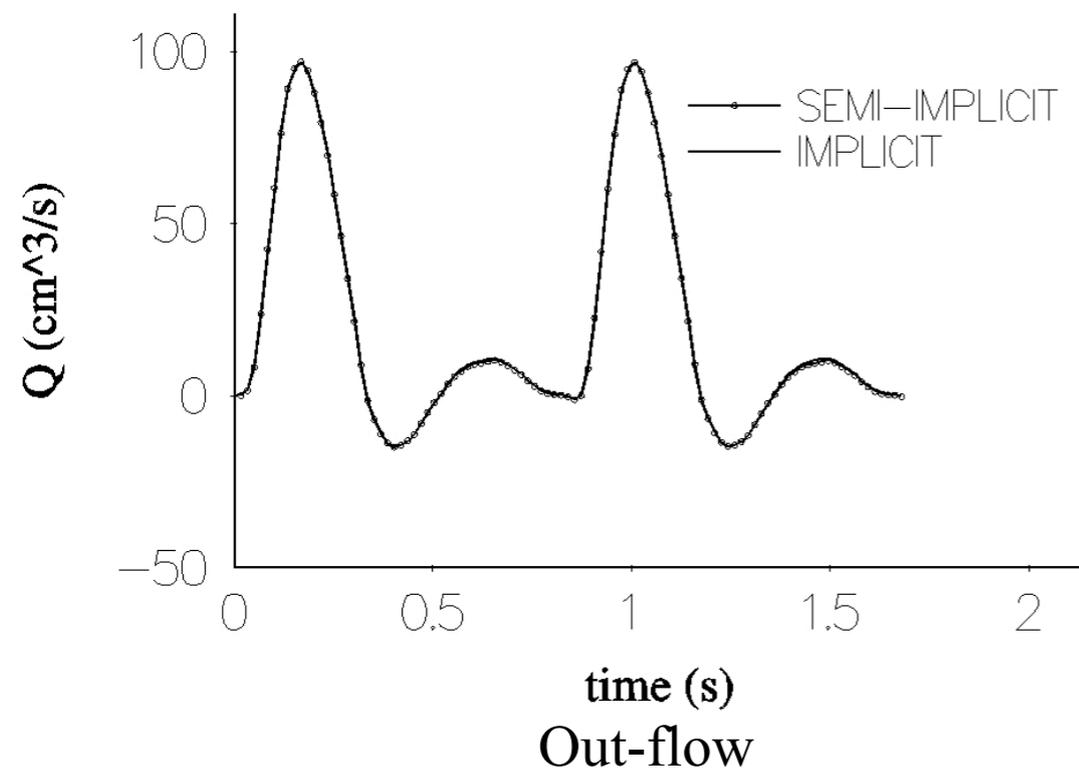
- Abdominal aortic aneurysm (in-vitro model): 2 cardiac cycles, 1000 times steps

- $\delta t = 1.68 \times 10^{-3} s$

- Fluid: 26950 Hexahedra (Q_1/Q_1 FE)

- Solid: 2240 Quadrilaterals (MITC4 FE)

- Parameters: $\mu = 0.035 \text{ poise}$, $\rho^f = 1 \text{ g/cm}^3$,
 $\rho^s = 1.2 \text{ g/cm}^3$, $E = 610^6 \text{ dynes/cm}^2$,
 $\nu = 0.3$

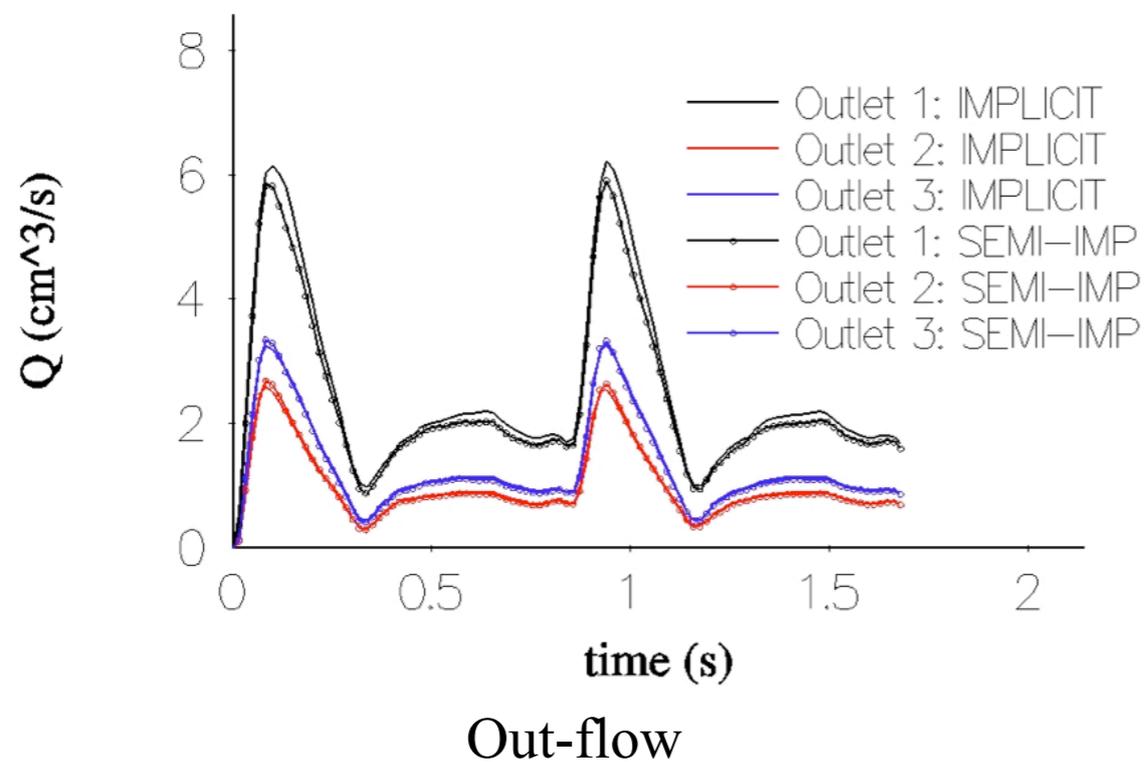


COUPLING	CPU time
Implicit	9.3
Semi-Implicit	1.0

Dimensionless CPU time

3D Navier-Stokes / Non-linear Shell coupling

- Carotid artery (in-vivo model): 9 cardiac cycles, 4500 time steps
 - $\delta t = 1.68 \times 10^{-3} s$
 - Fluid: 70047 Tetrahedra ($\mathbb{P}_1/\mathbb{P}_1$ FE)
 - Solid: 8103 Quadrilaterals (MITC4 FE)
 - Parameters: $\mu = 0.035 \text{ poise}$, $\rho^f = 1 \text{ g/cm}^3$,
 $\rho^s = 1.2 \text{ g/cm}^3$, $E = 6 \times 10^6 \text{ dynes/cm}^2$,
 $\nu = 0.3$.

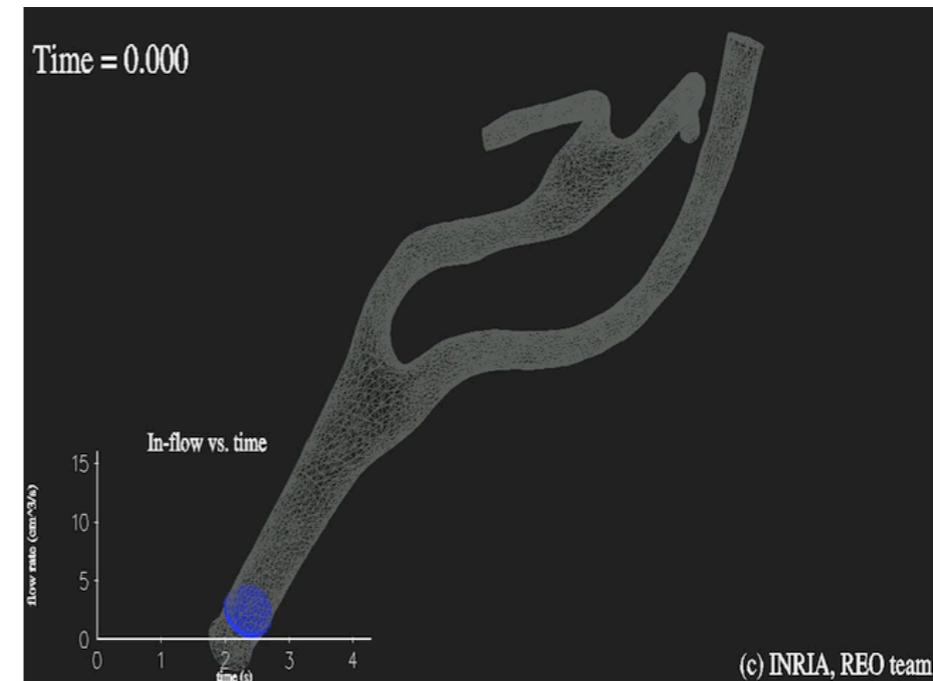
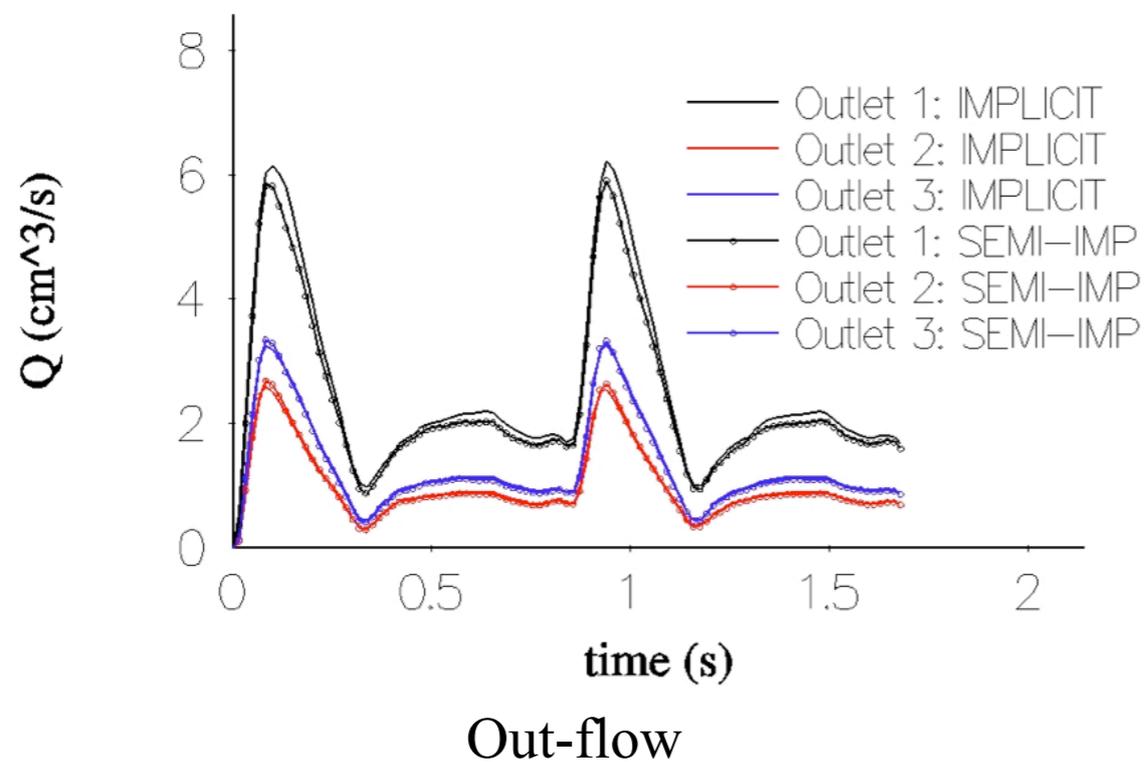


COUPLING	CPU time
Implicit	6.7
Semi-Implicit	1.0

Dimensionless CPU time

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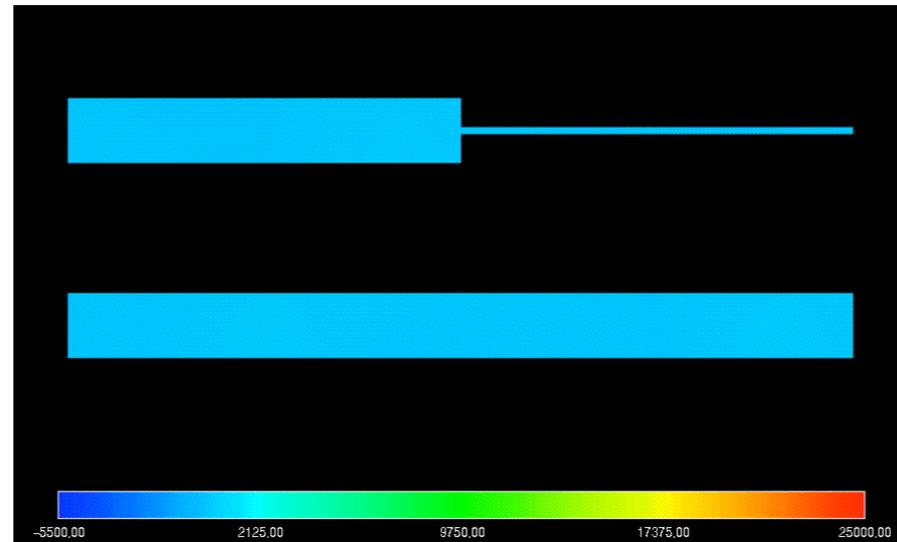
Dimensionless CPU time

Remarks on boundary conditions

- Spurious reflexion of pressure wave: 3D-ID coupling

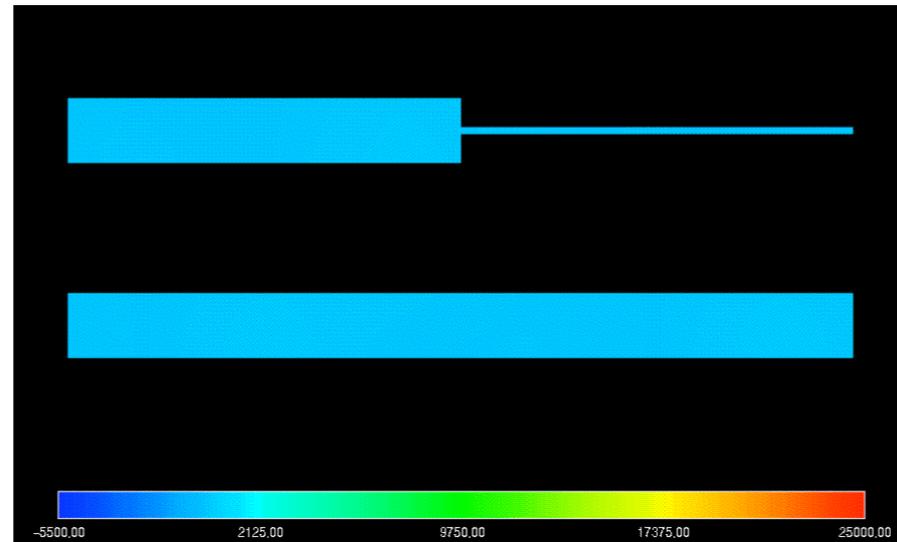
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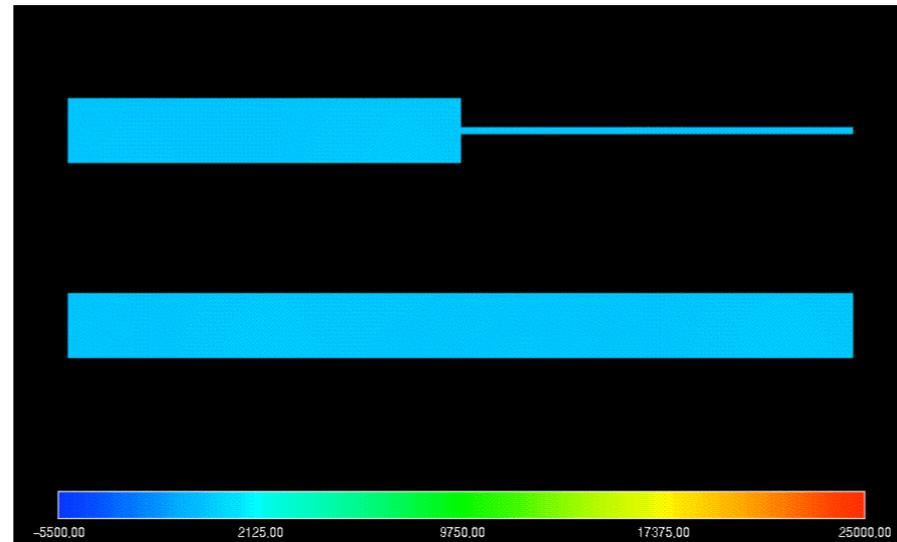
Formaggia, JFG, Quarteroni, Nobile, 2001

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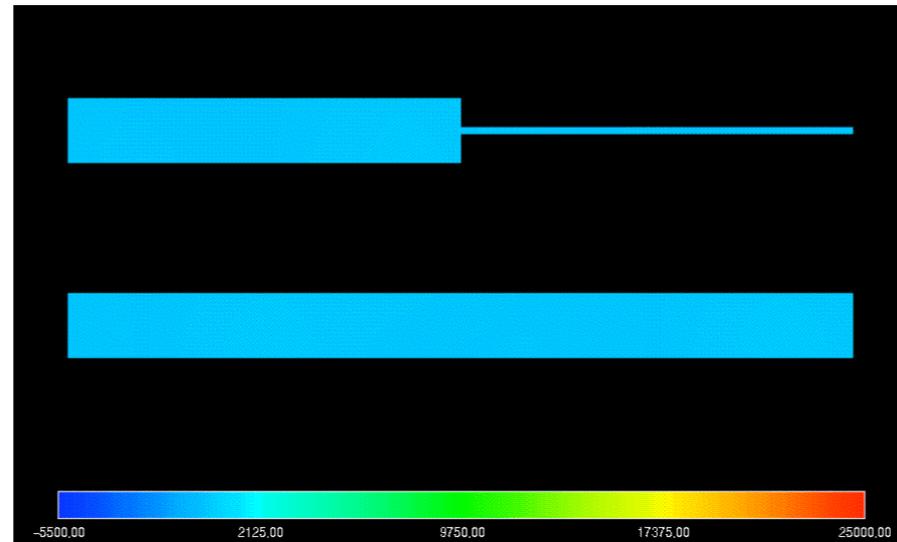
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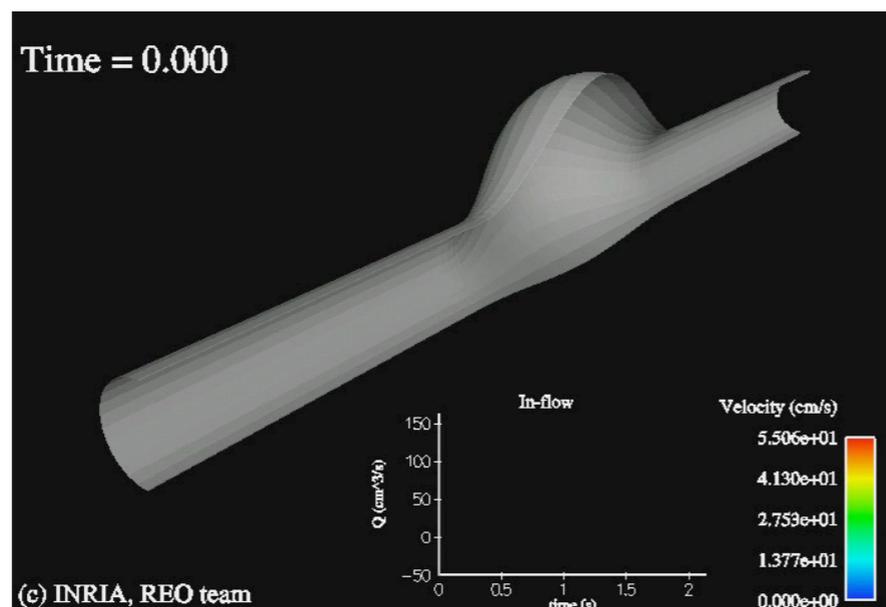


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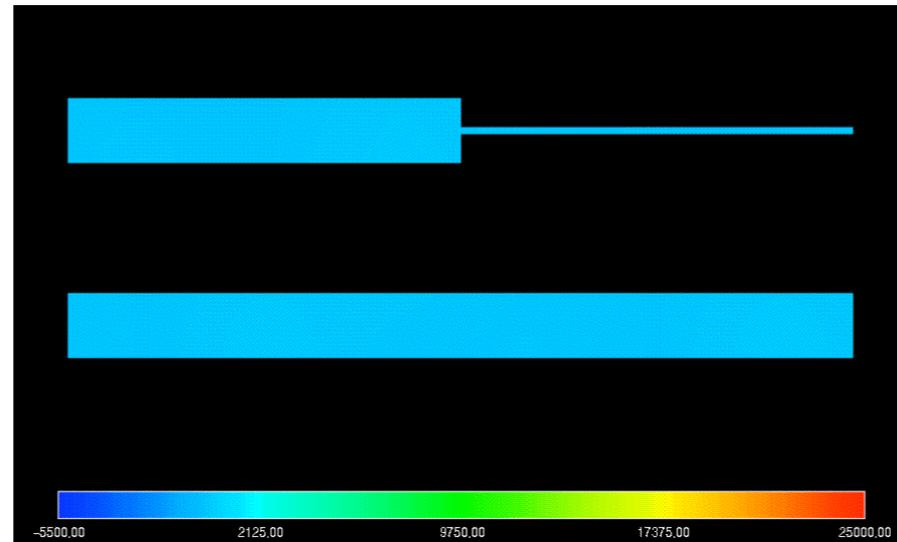
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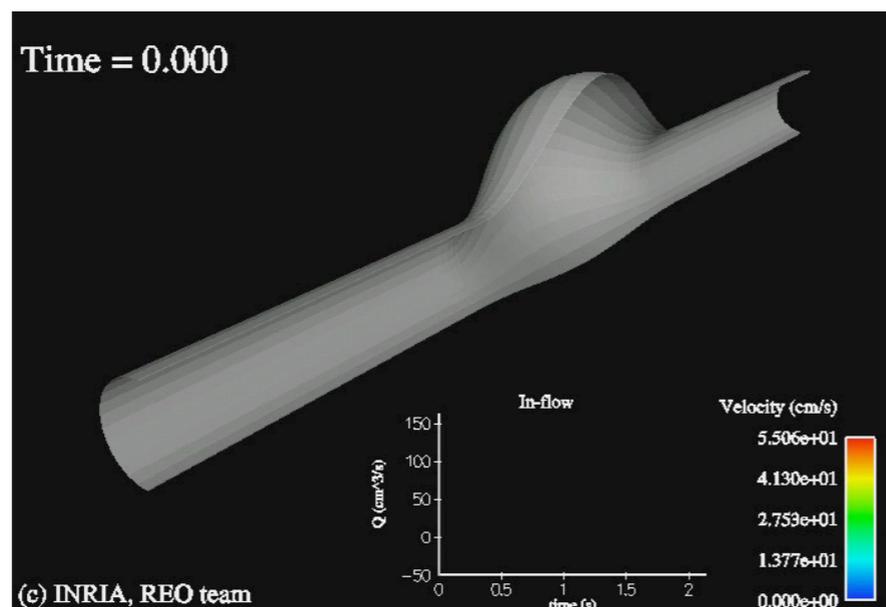


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- But pressure wave reflexion is not the only issue



The best non-reflecting outlet boundary condition cannot prevent the global (non physiological) bending !

Remarks on boundary conditions

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- Typical b.c. on the external part of the vessel :

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Remarks on boundary conditions

- Surrounding tissues play a key role

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$$F(d) S(d) \hat{n} = p_0$$

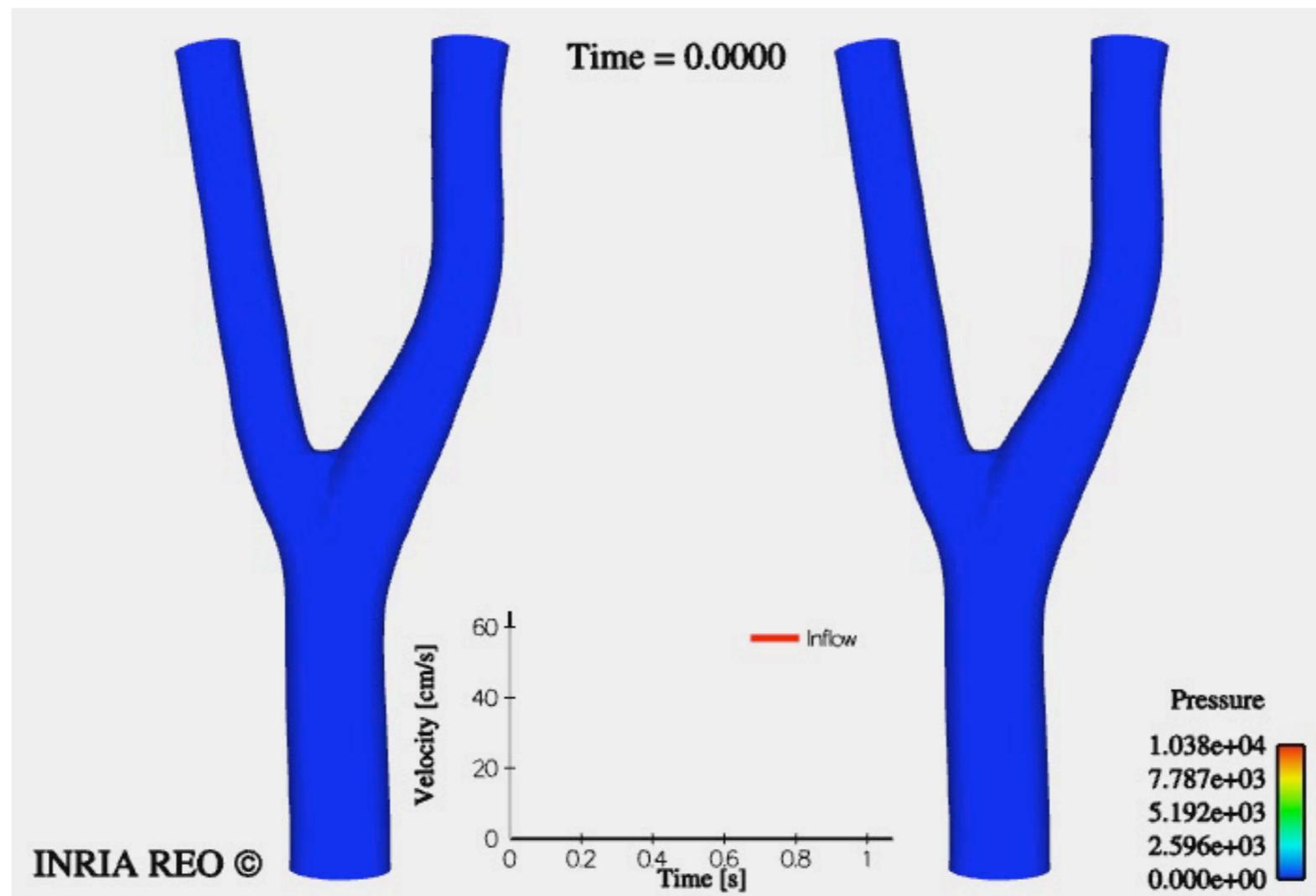
- A simple and affordable way to model the surrounding tissues (“silent blocks”):

$$F(d) S(d) \hat{n} = -k_s d - c_s \frac{\partial d}{\partial t}$$

Remarks on boundary conditions

$$F(\mathbf{d}) \cdot S(\mathbf{d}) \hat{\mathbf{n}} = -k_s \mathbf{d} - c_s \frac{\partial \mathbf{d}}{\partial t} \quad (\text{"silent blocks"})$$

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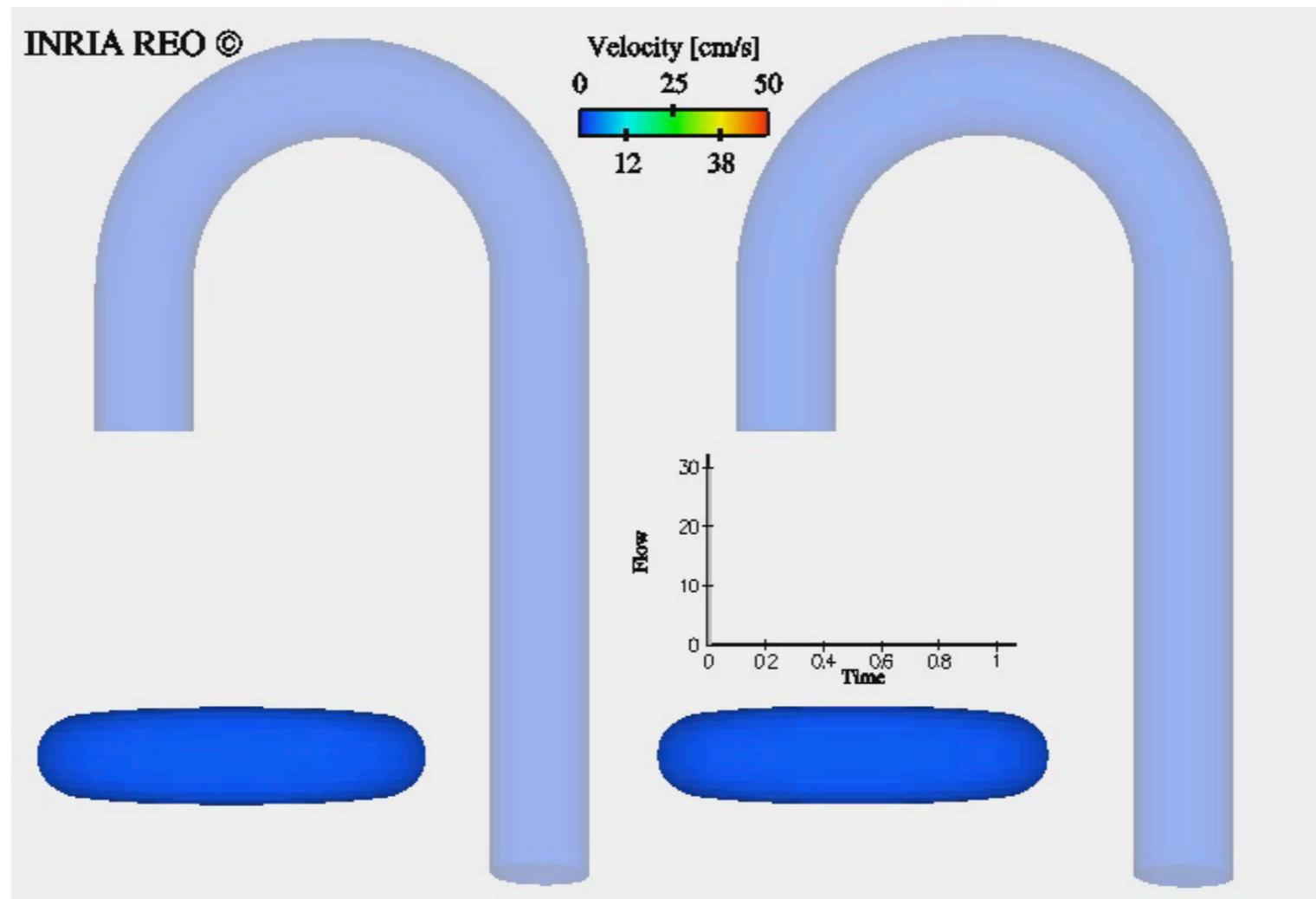


Astorino, JFG

Remarks on boundary conditions

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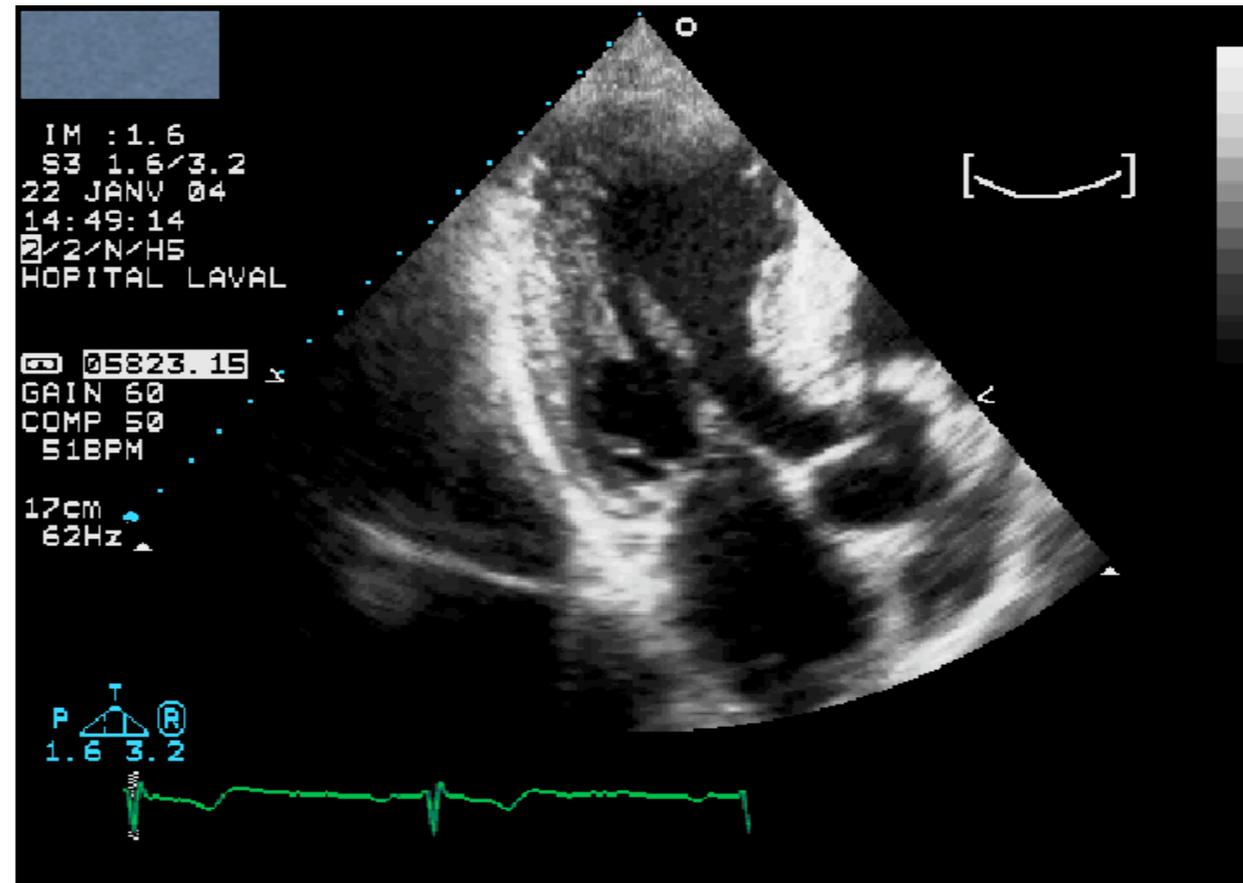
Outline

- Fluid-structure interaction in arteries
 - Stability issues - Strongly couple schemes
 - A stable weakly coupled scheme
- Fluid-structure interaction with valves
 - Fictitious domain method
 - FSI and Contact management

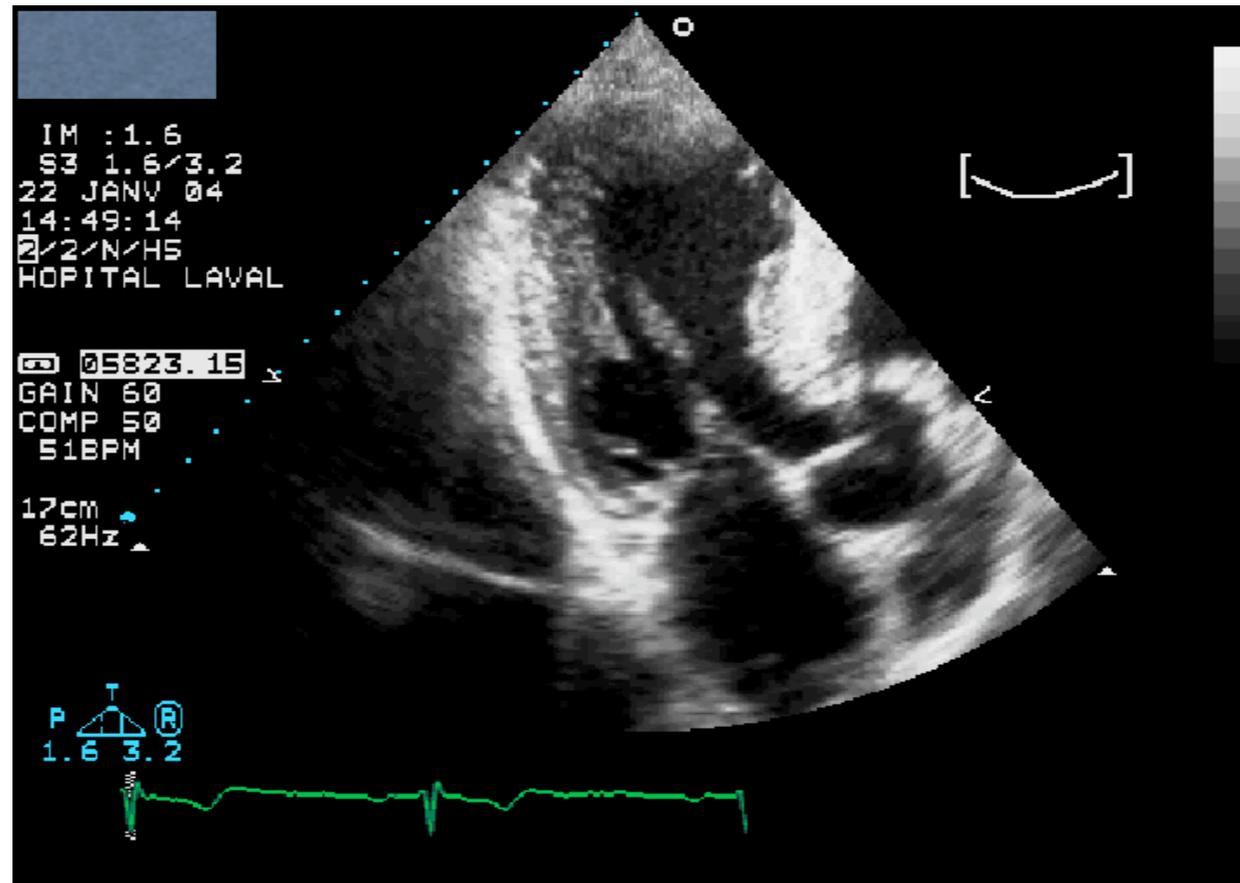
FSI with valves



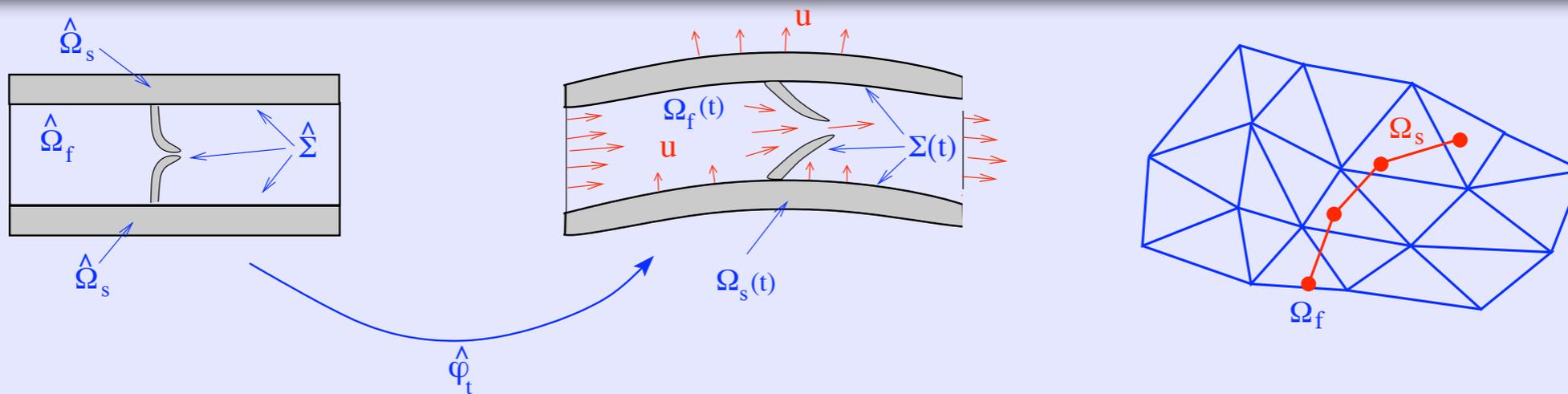
FSI with valves



FSI with valves



Valve : "Fictitious Domains" (FD)



“Fictitious Domain” for valves

- Basic idea: impose the kinematic constraint in a weak form

$$\langle \boldsymbol{\mu}, \boldsymbol{u}_f \rangle_{\Sigma} = \langle \boldsymbol{\mu}, \boldsymbol{u}_s \rangle_{\Sigma}, \forall \boldsymbol{\mu} \in \Lambda$$

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- A saddle point problem has to be solved in the fluid

$$\left\{ \begin{array}{l} a_f(\mathbf{u}_f, \mathbf{v}_f) + \langle \boldsymbol{\lambda}, \mathbf{v}_f \rangle_\Sigma = \int_{\Omega_f(t)} \mathbf{f}_f \cdot \mathbf{v}_f, \quad \forall \mathbf{v}_f \in X_f \\ \langle \boldsymbol{\mu}, \mathbf{u}_f \rangle_\Sigma - \langle \boldsymbol{\mu}, \mathbf{u}_s \rangle_\Sigma = 0 \quad \forall \boldsymbol{\mu} \in \Lambda \\ \hat{a}_s(\hat{\mathbf{u}}_s, \hat{\mathbf{v}}_s) - \langle \boldsymbol{\lambda}, \mathbf{v}_s \rangle_\Sigma = \int_{\hat{\Omega}_s} \hat{\mathbf{f}}_s \cdot \hat{\mathbf{v}}_s \quad \forall \hat{\mathbf{v}}_s \in \hat{X}_s \end{array} \right.$$

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$$\Lambda_h = \left\{ \boldsymbol{\mu}_h \text{ measure on } \Sigma, \boldsymbol{\mu}_h = \sum_{i=1}^{N_\Sigma} \boldsymbol{\mu}_i \delta(\mathbf{x}_i^{n+1}), \boldsymbol{\mu}_i \in \mathbb{R}^n \right\}$$

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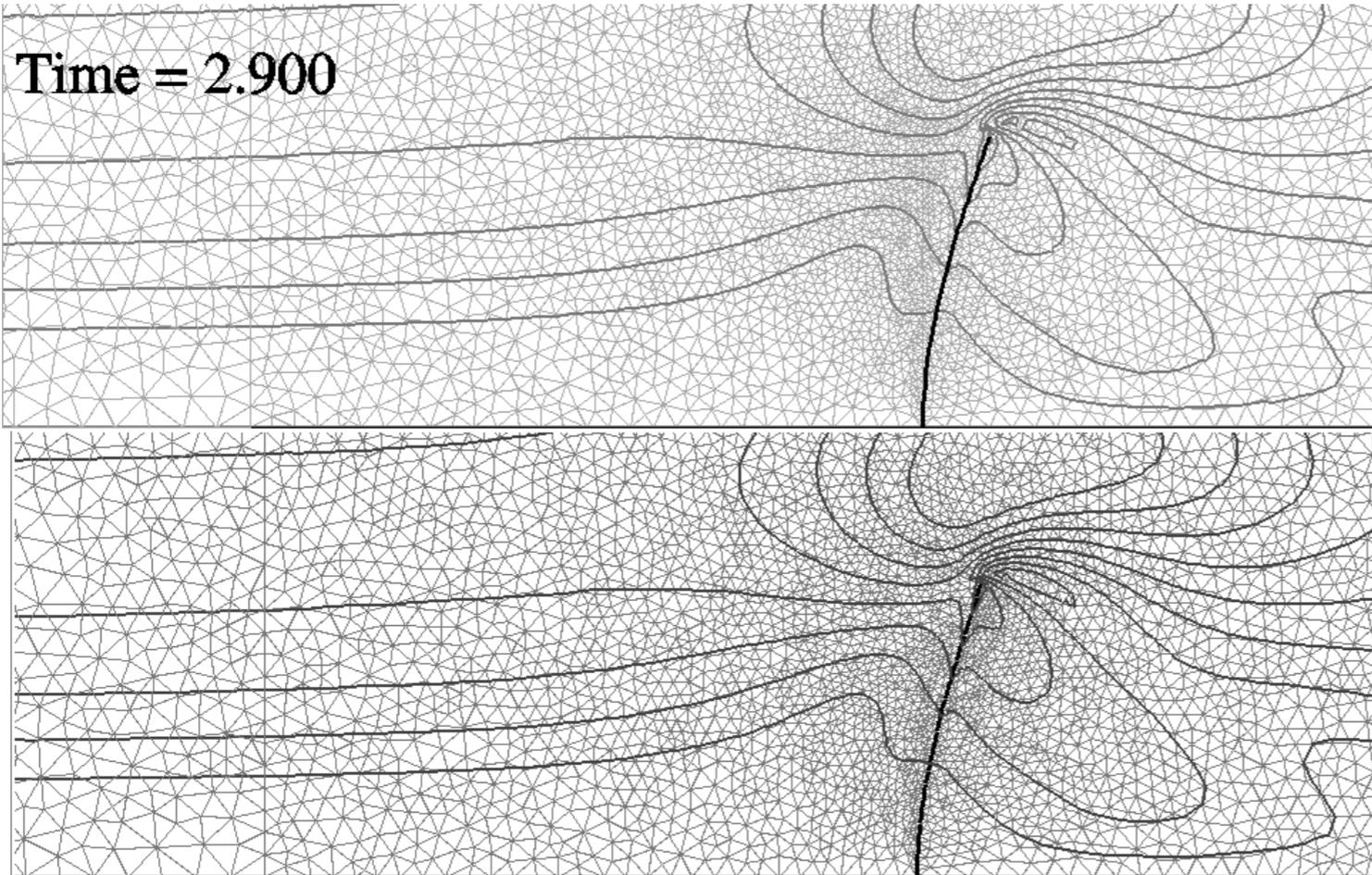
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- Other Lagrange multiplier spaces are possible

Baaijens, 2001, de Hart et al. 2003

ALE / FD

Comparison:

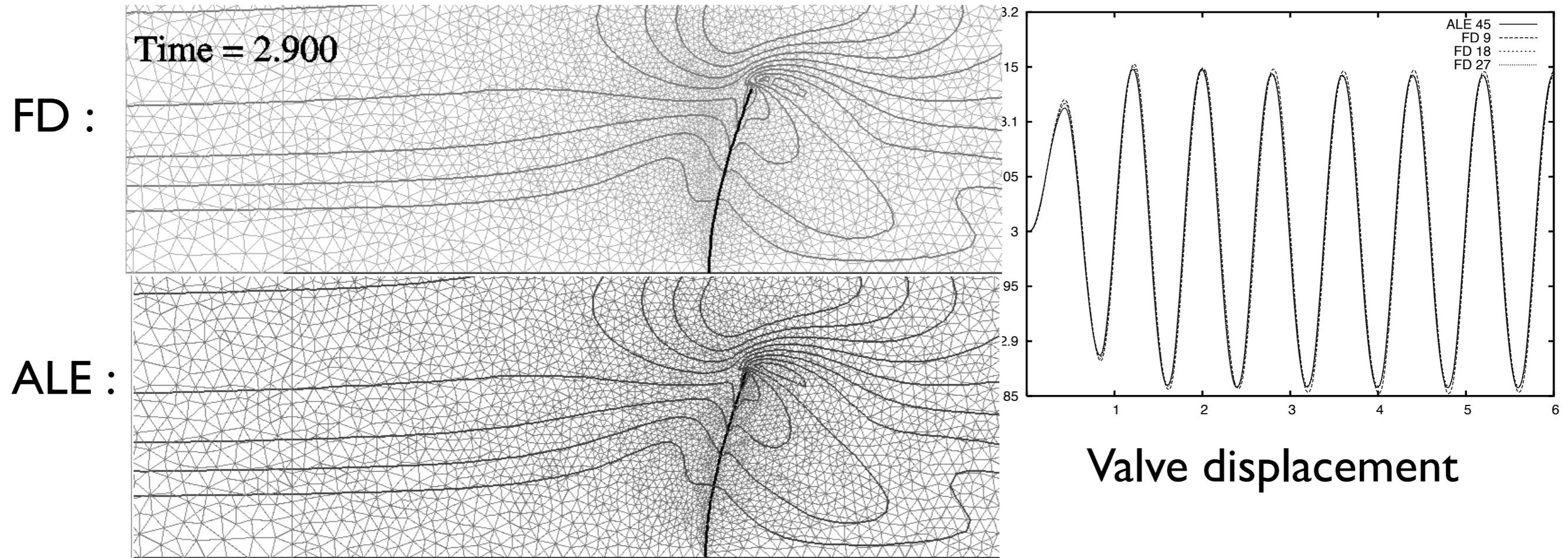


FD :

ALE :

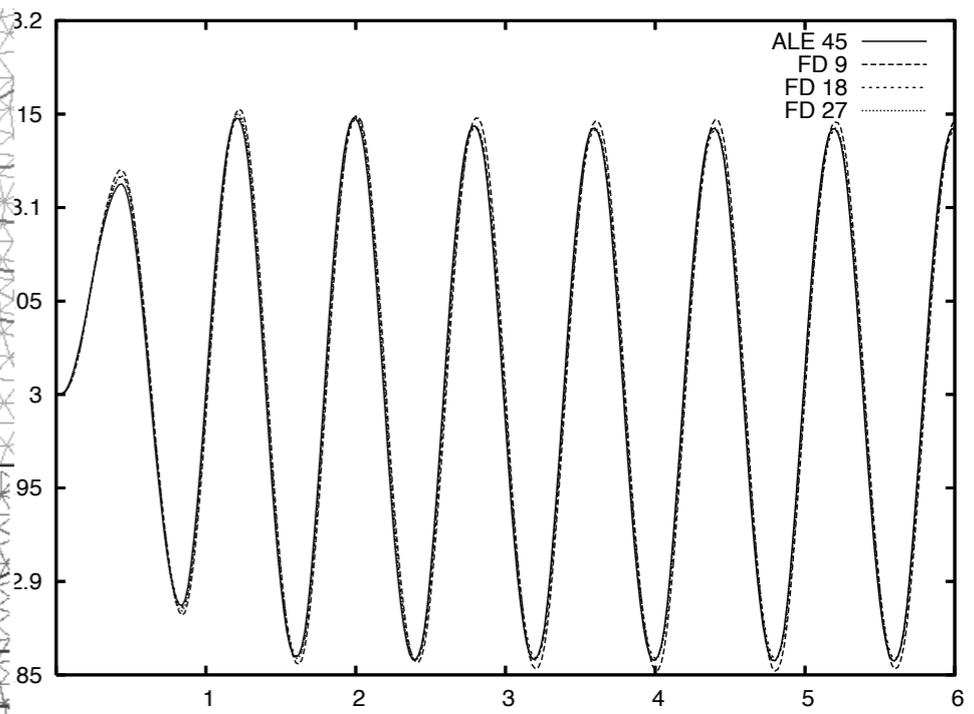
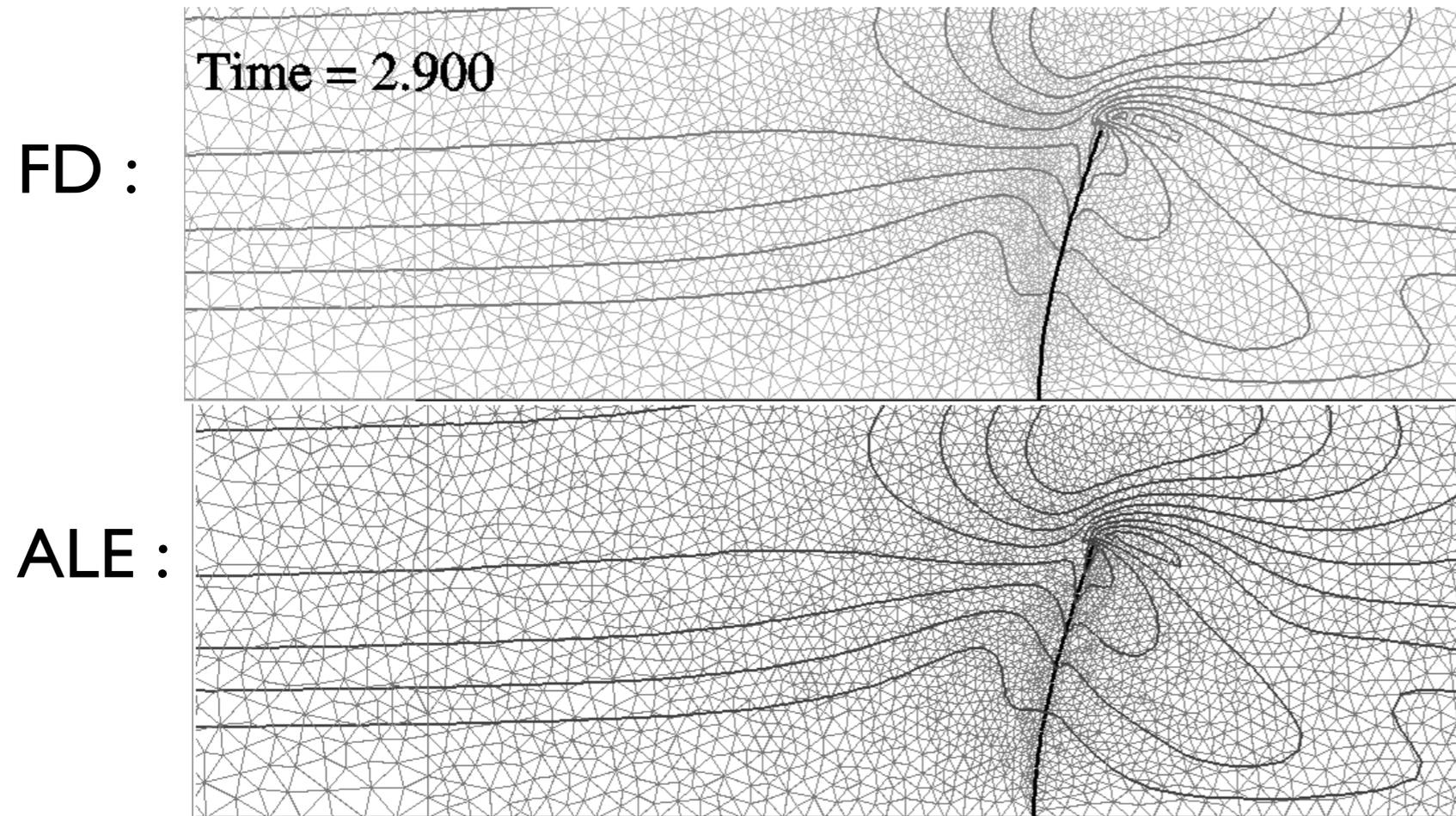
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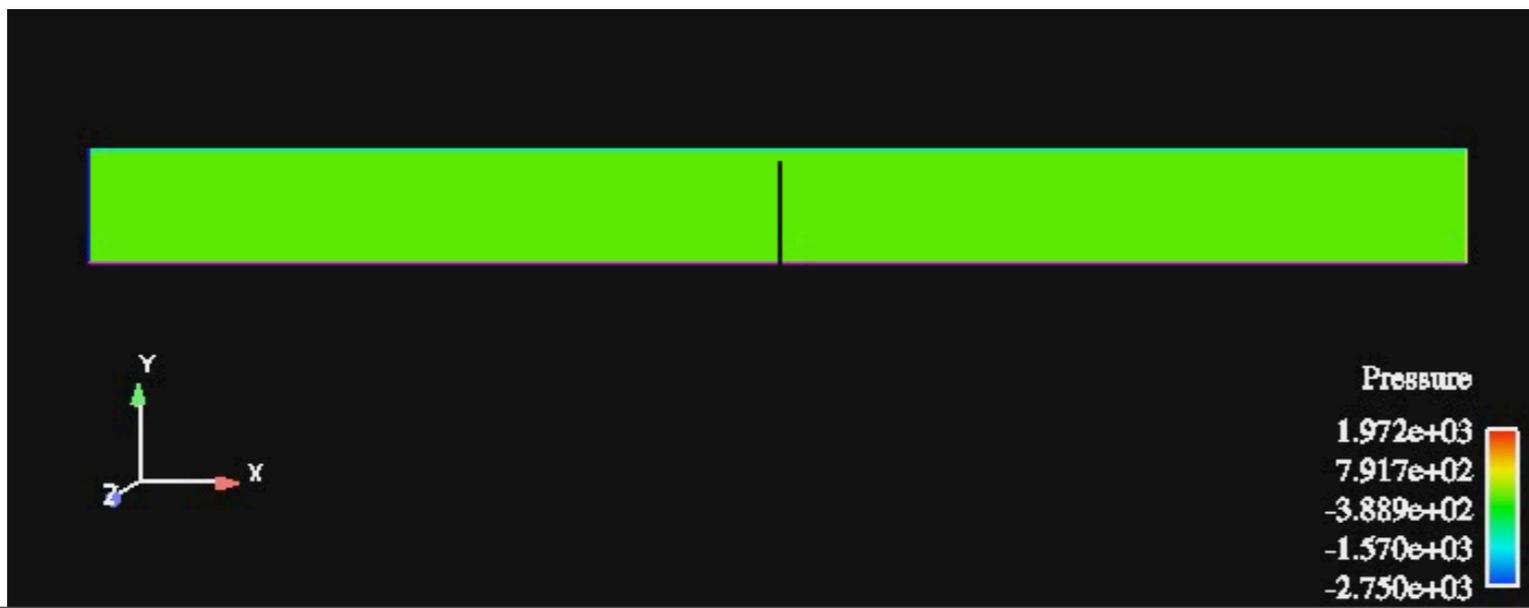
ALE / FD

Comparison:



Valve displacement

Mix ALE + FD:



FSI and kinematic constraints

FSI and kinematic constraints

- Valves are submitted to various kinematic constraints:

FSI and kinematic constraints

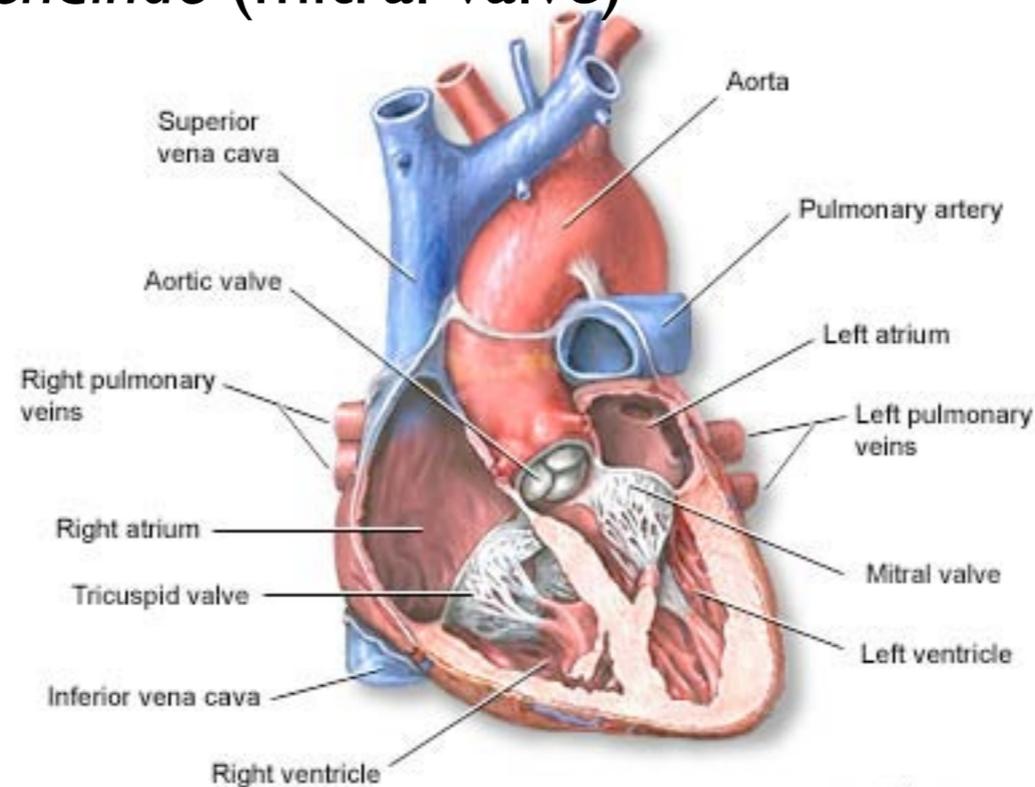
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FSI and kinematic constraints

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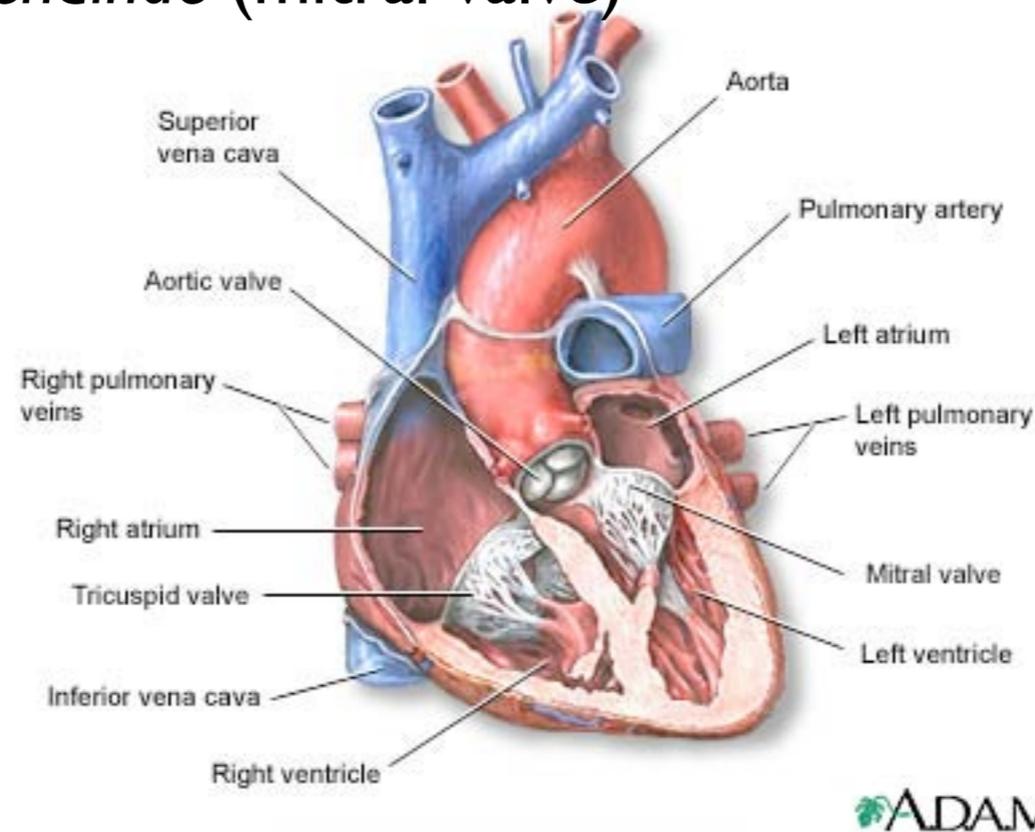
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FSI and kinematic constraints

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- We propose a framework to deal with these constraints in partitionned FSI algorithms.

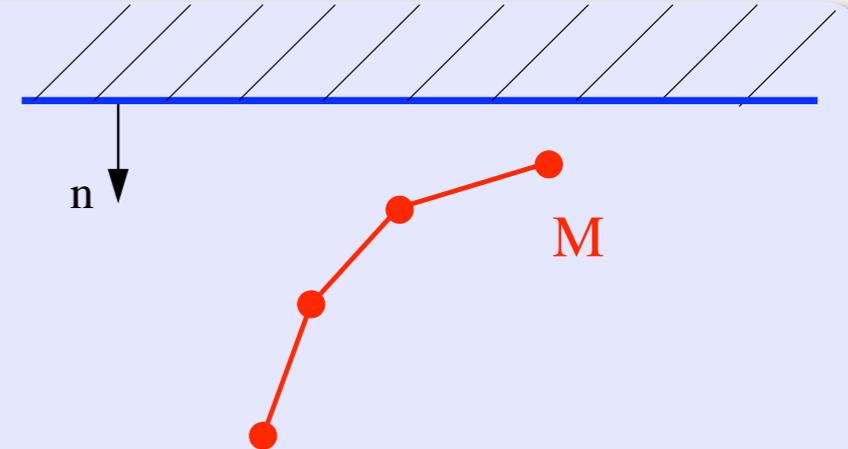
Solid-wall contact

M a solid with energy J

\mathcal{T}_h a mesh of M

$$X_h = \{\varphi_h \in C^0(M; \mathbb{R}^3), \varphi_h|_T \in P_1, \forall T \in \mathcal{T}_h\}$$

Minimization with convex constraint : $\inf_{\varphi_h \in \mathcal{U}_h} J(\varphi_h)$



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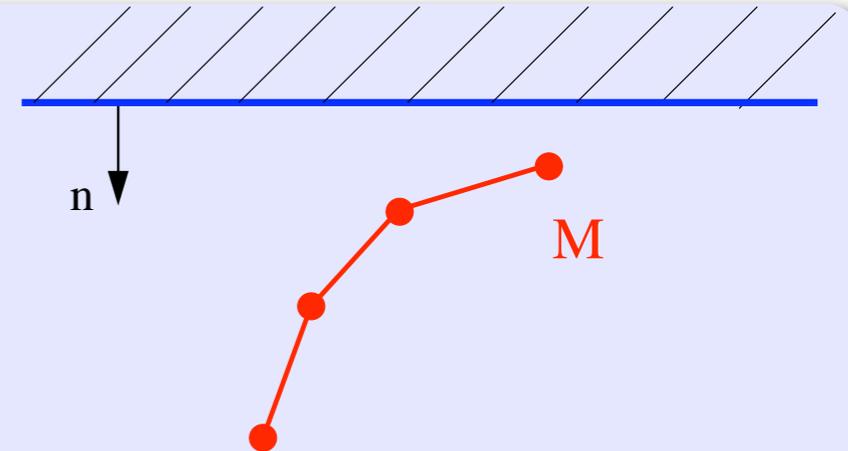
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With $\mathcal{U}_h = \{\varphi_h \in X_h, F_{x_i}(\varphi_h) \leq 0, \forall x_i \in M\}$

$$F_{x_i}(\varphi_h) = \varepsilon - \mathbf{n} \cdot \varphi_h(x_i) - c$$



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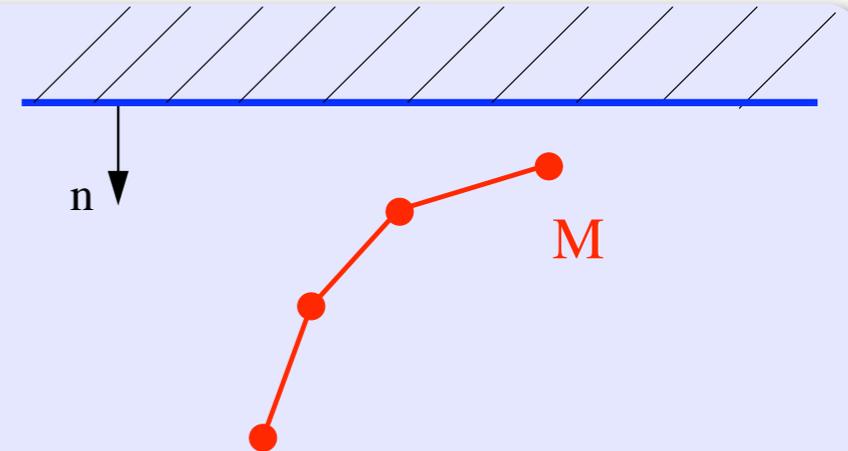
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Dual approach

$$G(\mu) = \inf_{\varphi \in X_h} \left[J(\varphi) + \sum_{i=1}^{N_\Sigma} \mu_i F_{x_i}(\varphi) \right]$$

$$G(\lambda_c) = \max_{\mu_i \geq 0} G(\mu)$$

λ_c : contact pressure

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Gradient method with projection

$$1) \langle J'(\varphi^k), \xi \rangle = - \sum_{i=1}^{N_\Sigma} \lambda_{c,i}^k \langle F'_{x_i}(\varphi^k), \xi \rangle = \sum_{i=1}^{N_\Sigma} \lambda_{c,i}^k \mathbf{n} \cdot \xi(x_i)$$

$$2) \lambda_{c,i}^{k+1} = \mathbf{P}_{\mathbb{R}^+} (\lambda_{c,i}^k + \alpha^k \nabla G(\lambda_c^k)_i) = \mathbf{P}_{\mathbb{R}^+} (\lambda_{c,i}^k + \alpha^k F_{x_i}(\varphi^k))$$

3) Iterate on k

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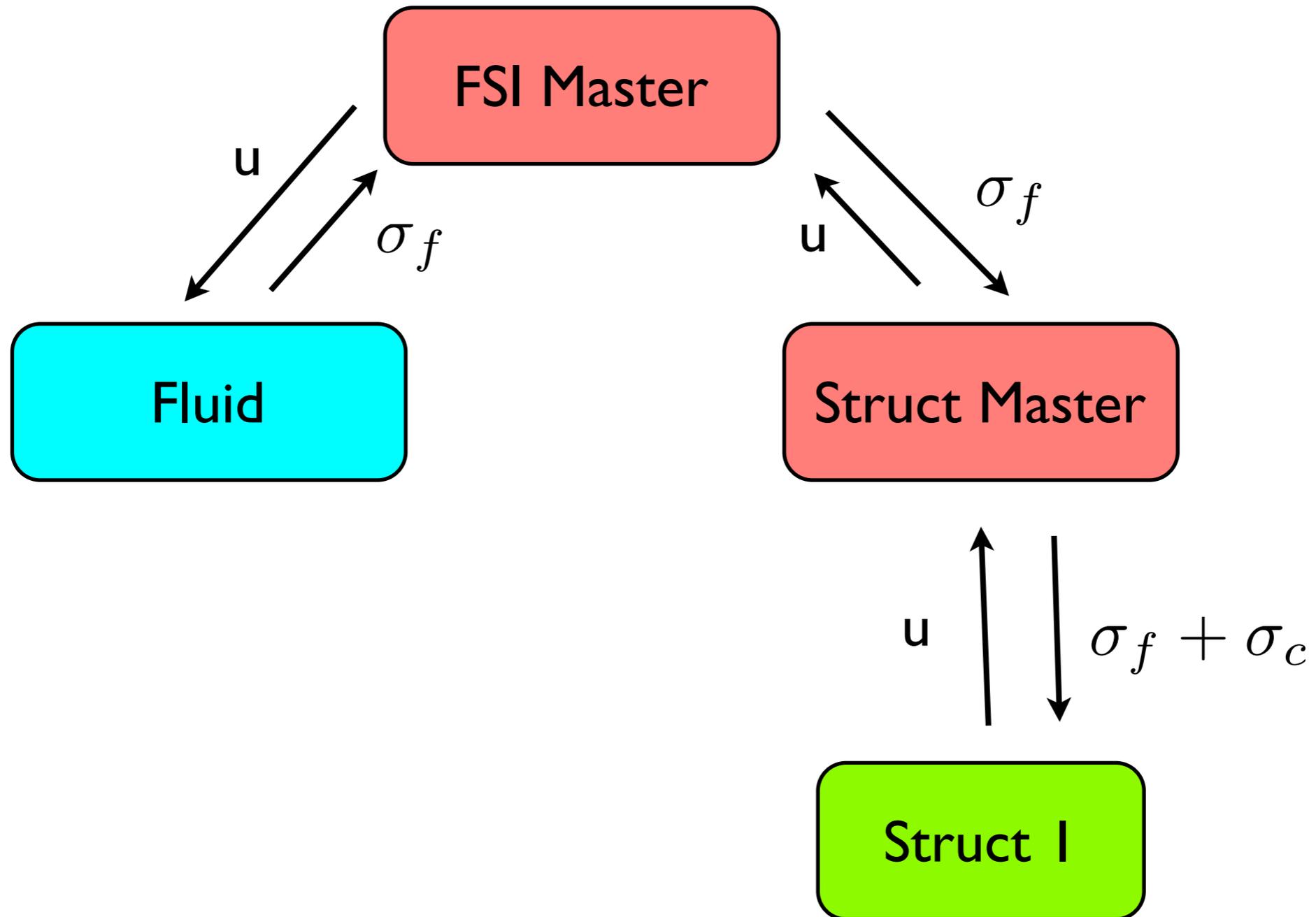
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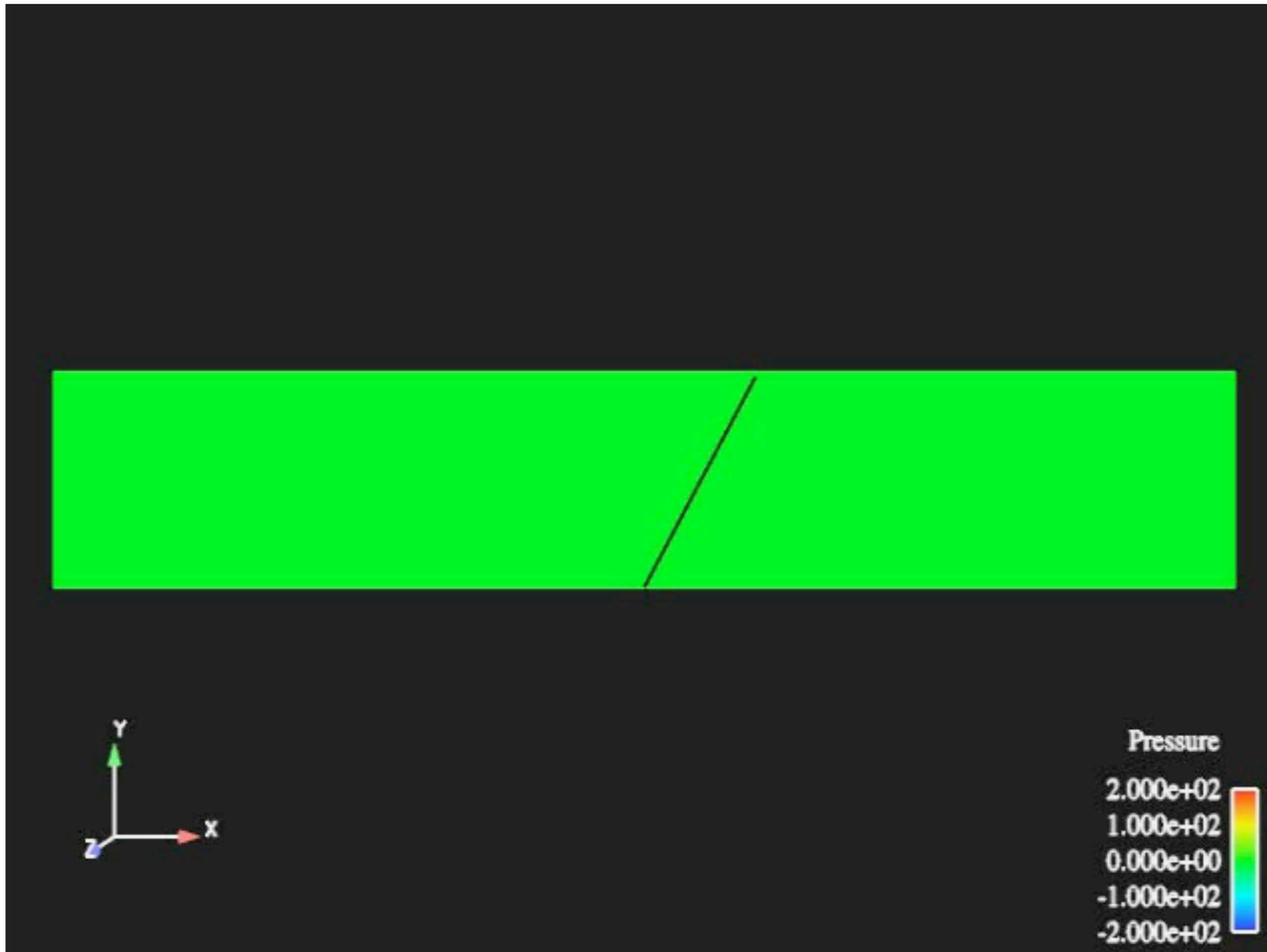
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3) Iterate on k

• The contact force is added to the hydrodynamics force

Implementation





Diniz dos Santos, JFG, Bourgat 2007

Solid-solid contact

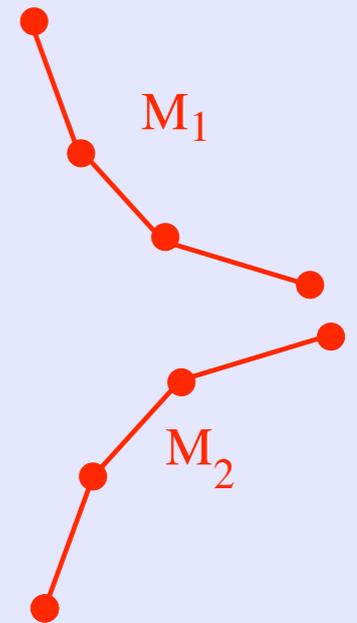
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Minimization with *non convex* constraints :

$$\inf_{\varphi_h \in \mathcal{U}_h} J(\varphi_h)$$



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\mathcal{T}_h a mesh of M

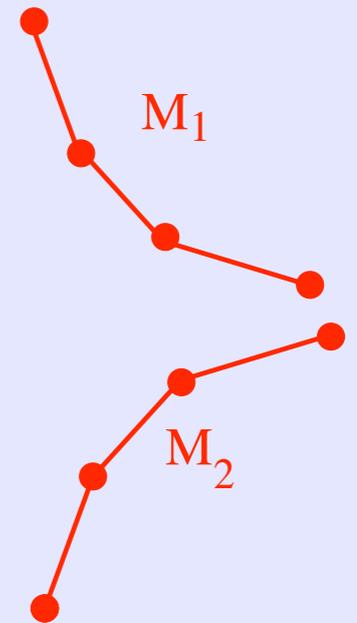
$$X_h = \{\varphi_h \in C^0(M; \mathbb{R}^3), \varphi_h|_T \in P_1, \forall T \in \mathcal{T}_h\}$$

Minimization with **non convex** constraints :

$$\inf_{\varphi_h \in \mathcal{U}_h} J(\varphi_h)$$

with

$$\mathcal{U}_h = \{\varphi_h \in X_h, \text{dist}(\varphi_h(T_1), \varphi_h(T_2)) \geq \varepsilon, \forall T_1, T_2 \in \mathcal{T}_h\}$$

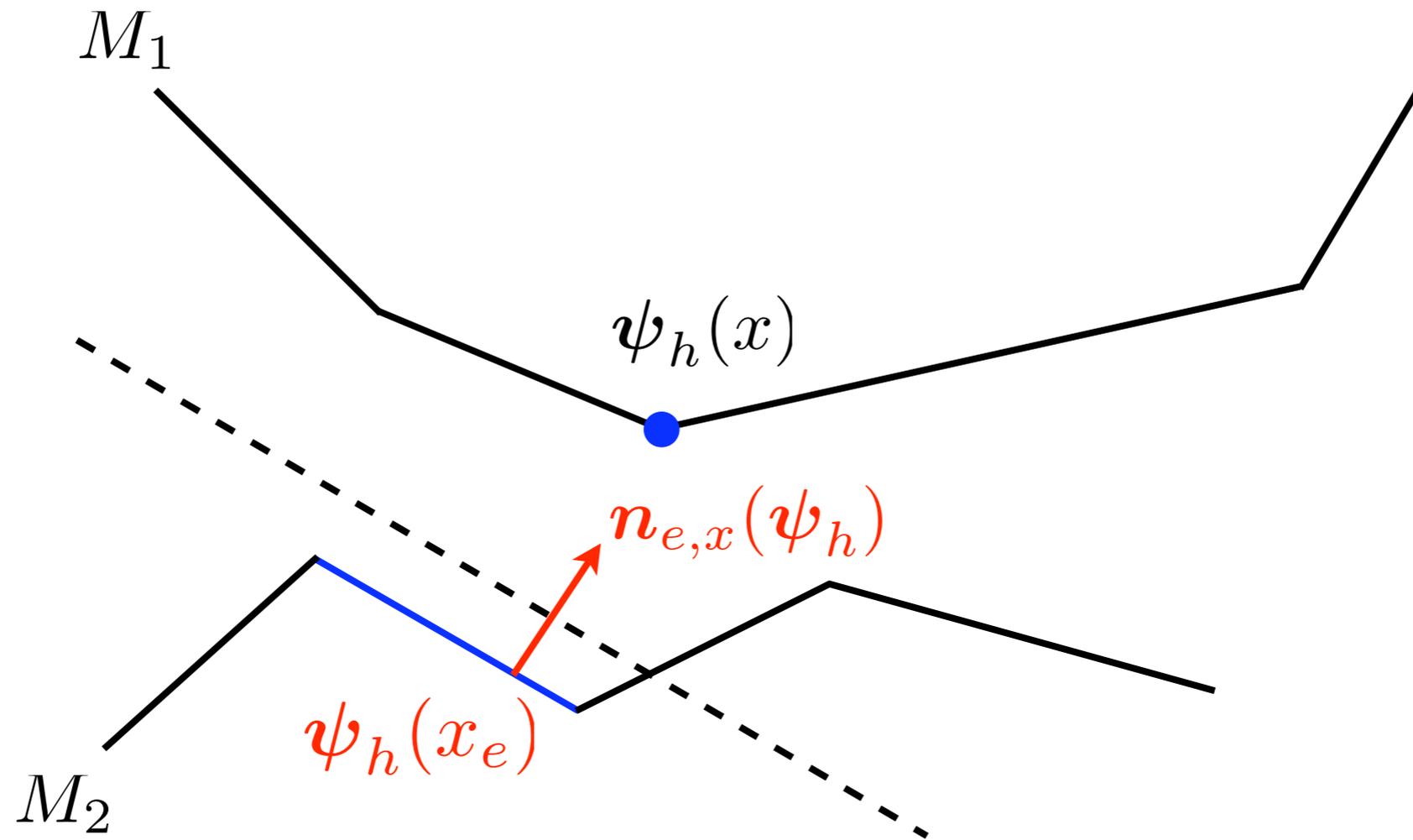


Solid-solid contact

Optimization algorithm (O. Pantz, 2007) :

- replace a problem with nonconvex constraints with a sequence of problems with convex constraints.
- Solve
$$J(\varphi_h^{k+1}) = \inf_{\psi_h \in T(\varphi_h^k)} J(\psi_h)$$
where $T(\varphi_h^k)$ is a convex neighborhood of φ_h^k
- Iterate on k until convergence

Solid-solid contact



$$T(\psi_h) = \left\{ \varphi_h \in X_h, \min_{x_e \in e} n_{e,x}(\psi_h) \cdot (\varphi_h(x_e) - \varphi_h(x)) \geq \varepsilon \right. \\ \left. \text{for all edges } e \text{ and all node } x \notin e \right\}$$



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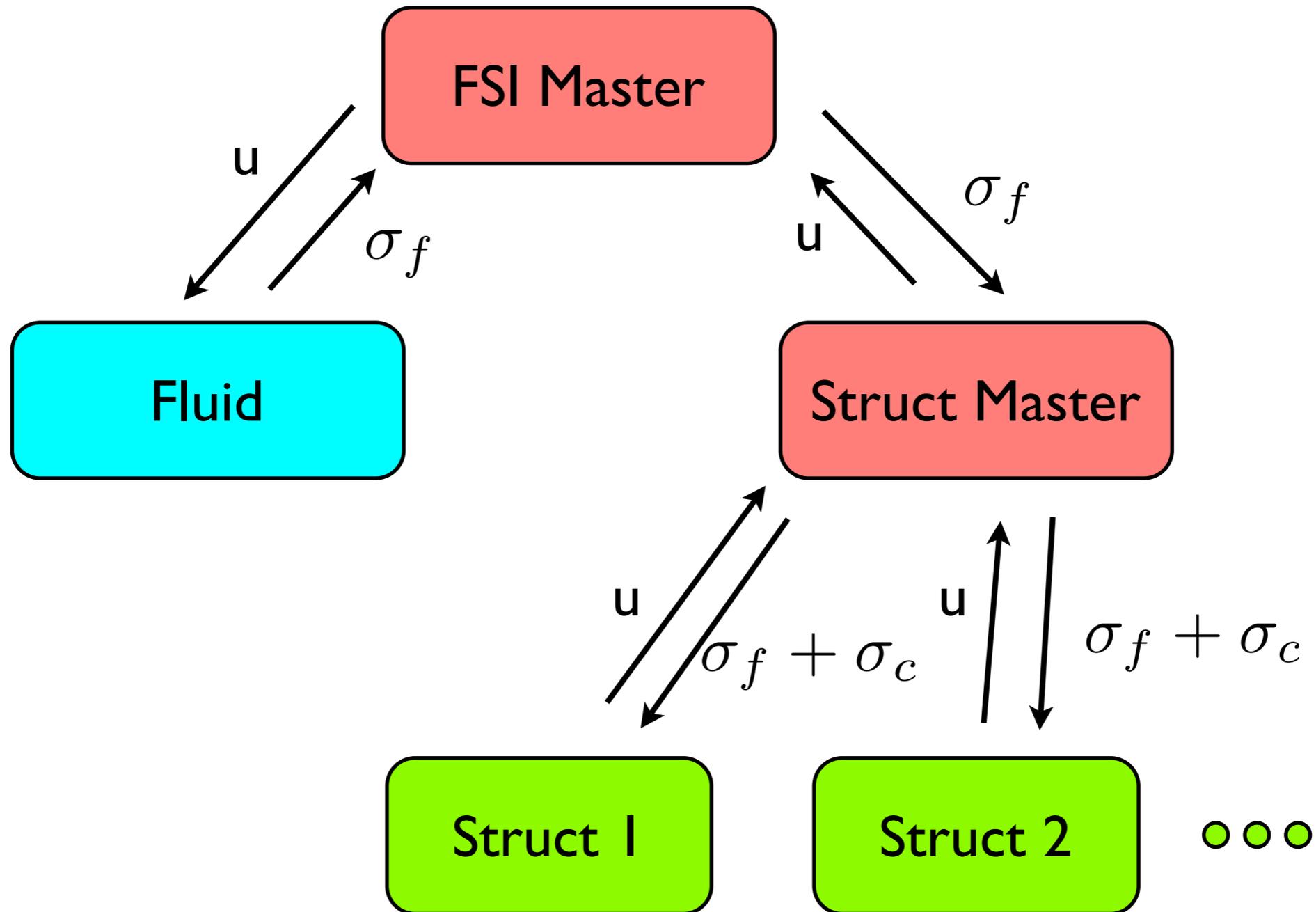
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$$T(\psi_h) = \left\{ \varphi_h \in X_h, F_{e,x}^0(\varphi_h) \leq 0, F_{e,x}^1(\varphi_h) \leq 0, \right. \\ \left. \text{for all edges } e \text{ and all node } x \notin e \right\}$$

$$F_{e,x}^j(\varphi_h) = \varepsilon - \mathbf{n}_{e,x}(\psi_h) \cdot (\varphi_h(e_j) - \varphi_h(x))$$

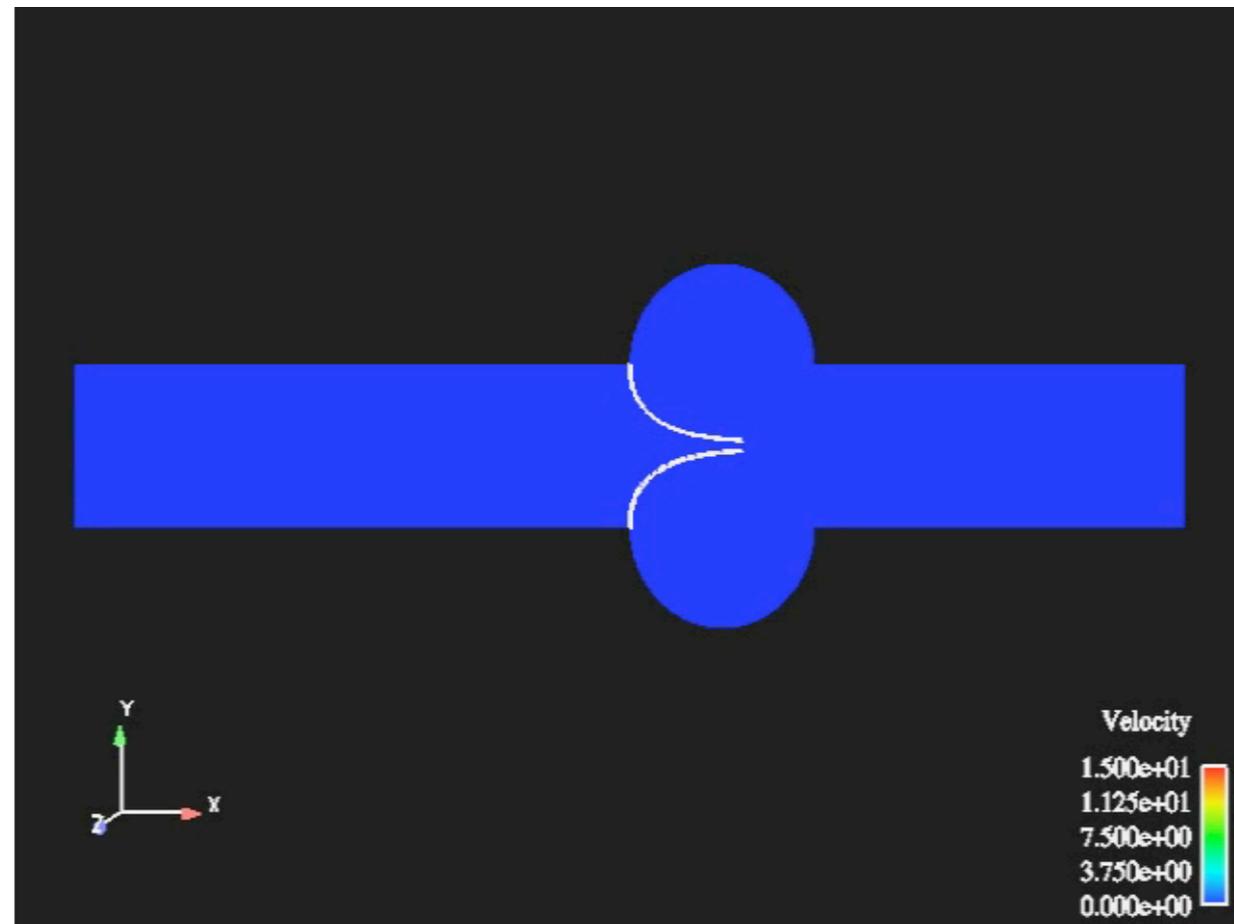
Implementation



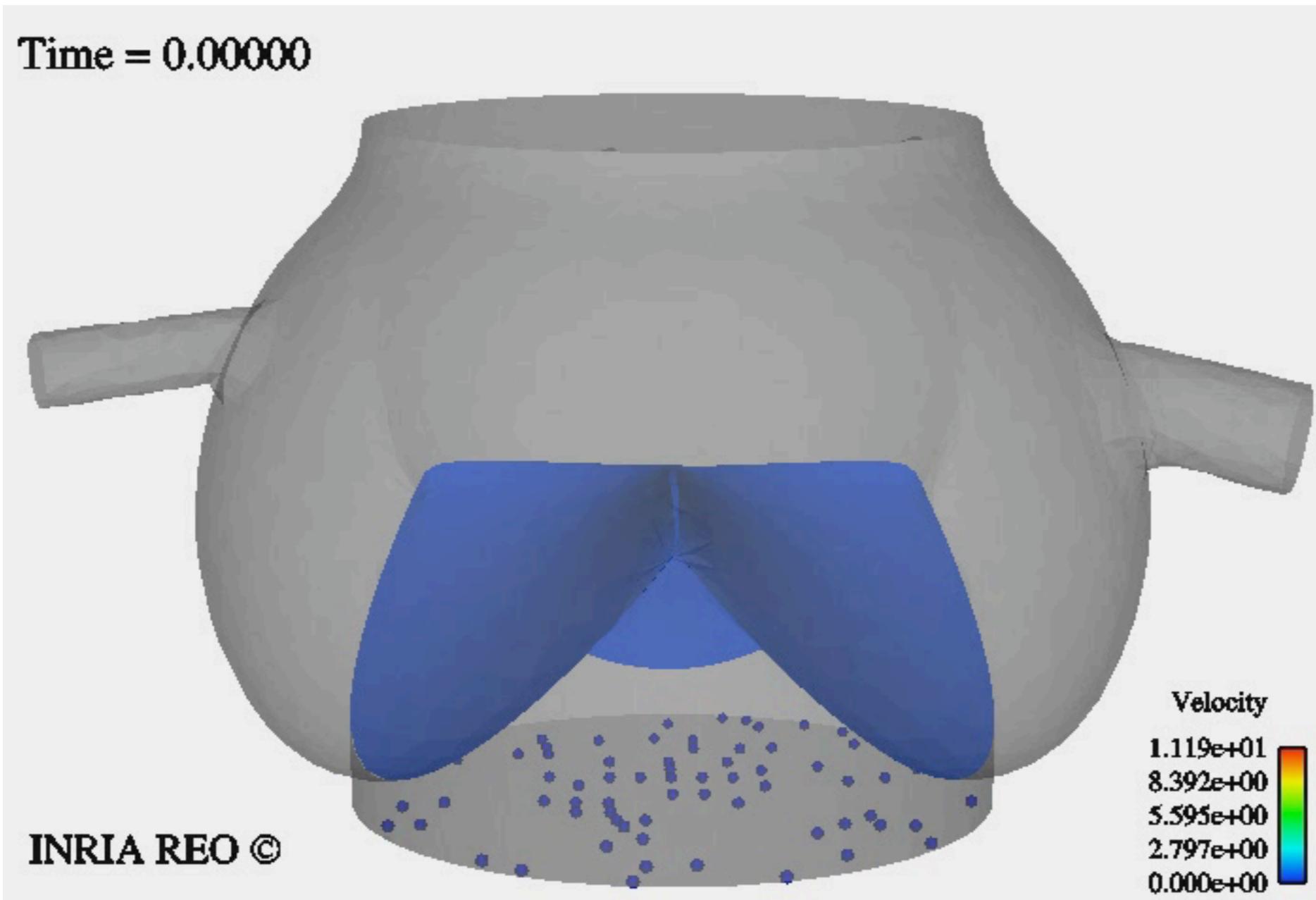
FSI & Solid-solid contact

Diniz dos Santos, JFG, 2007

FSI & Solid-solid contact



Diniz dos Santos, JFG, 2007



Astorino, JFG, Pantz, Traoré, 2008

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- Boundary conditions for FSI is still mainly an open problem
- Grand challenge: coupling numerical models with medical data.

Collaborators

- M. Astorino (INRIA)
- N. Diniz dos Santos (INRIA)
- M.A. Fernandez (INRIA)
- C. Grandmont (INRIA)
- V. Martin (UTC)
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